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## QUANTITATIVE ANALYSIS OF RESPIRATORY CELL ACTIVITY

by

Charles Lewis Webber, Jr.

A Dissertation Submitted to the Faculty of the Graduate School of Loyola University of Chicago in Partial Fulfillment of the Requirements for the Degree of Doctor of Philosophy

February, 1974

LIPRARY LOYOLA UNIVERSITY MEDICAL CENTER

### DEDICATION

I take great pleasure in dedicating this dissertation to my wife, Connie, in appreciation for her constant encouragement and positive attitude throughout the period of my graduate training.

#### ACKNOWLEDGEMENTS

The preparation of this dissertation would not have been possible without the help and encouragement of many individuals. I am greatly indebted to Dr. Walter C. Randall, Professor and Chairman of the Department of Physiology, for initially introducing me to physiological research four years ago. My sincerest appreciation is expressed to Dr. Clarence N. Peiss, Professor of Physiology and Associate Dean of the Graduate School, for directing this study and overseeing my training as a scientist. It is also a pleasure to acknowledge the expert technical assistance of Dr. Robert D. Wurster in neurophysiological problems and Dr. Robert D. McCook in computer software programming.

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#### BIOGRAPHY

Charles Lewis Webber, Jr., was born on July 26, 1947, in Bay Shore, Long Island, New York. He completed primary and secondary education requirements of the Sayville Public School system, graduating from high school in June, 1965, with a double diploma from the local district and New York State Board of Regents. He studied at Taylor University, Upland, Indiana, for the next four years and received the Bachelor of Arts degree, cum laude, in June, 1969, with a chemistry major and zoology minor.

Charles began graduate studies in June, 1969, in the Department of Physiology, Loyola University, Stritch School of Medicine, Maywood, Illinois, and was financially supported by a Research Training Grant of the National Institute of General Medical Sciences (NIGMS). After one year of study, he selected Dr. Clarence N. Peiss to direct his graduate training and research in the field of neural respiratory control. He also took advanced mathematics courses at Illinois Institute of Technology in Chicago.

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#### BIOGRAPHY (continued)

In June, 1970, Charles married Constance Anne Folkers, a 1969 Taylor graduate, from Minonk, Illinois. During his last three years of graduate training, his wife taught seventh grade language arts at Gurrie Junior High School in LaGrange, Illinois. The couple resided in Broadview, Illinois.

Charles has accepted an appointment as Postdoctoral Fellow at the Max-Planck-Gesellschaft, Bad Nauheim, Federal Republic of Germany, to continue studies on respiratory cell function with Prof. Dr. K. Pleschka. He holds associate memberships in the Society of the Sigma Xi, the American Physiological Society, and the Creation Research Society.

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- Webber, C.L., Jr. and C.N. Peiss. Computer analysis of activity patterns in single respiratory cells. Abstract, 1st Annual Society for Neuroscience, Washington, D.C., October, 1971.
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#### CHAPTER I

#### INTRODUCTION

Information transfer along central, efferent and afferent arcs of the respiratory system are coded in terms of interspike intervals of single unit spike discharges. At the output stage, respiratory muscles decode the neuronal signals into meaningful outputs of respiratory rate and depth, the two major determinants of alveolar ventilation. However, to follow dynamic changes in information flow in a control systems approach, it is necessary to evaluate mathematically the discharge patterns from various respiratory sub-systems. Comparison of such patterns can yield important information on transfer functions between various respiratory components. The plasticity of these functions during different ventilation demands can also be evaluated.

This study was designed to examine the discharge patterns of single respiratory neurons in the medulla over wide ranges of rate and depth. The combination of

new mathematical criteria and advanced computer techniques has revealed high neuronal correlates of respiratory rate and depth, identified as medullary outputs. This has been achieved by examination of thousands of interspike intervals, their distribution and sequencing.

### CHAPTER II

### LITERATURE REVIEW

## A. Respiratory Areas of the Medulla

Numerous studies during the last century and a half have implicated the medulla as the primary control area responsible for genesis of the respiratory act. Many technical advances have been made in the study of this system, but differences in opinion concerning medullary organization still exist today. In general, opposing views can be grouped into two broad categories irrespective of the experimental technique or animal used. One theory maintains that respiratory neurons can be assigned specific anatomical localizations within the medullary architecture, with a definite segregation of inspiratory and expiratory neurons. The alternate theory maintains that respiratory cells are freely scattered and intermingled throughout the reticular formation and are functionally tied together via extensive synaptic interconnections. It is important to consider the

evidence for each of these views.

The discrete localization or center theory was the first to gain prominence. Lorry in 1760 (111) confirmed the work of Galen (65) by showing that section of the spinal cord at the first cervical segment immediately arrested respiration in the expiratory position of apnea. This indirectly demonstrated that the genesis of rhythmic respiratory movements was rostral to the cord. Legallois in 1812 (107) supplied the first direct evidence that the medulla possessed respiratory function by showing that rhythmic breathing persisted in young rabbits with removal of the cerebellum and part of the upper bulb. Flourens in 1842 (59) further localized this active lower bulbar region to a one millimeter area at the apex of the calamus scriptorius. Destruction of this "vital node" halted all respiratory movements. Flourens (60) later relocated the "vital node" 2.5 millimeters on either side of the midline at the level of the obex. In 1880. Marckwald and Kronecker (118) attempted to divide the respiratory center into inspiratory and expiratory portions, and Lumsden in 1923 (112, 113, 114) distinguished between an expiratory and gasping center in the medulla of the cat by means of transection procedures.

Active expiratory and inspiratory regions were

mapped with stereotaxic placement of stimulating electrodes. Pitts, Magoun and Ranson (145) explored the brainstem of the cat from the hypothalamus to the cervical cord with a bipolar stimulating electrode and were able to elicit maintained inspiratory or expiratory responses from the medulla. Since maximal responses could not be evoked either above or below the medulla, the authors claimed that their stimulations were selective for cell bodies and not fiber tracts. Expiratory responses were concentrated dorsal, rostral and medial to inspiratory responses, each occupying approximately 30 cubic millimeters of the reticular formation bilaterally, although some overlapping was observed. Pitts (140) reconfirmed functional subdivisions of the respiratory center into inspiratory and expiratory portions in a subsequent publication. Monnier (124) arrived at similar conclusions from his own work.

In the monkey, Beaton and Magoun (23) reported the existence of two discrete regions which when activated produced either inspiratory apneusis or expiratory apnea. The inspiratory activity was located dorsal and medial to the rostral half of the inferior olive. The expiratory activity surrounded the inspiratory field rostrally, caudally, laterally and dorsally. The authors concluded

that this mapping in the monkey corresponded to that in the cat as reported by Pitts et al. (145), but this is guestionable. Amoroso, Bell and Rosenberg (6) completed a similar study in the sheep and found that respiratory responses were aggregated in the reticular formation of the medulla from the aroustic tubercles rostrally, to just behind the obex caudally. The expiratory region was located dorsal, anterior and lateral to the inspiratory region and both had bilateral representation. Ondina, Yamamoto and Masland (136) prepared stimulation maps of the rat brainstem. Respiratory regions identified by sustained inspiratory or expiratory apnea were clearly separated. The inspiratory center was found bilaterally above the rostral one-third of the inferior olive and the somewhat more diffuse expiratory center was located dorsal and caudal to the inspiratory center.

Localization of specific structures in the brainstem by the use of stimulating electrodes met with much criticism since such a large volume of tissue was activated. This technique was defended by Pitts (140) and Magoun and Beaton (115). The latter identified active respiratory sites in the medulla by stimulation, placed a lesion at the same locus and then restimulated. Lesions which extended no more than 0.7 millimeter from

the electrode tip abolished the respiratory response to the second stimulation. The authors used this as a measure of current spread during stimulation procedures.

Comroe (46) attempted to identify respiratory areas of the brainstem by microinjection of CO<sub>2</sub>-bicarbonate solutions into the brain tissue, but met with serious problems localizing the stimulus to a small area. Nevertheless, general areas which yielded immediate hyperpneic responses corresponded to the inspiratory region of Pitts (140, 145). No expiratory responses were seen.

Evidence for separation of inspiratory and expiratory regions in the medulla has also come from extracellular recordings of single respiratory cell discharges. Nelson (127) found 110 single units in the cat and concluded that the expiratory area was dorsal to the inspiratory area. He was careful to record only from cell bodies which could be distinguished from fiber pathways by a technique of wave form identification. Haber, Kohn, Ngai, Holaday and Wang (79), however, suggested a new location for the expiratory center. Recording from single cells, these workers found that the inspiratory region in the cat corresponded to the stimulation maps of Pitts <u>et</u> <u>al</u>. (140, 145), but the expiratory region was located

more caudal with no difference in dorsal-ventral distribution of inspiratory and expiratory areas.

Woldring and Dirken (180) explored the brainstem of the rabbit with extracellular microelectrodes from the caudal border of the corpora quadrigemina to the exit level of the first spinal roots. They found respiratory activity only in an area extending from the obex to a plane 3 millimeters rostral to the obex. In this area, inspiratory and expiratory cells had a definite anatomical distribution. The inspiratory area was located 2.5 millimeters from the dorsal surface and was associated with the ventromedial reticular substance at the level of the vagal rootlets. The expiratory area was located 2.0 millimeters from the dorsal surface and was associated with the dorsolateral reticular formation. The expiratory area appeared to be connected with the spinal trigeminal root laterally and coursed parallel to the solitary tract medially. Batsel (14) published similar results from microelectrode recordings in the cat, dog and monkey. The medulla was explored from 6 millimeters rostral to 4 millimeters caudal to the obex and two bilateral groups of bulbar respiratory cells were identified. The larger area was located in and along the motor nuclei of the ninth and tenth cranial nerves.

The smaller area was located ventrolateral to the fasciculus solitarius, just rostral to the obex. Inspiratory and expiratory cells could not be separated in the dorsalventral direction, but the latter were found more frequently in the caudal medulla. Batsel (14) suggested that the recorded electrical activity came from closely packed cells indicative of specialized respiratory centers.

Merril (122) was able to distinguish between two major concentrations of respiratory cells in the medulla by mapping the data from each cat separately. One group was near the nucleus ambiguus and the other was associated with the solitary tract. Achard and Bucher (1) suggested that the lateral respiratory cells were not reticular cells, but rather nucleus ambiguus motorneurons. Von Baumgarten and Kanzow (19) recorded inspiratory potentials from the reticular formation just ventral to the tractus solitarius and 1-3 millimeters rostral to the obex. Nesland, Plum, Nelson and Siedler (129) occasionally recorded from expiratory and inspiratory cells at the same location, but reported that cells with expiratory phasings were localized more caudal and dorsal to the inspiratory cells.

In contrast to the foregoing, other experimental evidence suggests that medullary neurons are diffusely

organized and do not exhibit anatomical localization of inspiratory and expiratory areas. Longet in 1847 (110) showed that respiration was not affected by localized destruction of the pyramids and restiform bodies. However, destruction of the reticular formation at the same level immediately halted respiration. Gad and Marinesco in 1892 (64) confirmed this observation by cauterizing certain areas of the medulla. Only when the reticular substance of the floor of the fourth ventricle was destroyed did breathing stop. Arnheim (8) was also of the opinion that the bulbar neurons responsible for the generation of respiration were located diffusely in the reticular gray matter.

The stimulation technique has been used to show diffuse organization. Brookhart (34) stimulated the brainstem of dogs from 9 millimeters above to 6 millimeters below the obex with microelectrodes. With low voltage stimulations he got variable respiratory rate changes which were not correlated with any structure. The results failed to confirm the existence of compact inspiratory and expiratory centers described by Pitts et al. (140, 145) in the cat. Brookhart (34) suggested that the reticular formation was the seat of primary respiratory cells without detectable anatomical

differentiation of function. Liljestrand (108) studied in depth the respiratory movements which could be induced by stimulation of the medulla both electrically and chemically. He stated that inspiratory and expiratory areas were not separated and in his own words added, "Until further evidence of a respiratory centre has accumulated the term should be strictly defined when used, or otherwise it should be avoided."

Kim and Carpenter (100) used a different stimulation technique to induce respiratory movements. Ventilation changes comparable to electrical activation of the same area could be produced by injections of isotonic solutions of  $HCO_3^-$ ,  $HPO_4^-$  or citrate into the medullary reticular formation of the cat. The apneustic responses observed could be evoked from random reticular formation sites and the authors concluded that chemical stimulation of respiratory neurons represents a functionally non-specific phenomenon.

The extracellular recording technique has also been used to demonstrate diffuse medullary organization. Gesell, Bricker and Magee (70) published the first report of single respiratory cell recordings. The medulla, upper cervical cord, thalamus, hypothalamus, midbrain and pons of the dog were explored with bipolar needle

electrodes. Areas yielding rhythmic respiratory discharges were lesioned for histological identification. In all the regions examined, respiratory potentials were found most frequently in the reticular gray in the region of the obex, but no correlation could be made associating cell type with any one particular brainstem structure, either nucleus or tract. The organization of inspiratory and expiratory regions appeared to be diffuse. The authors commented that the reticular gray is influenced by every type of sensory signal, which may explain activation of the respiratory system during different situations. Amoroso, Bainbridge, Bell, Lawn and Rosenberg (5) used metal microelectrodes to study single respiratory cell discharges in the dog, cat and rat. These electrodes recorded from a brain tissue volume which was one thousandth of that activated by a small stimulating electrode. Because of this high specificity, respiratory potentials were difficult to locate. The authors wrote, "The scarcity of respiratory potentials in the reticular formation of the medulla suggests that generally this structure does not function as a whole but only in parts. It seems to act as a trigger, periodically firing spinal, phylogenetically older, neuronal aggregates which are ultimately responsible for the

coordinated respiratory movements."

Hukuhara, Nakayama and Okada (91) recorded respiratory potentials from the striae acousticae level in the lateral reticular formation of the dog and cat brain and suggested that this was the normal respiratory center. Although this localization did not agree with that of Gesell et al. (70), no differentiation of inspiratory and expiratory areas was possible. Hukuhara et al. (91) also discussed the coursing of centrifugal respiratory pathways through the lateral reticular formation of the medulla. Salmoiraghi and Burns (155) prepared a map of the brainstem localizing respiratory discharges in the cat. While no respiratory cells were found in the pons, potentials in phase with the respiratory cycle were localized in the medulla 2-4 millimeters below the dorsal surface on either side of the obex. Inspiratory and expiratory cells could not be anatomically distinquished and were sometimes found within 100 microns of each other. Brodie (31) reported that one electrode could record activity from both inspiratory and expiratory cells at the same time and concluded that these cell types were intermingled. Harris (81) came to the same conclusion.

Finally, von Baumgarten and Salmoiraghi (21)

studied the localization of respiratory neurons in the goldfish via electrical recording. They found that respiratory cells were bilaterally organized in narrow bands extending rostrally from the mid-vagal lobes. The cells with opposite phasing patterns corresponding to inspiratory and expiratory units were not segregated into different areas. The cells laid close to the segmental columns of the motor nuclei from the fifth to twelth cranial nerves.

Conclusions defining strict medullary organization of the respiratory system are difficult to make. From the clinical work of Baker, Matzke and Brown (11), respiratory failure during bulbar poliomyelitis definitely involves pathologic alterations in cells of the nucleus ambiguus although similar structural changes are also seen among other large and small reticular cells, many of which must also subserve a respiratory function. Weighing the evidence presented, it can be suggested that any concept of medullary organization must simultaneously explain the following two characteristics. First, inspiratory cells are anatomically scattered throughout the medullary reticular formation apparently without any logical ordering. Second, inspiratory and expiratory divisions of the respiratory system each function in a

highly integrated fashion. Obviously, the respiratory representation in the medulla poses interesting structure-function problems.

### B. Apneusis

Knowledge concerning the organization of the brainstem respiratory system has been extended by many studies into the phenomenon of apneusis. It is now clear that medullary structures alone are not responsible for the coordinated act of respiration. The pons appears to contain two general populations of neurons which influence medullary respiratory cell discharge to respiratory motorneurons.

It is interesting that the definition of apneusis has slowly changed in the literature. When the concept was first introduced (ll6, ll7) it was associated with maximal inspiratory cramps which were maintained until the preparation died from asphxia. Later, apneusis was described as an abnormal respiratory pattern characterized by periodic escape from sustained inspiratory efforts (26, 87, ll2). Workers attributed this pattern to a specific cyclic function of the respiratory system which could be maintained for long periods of time. Other investigators (ll2) redefined apneusis as cyclic submaximal inspiratory holds. This, along with the
observation that apneusis was not a permanent pattern, prompted the suggestion that apneusis was the result of non-specific facilitation of medullary respiratory areas (26, 87). These differences in length and depth of inspiratory holds and duration of apneusis are a reflection of the various techniques used to induce this unusual breathing pattern.

Marckwald in 1887 (116) and 1890 (117) observed long inspiratory cramps in vagotomized rabbits if the brainstem was transected just behind the posterior colliculi. These inspiratory holds continued uninterrupted until asphyxial death if the trigeminal nerves were damaged. Vagotomy in preparations with transections placed just in front of the posterior colliculi failed to develop the characteristic inspiratory movement. Breathing simply became deeper and slower as seen after vagotomy in animals with intact brainstems. Marckwald (116, 117) concluded that the posterior colliculi contained a center inhibitory to inspiration. Loewy in 1888 (109) confirmed this observation.

Lumsden (112, 113, 114), using the transection technique, made major contributions on pontine organization. In one paper (112) he showed that vagotomy in cats with brainstem sectioned immediately behind the

posterior colliculi did not produce the inspiratory cramps described by Marckwald (116, 117). The inspiratory holds or apneusis, as Lumsden (112) called them (Greek for a holding of the breath), occurred only in cats with transections a few millimeters below the upper border of the pons when the vagi were cut. This apneusis was converted into a gasping respiration when another transection was introduced below the striae acousticae. The conclusions were obvious. That is, the lower pons contained an apneustic center which drove the gasping center of the medulla continuously when inhibition from the pneumotaxic center in the upper pons and vagi were removed. In another article, Lumsden (113) discussed his concept of an expiratory center in the medulla in order to explain active forced expirations and summarized his thoughts in a third publication (114) relating vagal impulses to central respiratory organization and rhythmic breathing.

An alternate view of apneusis was presented by Henderson and Sweet (83) and Hess (85) who suggested that the phenomenon was a manifestation of decerebrate rigidity. The authors explained that the apneusis they saw in mid-pontine cats with cold blocked vagi was due to tonic activity of medullary centers released from red nucleus inhibition by severing of the rubro-spinal

The vagi were believed to inhibit inspiration tracts. via direct inhibition of the general brainstem facilitatory mechanism. Hoff and Breckenridge (26, 87) also concluded that apneusis was best regarded as decerebrate rigidity of the respiratory system. They made the following major observations in the dog and cat. First, apneusis was not permanent as suggested by Marckwald (116, 117), but was an oscillating respiratory pattern. Second, apneusis was not total since alternating inspiration-expiration efforts were often seen superimposed on apneustic breaths. Third, as preparations deteriorated, apneusis was replaced by relatively normal respiratory patterns. Last, apneusis could be abolished by separation of the medulla from the pons as described by Lumsden (112). Breckenridge, Hoff and Smith (28) also showed that intravenously administered myanesin, a drug which blocks decerebrate rigidity, also converted apneustic breathing into normal respiratory patterns.

Stella (167) refuted the conclusions of Henderson and Sweet (83), Hess (85) and Hoff and Breckenridge (26, 87) and maintained that apneusis was a specific respiratory event. He showed that elimination of the red nucleus and/or posterior colliculi did not alter normal respiratory patterns. Apneusis resulted only when the upper pons

was removed in vagotomized preparations. This confirmed the inhibitory function of the upper pons (pneumotaxic area) first introduced by Lumsden (112). Stella (167) also demonstrated that apneusis was not dependent on proprioceptive reflexes from the respiratory muscles by showing that apneusis persisted in a deafferented brainstem preparation. This, of course, differentiated apneusis from decerebrate rigidity, since the latter could be terminated by dorsal root section.

Wang, Ngai and Frumin (176) reexamined the results of Breckenridge, Hoff, and Smith (28) who abolished both decerebrate rigidity and apneusis with myanesin. By using low doses of this drug, Wang <u>et al</u>. (176) were able to differentially block body rigidity without altering the apneustic breathing pattern. The authors interpreted these results as inferring that apneusis and decerebrate rigidity were two separate phenomena. Ondina, Yamamoto and Masland (136) qualified these results by suggesting that if apneusis were a phenomenon of bulbar facilitation, the sources of this facilitation did not lie in the same cells as those which facilitated the postural musculature. They demonstrated that in the rat, an animal which rarely displays decerebrate rigidity, apneusis can readily be induced by brainstem transection

at the mid-pons level and vagotomy without the manifestation of body rigidity.

Electrophysiological evidence supports the notion of a pontine apneustic area. Ngai and Wang (135) used the stimulation technique in cats with intact brainstems. They found that stimulation from a level 3 millimeters behind the rostral border of the pons extending caudally to the trapezoid body interrupted rhythmic respiration with a maximal inspiratory movement. The active brainstem area corresponded to Lumsden's (112) apneustic center. Kahn and Wang (96) recorded from single inspiratory and expiratory cells in midpontine cats and monitored the phrenic discharge. After vagotomy, inspiratory cells and phrenic patterns became continuous as apneustic breathing was initiated. Expiratory cells discharged only during the brief interruptions of inspiratory holds. In a central vagal stimulation study, Kerr, Dunlop, Best and Mullner (99) assigned the apneustic area to a supramedullary level at the origin of the eight cranial nerve just lateral to the midline. The authors suggested that the apneustic area may have some involvement with the vestibular system.

The removal of pneumotaxic and vagal inhibitions is important for the unmasking of apneustic drive.

Consequently, apneusis has been used as an endpoint in vagotomized preparations to locate pneumotaxic areas in the upper pons by tissue destruction. Pitts, Magoun and Ranson (147) made bilateral electrolytic lesions in the cat brainstem with stereotaxic placement of electrodes and localized the pneumotaxic area to the tegmentum of the upper few millimeters of the pons. Lesions in the inferior colliculi and red nuclei did not result in apneusis thereby refuting the work of Marckwald (116, 117) and Henderson and Sweet (83) respectively. Tang and Ruch (172) localized the pneumotaxic area in the dorsolateral portion of the rostral pons by suction destruction or electrolysis. Tang (170) later refined the location to the extreme dorsolateral portion of the anterior pontine tegmentum, the isthmus. Ngai and Wang (134) associated the pneumotaxic region with the dorsolateral reticular formation since stimulation in this area accelerated respiratory rate and destruction led to apneusis when the vagi were cut. Johnson (93) found similar results and placed the pneumotaxic area in the latero-dorsal tegmental nucleus or locus coeruleus. Baxter and Olszewski (22) also suggested that the cells of the locus coeruleus nucleus formed a major part of the pneumotaxic area.

Using the above localization data for the pneumotaxic center, St. John, Glasser and King (151) placed chronic lesions in the dorsolateral pontine regions of the cat. Rhythmic respiration was observed in all cats after recovery from anesthesia, but when the vagi were severed up to thirteen weeks later, cats with pneumotaxic center lesions immediately developed apneustic patterns. Cats with control lesions a few millimeters anterior or posterior to the pneumotaxic level did not develop apneusis. The authors concluded that their lesions chronically knocked out pneumotaxic participation in the genesis of eupnea. St. John, Glasser and King (152) later showed that vagotomized cats with chronic pneumotaxic lesions were capable of normal respiratory rhythmicity when awake. This demonstrated that higher regions of the central nervous system could maintain respiratory rhythmicity in the absence of pneumotaxic or vagi inhibitions.

From these accumulated data it has been concluded that the pneumotaxic and apneustic areas of the brainstem are directly involved with respiratory mechanisms. Unlike medullary inspiratory and expiratory areas, the pontine regions appear to be anatomically discrete.

The length and depth of apneustic breaths depend

on a number of factors besides the removal of pneumotaxic and vagal afferent inhibition. Additional factors to be considered are the chemical status of the preparation, integrity of cerebellar structures and the anesthetic drug type and level.

Stella (168) produced apneustic breathing in cats by transecting at the mid-pontine region and cold-blocking the vagus nerves. When the CO<sub>2</sub> content of the inhaled air was elevated to 8-10%, apneustic breaths became much deeper and prolonged. These results could be duplicated by using a rebreathing procedure. Hoff and Breckenridge (87) found that peripheral chemoreceptor stimulation by carotid occlusion prolonged or intensified the apneustic pattern in dogs. Also, vagotomy failed to induce apneusis in mid-pontine dogs with carotid denervation. The authors suggested from these results that apneusis derives from the interplay of peripheral carotid body and central lower pontine factors.

Ngai (130) determined the  $O_2$  consumption, arterial blood pH, PaCO<sub>2</sub>, PaO<sub>2</sub> and O<sub>2</sub> saturation during apneustic breathing in cats. Compared with control respiratory values, apneusis induced a respiratory acidosis with no change in the PaO<sub>2</sub> or O<sub>2</sub> consumption (cats breathed oxygen rich mixtures). Administration of 10% CO<sub>2</sub> increased the

depth of each apneustic breath and accelerated the apneustic cycle. The latter finding is in disagreement with that reported by Stella (168). Since this response persisted after carotid denervation, Ngai (130) concluded that apneustic cycling was probably due to the elevated arterial CO<sub>2</sub> tensions and was independent of the peripheral chemoreceptors.

Katz, Ngai, Nahas and Wang (98) studied the effect of pH alterations on apneusis. Two agents which elevate the pH (THAM, an organic buffer, and sodium bicarbonate) were infused intravenously in mid-pontine vagotomized cats displaying apneustic respiration. Neither agent altered the depth of apneusis, but THAM decreased the apneustic cycling while sodium bicarbonate increased the cycling. These apparently conflicting results were explained on the basis of possible differential distribution of the two agents across cell membranes. The authors suggested that if this were the case, the intracellular pH may be the critical factor for modulation of apneusis.

The effect of cyanide on apneusis was studied by Brodie and Borison (32). They showed that cyanide can Convert apneustic breathing into a gasping pattern, a response which was independent of peripheral chemoreceptor

denervation. Ngai (130) reported that intracarotid injection of sodium cyanide can accelerate apneustic cycling thus demonstrating that cyanide does exert a peripheral influence also.

Although it is not commonly recognized, the cerebellum appears to have some connections with the brainstem respiratory system. Henderson and Sweet (83) mentioned that cerebellectomy could produce apneusis which disappeared after a short period. Using mid-pontine cats, Glasser, Tippett and Davidian (76) studied respiratory pattern changes during cerebellar depression induced by several techniques: occlusion of the cerebellar arteries, procaine or xylocaine application to the surface or subcortex of the cerebellum, or removal of part or all of the cerebellum by suction. Irrespective of the method used, cerebellar depression in mid-pontine cats with intact vagi led to a fall in respiratory rate and an increase in respiratory depth to the point of apneusis in many cases. The authors concluded that the cerebellum exerted a tonic inhibitory influence on the brainstem respiratory mechanism. The inhibition might have arisen in the anterior and posterior lobes of the corpus cerebelli, but brainstem projections were unknown. Another interesting report from Gesell, Bricker and Magee (70)

suggested that the cerebellum may contribute to the integration of the respiratory act. They were able to locate three single cell potentials in the region of the brachium conjunctivum (superior cerebellar penduncle) which had respiratory discharge patterns. It is possible that these were efferent fiber tracts from the cerebellum to the pons or medulla mediating respiratory inhibition.

There is a considerable body of evidence which indicates that high levels of barbiturate can convert normal respiratory patterns into apneustic ones even when all brainstem structures and vagi are intact. Harris and Borison (82) anesthetized cats with 36 mg/Kg pentobarbital and stimulated inspiratory regions of the medulla during pentobarbital titration until the spontaneous respiration was arrested. With progressively higher doses, the threshold to produce apneusis via medullary stimulation consistently decreased. At an accumulated dose of 45 mg/Kg pentobarbital, the respiratory cycle was lengthened with a progressive increase in the expiratory phase. With higher doses approaching the respiratory depression level of pentobarbital (mean 50 mg/Kg, range 33-70 mg/Kg) inspiratory holds of apneusis were observed in preparations with intact brainstems and vagus nerves. These results showed that pentobarbital selectively depressed systems

which were inhibitory to inspiration. The inspiratory apparatus was presumably depressed to some extent since apneustic breaths were of low amplitude.

A similar study was done by Ngai (131) who extended stimulation sites to the pons during pentobarbital accumulation in the midcollicular, vagotomized cat. At doses from 24 to 30 mg/Kg the inspiratory movements became apneustic in type except for a greatly reduced depth. At this same dose level, stimulation of the pneumotaxic region failed to accelerate respiratory rate as in control cases, but central vagal stimulation was still effective. The author concluded that pentobarbital produced apneusis in the decerebrate vagotomized cat by blocking pneumotaxic inhibition of the apneustic areas. Comparison of Ngai's (131) data with those of Harris and Borison (82) reveals that the pneumotaxic mechanism is more sensitive to pentobarbital depression than is vagal afferent feedback. St. John, Glasser and King (151) reported that cats with chronic pneumotaxic lesions, anesthetized with 35 mg/Kg pentobarbital, repeatedly had bouts of apneusis following small additional doses of pentobarbital and bilateral vagotomy. A similar prolongation of the inspiratory phase with thiopental has been published by Brodie (31).

Korczyn, Leibowitz and Bergmann (104) studied the

effect of pentobarbitone dose level on the respiratory response evoked by sciatic nerve stimulation. Control responses ranging from acceleration at low frequency stimulation to deceleration of breathing at high frequency stimulation could all be blocked by high doses of the barbiturate. These data parallel the blockade of vagal inhibition in the experiments of Harris and Borison (82) who observed apneusis in vagi intact cats with high doses of pentobarbital.

Robson, Houseley and Solis-Quiroga (148) studied barbiturate effects on respiration at the single neuron level. Successive increments of sodium pentobarbital or sodium thiopental in cats caused either the inspiratory or expiratory cell discharges to fire continuously. The inspiratory cell pattern resembled that of apneusis. The authors explained that the elevated excitatory firing of expiratory cells was due to barbiturate arrest of mutually inhibitory pathways between inspiratory and expiratory neurons.

Finally, Naifeh, Huggins and Hoff (125) studied respiratory pattern changes in crocodiles during pentobarbital accumulation. The authors termed this technique "anesthetic dissection," but were not able to induce apneusis as observed in other animal preparations under

similar conditions. These results were explained by Naifeh, Huggins and Hoff (126) in another publication in which serial transections were made in the crocodile brainstem. No evidence was found for an apneustic area in this animal. This is a good example of species differentiation in brainstem organization of the respiratory control system.

## C. Medullary Outputs

The primary function of respiration is to maintain arterial blood oxygen, carbon dioxide and hydrogen ion concentrations in homeostatic proportions. To do this, metabolic drives determine the proper alveolar ventilation for the situation at hand by adjustment of respiratory rate and tidal volume, the two outputs from the brainstem respiratory complex. Although there are numerous respiration rate - tidal volume combinations which can generate a specific alveolar ventilation, workers such as Rohrer (149) and Otis, Fenn and Rahn (137) have suggested that the respiratory frequency is selected so as to minimize the amount of work expended by the respiratory musculature. Alternately, Mead (120, 121) has proposed that breathing is adjusted to minimize the muscle force instead of the work. In either case, any acute or chronic change in the mechanical properties of the chest or lung should manifest itself by a different optimal

breathing frequency. Also, removal of major compliance feedback via vagotomy should increase the work of breathing. Zechman, Salzano and Hall (184) confirmed this by showing that the regulation of rate and depth of breathing was less efficient when pulmonary afferents were blocked. Salzano and Hall (157) later reported that vagal reflexes did not influence the work of breathing during severe hypoxia or hypocapnia as much as they did during normal or obstructive breathing.

It is difficult to rank medullary outputs in order of primary (active) or secondary (passive) control. Many experiments have shown that rate and depth components are highly integrated and only a few have succeeded in separating the outputs into two component systems. The following discussion will consider system interactions responsible for the genesis of rate and depth outputs.

The respiratory rate output presents itself as a two-fold problem. First, generation of the basis rhythmicity must be explained and second, basic mechanisms which modulate this rhythm need to be examined. Hoff and Breckenridge (88) have classified breathing into three normal patterns (eupnea, sighing and panting) and three abnormal patterns (Cheyne-Stokes, Biots and apneusis). Each pattern is characterized by a specific rate-depth

combination which derives from medullary, pontine and vagal afferent interactions.

A large body of experimental evidence suggests that respiratory systems of the medulla are spontaneously rhythmic. One of the first observations came from Lumsden (112) who showed that medullary cats gasped rhythmically. Stella (167) reported that regular and smooth respiration was seen in the cat after thorough deafferentation of the medullary centers and concluded that the pattern was due to automaticity of the centers involved. Hoff and Breckenridge (87) showed that a dog can continue to breath for 5 to 6 hours in an approximately normal fashion after having been deprived of all pontine and vagal connections. The authors suggested that the rhythm was maintained via reciprocal innervation of inspiratory and expiratory neurons. In another paper, Breckenridge and Hoff (26) repeated these experiments in the cat. Again, medullary preparations showed rates and depths similar to those seen in midcollicular preparations before vagotomy. The authors concluded that medullary centers were automatic and were regulated only secondarily by facilitatory and inhibitory areas of the brain. Breckenridge and Hoff (27) later showed that breathing could be maintained reflexly when medullary centers were depressed to apnea

following drug administration or anoxia.

other workers have agreed that the medulla possesses inherent rhythmicity. Ngai, Frumin and Wang (133) wrote, "The medullary respiratory centers have an autonomous rhythm when released from the influence of pneumotaxic and other pontine centers and afferent vagal impulses." Tang (170) wrote, "It thus appears that vagal and pneumotaxic afferent influx is not the sole determinant of respiratory periodicity for rhythmic breathing persists after elimination of such influx."

Brodie and Borison (33) attempted to study the relationship between gasping mechanisms and the generation of other rhythmic forms of respiration. In decerebrate cats, gasping could be induced by stimulation of the floor of the fourth ventricle a few millimeters rostral to the obex. Since ablation of Pitts' (145) expiratory region did not abolish this gasping response, the workers suggested that the gasping rhythm was not due to reciprocal connections between inspiratory and expiratory neurons. An alternate interpretation is that all expiratory cells were not destroyed.

Ondina, Yamamoto and Masland (136) observed the medullary rat for a prolonged time and described the development of respiratory incoordination or ataxia

consisting of a dissociation of inspiration-expiration sequencing. The authors suggested that this might have been due to altered linkage between loosely associated inspiratory and expiratory systems in the cat medulla.

In a series of stimulation experiments, Borison (25) described a spasmodic respiratory response which could be evoked from activation of the dorsolateral region of the myelencephelon. The response consisted of a series of strong inspiratory and expiratory movements every one to four seconds. Borison (25) suggested that medullary cats without pontine and vagal connections may rhythmically breathe or gasp because of oscillatory drives from this spasmodic center.

Other workers have suggested that gasping is not a normal respiratory pattern. Hukuhara and Nakayama (90) showed that eupneic-like gasping did not develop immediately following isolation of the medulla, but depended on deterioration of the animal. Barcroft (13) described gasping as an all or none type of breathing in which inspiratory depth appeared to be maximum. Brodie and Borison (32) showed that gasping rate was not increased by chemoreceptor activation at low PaO<sub>2</sub>. Ngai (130) showed that gasping provided inadequate ventilation for the cat, resulting in respiratory acidosis. From this

evidence it is concluded that medullary areas are spontaneously rhythmic, but the isolated medulla is incapable of providing adequate ventilation.

Kahn and Wang (96) emphasized that pontine circuits must be accounted for in any explanation of the genesis of eupneic respiration. Coordinated oscillations of pontine and medullary structures was demonstrated by Adrian and Buytendijk (4) in isolated goldfish brains. They recorded gross potential discharges from the vagal lobes which oscillated at frequencies close to the gill movement rhythm in the intact fish. This paper demonstrated that rhythmicity can be present in the absence of afferent input, although the frequency did depend on the  $O_2$  and  $CO_2$  tensions in the surrounding fluid.

Mechanical afferent input can be eliminated by pharmacological blockade of the respiratory musculature. Von Baumgarten and Salmoiraghi (21) recorded rhythmic cell discharges from respiratory neurons in goldfish treated with succinycholine to produce myoneural block. Gesell, Atkinson and Brown (69) showed that curare-induced motor paralysis in the dog did not block rhythmic phrenic discharges. Kahn and Wang (94) reported the same results in gallamine-blocked cats. Joels and Samueloff (92) found that the recurrent laryngeal nerve still

exhibited rhythmic bursts of action potentials in the dog and cat whose respiratory movements had been blocked with succinlycholine.

While there is general agreement that midcollicular-decerebrate and vagotomized preparations exhibit rhythmic respiratory movements, the mechanism for the genesis of these oscillations is still disputed, mainly due to differences of opinion on pontine-medullary organization. Lumsden (113) attributed rhythmicity in the mammal to an interaction between his apneustic and expiratory centers which were both under the control of the higher pneumotaxic center. He suggested that the gasping center was overridden by pontine influence when both pons and medulla were intact.

Pitts, Magoun and Ranson (147) suggested that medullary centers were not inherently rhythmic since their medullary cats displayed apneusis. Rhythmic breathing was believed to be due to periodic inhibition of the tonically active inspiratory areas via pneumotaxic or vagal afferent feedback. Although rhythmicity could be explained on the basis that the pneumotaxic system was either spontaneously rhythmic or reflexly activated via proprioceptive afferents like the vagal mechanism, the authors favored the concept that the inspiratory area

sent collaterals up to the pneumotaxic region to activate inhibitory outflow. The reciprocal interchange between these two areas could produce rhythmic respiration even when the vagi were severed.

Wang, Ngai and Frumin (176) modified the schema of Pitts <u>et al</u>. (147), in whose experiments a portion of the lower pontine area had been left intact in the preparation of medullary animals. Wang <u>et al</u>. (176) made a definite distinction between the apneustic region of the lower pons and the medullary inspiratory area. Rhythmicity was believed to result from periodic inhibition of the apneustic region by vagal afferents and by the pneumotaxic area which was activated via apneustic center output. The authors suggested that inspiratory areas of the medulla, passive by themselves, were driven by apneustic outflow.

The pneumotaxic region may exert some modulatory control on respiratory rate since both Ngai and Wang (134) and Johnson (93) have shown that stimulation of the dorsolateral reticular formation of the pons accelerated respiratory rate. Kahn and Wang (95) studied the role of the pneumotaxic area in the establishment of rhythmicity by examining phrenic nerve discharges. Bilateral vagotomy had only slight effect on the phrenic discharge

pattern. Mid-pontine transection, however, greatly modified the discharge which became semi-continuous, yet still oscillatory. It was concluded that the pneumotaxic center provided important information for respiratory manifestation of eupnea and rate-setting control. Cohen and Gootman (44) suggested that the pneumotaxic region may be involved in reverberating mechanisms of respiratory rhythmicity in the brainstem.

Further evidence of pneumotaxic function has come from two different laboratories although both substantiate each other. First, Bertrand and Hugelin (24) delivered single or double stimuli, given at random within the respiratory cycle, to the nucleus parabrachialis medialis of the upper lateral pons. They found that the phrenic discharge could be synchronized by this pneumotaxic stimulation suggesting direct excitation of a self-reexciting system acting as a pacemaker. Cohen (43) brought the evidence one step further and was able to differentiate between two pneumotaxic functions: (1) stimulation of the dorsolateral pons facilitated phrenic discharge with earlier burst termination and decreased the expiratory phase; (2) stimulation of the ventrolateral pons reduced the phrenic discharge with an even earlier burst termination and prolonged the expiratory phase. The phase

switching response was shown to be dependent on stimulus current, frequency, total number of stimuli, and the timing of stimulation in relation to the respiratory cycle. Cohen (43) concluded that the pneumotaxic region may function to smooth transitions from inspiration to expiration and vice versa.

Tang (171) reported that destruction of the pneumotaxic center in cats with intact vagi depressed the depth response to CO2. The respiration rate increase evoked by CO, was essentially unaffected. Tang (171) suggested that the pneumotaxic mechanism was responsible for depth modulation and could maintain constant rates in absence of vagal feedback. The pneumotaxic control was believed to operate through the apneustic system. St. John (150) confirmed this observation in conscious cats with either unilateral or bilateral chronic lesions placed in the pneumotaxic region. These cats displayed diminished tidal volume responses to hypercapnia. The tidal volume response to hypoxia was unaffected, however, and St. John (150) concluded that other regions of the central nervous system had tidal volume regulating capability in the conscious animal.

For a long time it has been recognized that bilateral vagotomy results in slower and deeper breathing.

As early as 1868, Hering and Breuer (84) and Breuer (29) demonstrated that inflation and deflation reflexes were mediated via vagal afferents and concluded that the oscillatory nature of breathing was regulated by pulmonary reflexes. Widdicomb (178, 179) has reviewed a multiplicity of reflexes which are carried in the vagu nerves, but one, the inflation reflex, has prime importance in directly modifying respiratory rate and depth. Consequently, much evidence has been complied on this reflex concerning receptor site, afferent path, anatomical and functional central projections and involvement in rate and depth control.

Receptors mediating the inflation reflex have been found in the small and large air passages in the lungs. Whitteridge and Bülbring (177) assigned a bronchial or bronchiolar location to the receptors and Hammouda and Wilson (80) showed reflex inhibition of inspiration by tracheal distension. Davis, Fowler and Lambert (49) found that many pulmonary afferents exhibited discharge patterns which paralleled airway pressures more closely than lung volume changes and concluded that the receptors were located in the air passages. An interesting confirmation of this came from Aviado and Schmidt (10) who showed that steam inhalation blocked the inflation reflex

without any apparent alveolar damage.

The afferent nervous pathway for the inflation reflex has been established as vagal. Hering and Breuer (84) and Steffensen, Brookhart and Gesell (166) showed that the inflation reflex could be blocked in the dog, cat and rabbit by cooling the vagi to 8°C while other vagal reflexes were left unimpaired. Paintal (138) identified fibers mediating the inflation reflex as belonging to the A $\alpha$  and A $\beta$  groups. Einthoven (52) in 1908, studied vagal afferent action currents from the cut peripheral vagus nerve with the string galvanometer and showed that discharge frequency increased with inflation of the lungs. Adrian (2) recorded from single inflation afferents using the new fiber splitting technique. Discharges were identified by lung inflation and receptors were found to be slowly-adapting to maintained lung inflations. Knowlton and Larrabee (103) confirmed this observation, but also described a second rapidly-adapting receptor discharge.

Inflation afferents project to the brainstem in the rostral vagal rootlets and distribute to the vagal nucleus and solitary tract of the cat as shown by Foley and DuBois (61). Wyss (182) showed that central vagal stimulation responses could be blocked by localized lesions in the tractus solitarius. He concluded that the

tractus solitarius is probably the locus proper of vagal respiratory reflex centers. Harris (81) applied single shocks to the vagi and recorded maximal evoked potentials in the medullary tractus solitarius, nucleus solitarius and nucleus ambiguus. Wyss, Andereggen and Oberholzer (183) suggested that the afferent fibers synapse in the solitary nucleus and then travel caudally in the solitary tract. Culberson and Kimmel (48) found degenerated vagal afferents which coursed dorsomedially through the medulla, passed through the spinal trigeminal tract and entered the tractus solitarius. These connections may interface respiratory reflex afferents with inspiratory and/or expiratory areas of the medulla.

Other workers believe that vagal afferent fibers project to the apneustic region in the lower pons. Kerr, Dunlop, Best and Mullner (99) observed that apneustic patterns in mid-pontine vagotomized rabbits could easily be modified by central vagal stimulation. Wang, Ngai and Frumin (176) found that vagotomy failed to alter gasping patterns in medullary cats. However, Hoff and Breckenridge (88) showed that vagotomy could release eupnea by increasing rate and depth, provided vagal inflow was initially intact in the medullary dog. Finally, Ngai and Wang (135) showed that upper pontine transection or removal of the

pneumotaxic area had very little effect on activity of the inflation reflex. From all of this evidence, it is believed that respiratory vagal afferents have an influence confined to medullary and lower pontine brainstem structures.

Evidence has accumulated that vagal afferents affect both the inspiratory and expiratory phases of respiration. Wyss (181) was able to produce opposite respiratory responses in the monkey by stimulating the central vagus at different frequencies. Low frequency stimulations (30-80 Hz) caused slight but distinct inspiratory effects with rate acceleration. High frequency stimulations (100-400 Hz) caused marked respiratory slowing with shifts favoring expiratory movements. These results were ascribed to selective activation of the inflation and deflation reflexes respectively. Pitts, Magoun and Ranson (146), using constant stimulating frequency of 240 Hz were able to evoke inspiratory or expiratory movements, respectively, by low or high intensity stimulation of the central vagus of the cat. In either case, stimulation of the inspiratory or expiratory center would override vagal stimulation effects. Pitts et al. (146) discussed results in terms of reciprocal inhibition between inspiratory and expiratory systems.

Gesell and Worzniak (74) made the comment that either inspiration or expiration may coincide with pulmonary inflation by a pump. Dirken and Woldring (51) investigated this further by occlusion of the airways during either the inspiratory or expiratory phase of spontaneous respiration in the rabbit. Occlusion during inspiration led to a gradual decrease in lung volume with a subsequent decrease in vagal afferent discharge frequency. Occlusion during expiration produced just the opposite results. Also, inspiratory occlusion tended to elevate the discharge frequency of expiratory cells, but had no effect on inspiratory cell frequency. Blockade of the vagus by anelectrotonus depressed expiratory discharges but enhanced inspiratory discharges. Stimulation of the central vagus at 9 Hz depressed inspiratory cells and at 200 Hz inspiratory cells were completely inhibited. Expiratory cells tended to go into continuous patterns during vagal stimulation at both frequencies. Dirken et al. (51) came to the conclusion that vagal afferents activate expiratory cells, while they reciprocally inhibit inspiratory cells.

Finally, Gesell, Atkinson and Brown (69) suggested that the act of respiration may be coordinated by vagal afferents that shift their drive to the quiescent medullary

center. This could explain the smooth transition between inspiratory and expiratory phases.

The vagal inflation reflex is of prime importance for control of rate and depth mechanisms. Gesell, Steffensen and Brookhart (73) concluded that, "The pulmonary vagi exercise two diametrically opposite functions: curtailment of the central respiratory discharge which reduces the depth of breathing, and acceleration of the inspiratory act, which allows increased depth of breathing." Tang (171) found that CO<sub>2</sub> administration failed to induce a rate change if the vagi were severed. Only changes in depth were observed. In the absence of pneumotaxic circuits, vagal afferents maintained a relatively constant depth during respiratory stimulation. Von Euler, Herrero and Wexler (55) also reported that the increase in respiratory rate during CO2 stimulation depended on intact vagal mechanisms. The conclusions of Nesland, Plum, Nelson and Siedler (129) were identical.

Shannon, Zechman and Frazier (162) studied the first-breath response of inspiratory cells during mechanical loading in cats. In preparations with intact vagi, elevation of the resistance or elastance led to an increased depth and decreased rate of respiration, which were paralleled by increased frequency and increased

duration of single cell discharges. Vagotomy abolished the single cell changes during loading, but depth increases were still present. The authors concluded that the vagi were the only source of sensory information for activation of medullary inspiratory neurons during mechanical loading. Increase in depth in vagotomized preparations was believed to be due to modulation at the spinal cord level involving facilitation of external intercostal motor activity by their muscle spindles during loading. This conclusion was confirmed by Shannon and Zechman (161).

Finally, Fallert and Mühlemann (57) studied entrainment of respiratory centers during pump inflation with different tidal volumes and frequencies in the intact rabbit. Elevation of inflation volume increased the frequency range to which the rabbit would entrain. Small frequency ranges correlated with small volume inflations. The authors concluded that the Hering-Breuer reflex was important for determination of respiratory rates and depths.

## D. Discharge Patterns

The ability to monitor single cell activity from the central nervous system has been of great value in the study of respiratory control. Various testing

procedures have been introduced whereby primary respiratory neurons can be distinguished from other cell types. Qualitative and quantitative assessment of respiratory cell discharge patterns have yielded satisfactory neural correlates of respiratory rate and tidal volume outflows from medullary structures. Consequently, numerous respiratory cell subtypes have been described and new theories on respiratory rhythmicity have been introduced.

Single respiratory potentials can be recorded from the medulla by using glass or metal microelectrodes (12, 20, 62, 78, 89). Gesell, Bricker and Magee (70) first reported that finding extracellular respiratory discharges was slow and tedious work. Von Baumgarten (16) found only 23 cells with 900 penetrations using 25 microelectrodes. Salmoiraghi and von Baumgarten (154) worked for a year and were successful in penetrating only eight respiratory cells for intracellular recording. Once located, extracellular respiratory potentials can be recorded for extended periods of time. Brodie (31) reported that he could usually hold cells for 30-60 minutes. Occasionally, cells were observed for more than seven hours.

Positive identification of primary respiratory neurons is based on phasing and spiking characteristics of the discharges and modification of patterns during

various testing procedures. Although both tonic and phasic cells may function in respiratory systems, the phasic cells have been classified as primary respiratory cell candidates since they fire during one phase of respiration and are quiescent during the alternate phase. Classically, respiratory neurons are grouped into inspiratory or expiratory categories. Tonic cells can show a frequency peaking in phase with the respiratory cycle, but these cells never become quiescent.

Care must be taken to show that phasic discharges do not arise from movement artifacts. Various techniques have been used to eliminate mechanical movement. Von Baumgarten, Kanzow, Koepchen and Timm (20) covered the brainstem with a thick layer of stiff agar jelly before recording respiratory potentials. Batsel (15) reported that cisternal drainage resulting from compression of the abdomen and chest was equal to or superior to the use of agar to arrest movements. Batsel (14) also found that cells responding to fluctuations in the blood pressure, which has a slow oscillating component in phase with respiration, could not be recorded from for a long time. Artifacts from this source were eliminated because of their instability. Cohen (39, 40, 41) used cats with neuromuscular blockade to avoid movement potentials. Movements

due to pump inflations were minimized by using preparations with a pneumothorax. Finally, von Baumgarten (17) introduced a floating electrode technique which permitted recording of respiratory potentials from moving brainstems.

probably the best way to screen out rhythmic discharges due to movement is by examination of the spike potentials. Dirken and Woldring (51) and Hukuhara, Nakayama and Okada (91) used constant spike amplitude as their criterion. Any modulation of amplitude in phase with the respiratory cycle must be due to cell movement in relation to electrode tip position in the potential fields around active cells. Also, differences in spike amplitude can be used as a check against recording from more than one cell at the same time.

The phasing of periodic discharges is important in respiratory cell identification. Amoroso, Bainbridge, Bell, Lawn and Rosenberg (5) accepted as primary respiratory neurons only those discharges which preceded muscular electrical activity and which fired throughout the inspiratory or expiratory phase. Special care must be taken in identification when rhythmic potentials are found in the region of the solitary tract or nucleus since they may arise from vagal afferents or vagal motorneurons. The former are easily identified by their phase

spanning patterns as shown by Adrian (2), but the latter are more difficult to distinguish. Eyzaquirre and Taylor (56) showed that vagal motorneurones had discharge patterns paralleling phrenic bursts. Some had expiratory phasing patterns. In addition, von Baumgarten and Kanzow (19) described two respiratory cell types in the region of the tractus solitarius, neither of which were vagal afferents or vagal motorneurones. Both had inspiratory patterns, but lung inflation led to an inhibition of one and an excitation of the other.

When recording respiratory discharges it is important that the potentials arise from cell bodies, It is possible that ascending afferent and descending efferent traffic may carry respiratory potentials along fiber tracts which traverse medullary regions. These, of course, cannot be considered as primary respiratory potentials. Various techniques have been used to differentiate between cell body and fiber tract recordings. Due to differences in diameters, Cohen and Wang (45) suggested that cell bodies have a higher current output than single fibers. For this reason, potentials from the former have larger amplitudes (47) and longer durations (30, 79) than the latter and are found more frequently. Since the recording volume of steel microelectrodes with tip diameters

of 10-40 microns is only 5 x 10<sup>-3</sup> cubic millimeters (5), fiber potentials are more susceptible to electrode movement than cell body potentials. For example, von Baumgarten and Salmoiraghi (21) concluded that they were recording from a cell body if the microelectrode could be moved 30-100 microns without losing the potential. Haber, Kohn, Ngai, Holaday and Wang (79) could not record respiratory activity from the caudal medulla and suggested that their microelectrodes were sensitive only to cell body potentials.

Nelson (127) and Cohen and Wang (45) introduced a new criterion and claimed that sources of unit activity could be distinguished on the basis of spike polarity. Pure negative or positive-negative waves were believed to arise from cell bodies. These were the most common. Pure positive or positive-negative-positive triphasic spikes were believed to arise from axons or fiber tracts.

Cells with respiratory characteristics may not always function in the respiratory complex and are therefore probably not primary respiratory neurons. Scheibel and Scheibel (158) observed reticular cells for many hours and reported that some non-respiratory cells assumed activity characteristics resembling respiratory patterns. The authors concluded that such neurons may function in different

neural nets at different periods of time. Gesell, Bricker and Magee (70) found that respiratory discharges may differ considerably in frequency and may vanish and reappear under modifying conditions. This indicated that the reticular formation could command recruitment and adjustment of respiratory cell patterns. Cohen (38) described periodic discharges recorded in the isolated pons which resembled respiratory discharges in both burst duration and firing frequency. On close examination, however, these cells were not locked to the respiratory cycle, but tended to drift in random patterns. This demonstrated that cells in the reticular formation could exhibit similar respiratory patterns without having any known respiratory function.

Elementary descriptions of respiratory cell discharge patterns have most commonly included measurements of the number of action potentials per burst (spikes per train), the discharge duration (train length) and the average discharge frequency. It has been implied that increases in these parameters for inspiratory cells correlate with deeper respiratory movements. Pitts (141) stimulated the inspiratory region of the medulla with various intensity and frequency combinations and found increased firing frequency of single motor units and motor unit
recruitment from the subliminal fringe of the phrenic population. Adrian and Bronk (3) found a linear relationship between interpleural pressure and stimulation frequency of the phrenic from 20-50 Hz. Integrated total phrenic nerve activity has subsequently been shown to be proportional to the tidal volume (39, 50, 58). Eldridge (53) recently demonstrated that integration of the phrenic signals during the 100 milliseconds coincident with the peak of inspiration is the best neural analog of tidal volume over wide ranges of tidal volume and respiratory rate.

Nesland, Plum, Nelson and Siedler (129), studying inspiratory cell patterns, introduced the product of spikes per train times respiration rate and showed that this spike output increased proportionally with elevation in minute ventilation. For example, CO<sub>2</sub> administration in intact cats led to increases in depth and rate of respiration, increase in mean frequency discharge, and decrease in train length. Spikes per train remained constant. Parameter changes due to alteration of respiratory rate were prevented by vagotomy. In vagotomized cats, CO<sub>2</sub> administration induced pure depth changes with corresponding increases in mean frequency discharge and spikes per train. Train length did not change. It was also shown that hypoxia produced less consistent responses than CO<sub>2</sub>

administration. Hyperoxia depressed all parameters and some cells were completely inhibited. Nesland <u>et al</u>. (129) concluded, "It appears that the medullary respiratory neuron population regulates the magnitude of ventilation primarily by changes in the impulse frequency and total number of discharges of already active cells rather than by increasing or decreasing the number of cells actively discharging during each breath."

Nelson (127) recognized the importance of sampling from many respiratory cells to "resynthesize" characteristics of the whole population. Discharge parameters from inspiratory and expiratory cells were examined at different respiratory rates and the following conclusions were The train length is directly proportional to the made. respiratory cycle time. The spikes per train are proportional to the train length. The spike frequency is proportional to the spikes per train. Dirken and Woldring (51) confirmed the train length-spikes per train length relationship for expiratory cells at a constant discharge frequency. Cohen (41) confirmed the spikes per train-inspiratory phase duration relationship for inspiratory cells in lung inflation studies. Brodie (31) studied discharge patterns in inspiratory cells during modification of the spontaneous respiratory rate with drugs.

Thiopental, a respiratory depressant to both rate and amplitude, increased the spikes per train and burst duration but slightly decreased the discharge frequency. Cyanide, a respiratory stimulant, reversed all the responses. Brodie (31) concluded that respiration rate and train length were reciprocally related while respiration rate and discharge frequency were directly related.

Wang and Ngai (175) have stated that respiratory rate is probably determined by the rate of depolarization of respiratory neurons. In this case, measurements of spikes per train, train length and mean discharge frequencies fail to account for dynamic changes that take place in burst discharges during depolarization of respiratory cells. To quantitate these dynamic events, frequency modulation curves have been constructed where the instantaneous spike frequency is plotted as a function of time. Salmoiraghi and Burns (155) showed that respiratory cells fired in non-regular patterns, necessitating curve fitting for single burst discharges.

Gesell, Magee and Bricker (72) reported that inspiratory cells exhibited a slowly augmenting pattern in which the spike frequency consistently increased as the train progressed. The frequency discharge rapidly decreased just prior to the off-phase for the cell. This

frequency pattern correlated with tidal movement of air. Two expiratory patterns were described. One was a steady state discharge in which expiratory cells fired with a constant frequency throughout the whole train. The other pattern showed a rapid increase in frequency which slowly declined before the cells turned off. Similar discharge patterns were found at all points along the respiratory arc from the respiratory muscles through the central neryous system and back along sensory nerves. These parallel patterns suggested serial linking between stations of the respiratory mechanism. Gesell, Atkinson and Brown (69) restudied respiratory discharge patterns in muscleblocked dogs. No alteration in inspiratory patterns were seen, suggesting that the frequency modulation of these cells was of central origin. Expiratory cell patterns were all of the steady state type. The authors suggested that the rapidly augmenting expiratory patterns might have been due to reflex modification of the basic steady state pattern. Gesell and Worzniak (74) supported this suggestion by showing that steady state expiratory cell patterns could be converted into rapidly augmenting patterns during spontaneous respiration or into slowly augmenting patterns during pump inflation.

Dirken and Woldring (51) studied the frequency

curves of inspiratory cells, expiratory cells and vagal afferents. Decreasing lung volume by tracheal blockade in mid-inspiration caused inhibition of vagal afferent frequency discharge and drop in the respiratory rate. The time course of frequency modulation in inspiratory cells was unaltered except for the duration of inspiration, which was increased. Vagal blockade by anelectrotonus, however, depressed the initial rate of change in frequency in the same cells. Assuming that rate of frequency change depends on the rate of depolarization in respiratory cells, a depression in the latter can be associated with low respiratory rates after vagotomy.

Hukuhara, Nakayama and Okada (91) described frequency modulation patterns of inspiratory and expiratory cells in cats and dogs. The basic patterns observed agreed with those of Gesell <u>et al</u>. (72) and up to four variations were noted for both cell types. Variations ranged from slowly and rapidly augmenting discharges to steady state patterns. The authors attributed variations in starting time, spike frequency and number of spikes per train to differences in thresholds throughout both inspiratory and expiratory populations.

Von Baumgarten, Balthasar and Koepchen (18) and Salmoiraghi and von Baumgarten (154) studied intracellular

discharge patterns from inspiratory and expiratory neu-Burst discharges were initiated by a spontaneous rons. depolarization of the resting membrane potential which continued to depolarize slowly until the burst was terminated. Inspiratory cells showed a frequency increase paralleling the degree of membrane depolarization. The authors suggested that the high depolarization level at the end of each spike train reflected a maximum threshold, above which the cells could not generate additional action potentials. This self-limiting theory quickly replaced the suggestion of Burns (35) that spike discharges terminated because of fatigue. Batsel (15) argued against the latter view by pointing out that respiratory cells could be driven at higher than normal rates for long periods of time without any sign of fatigue. Also, Robson, Houseley and Solis-Quiroga (148) showed that respiratory cells could fire continuously after barbiturate administration.

Salmoiraghi (153) proposed a theory for rhythmicity of breathing based on three excitatory mechanisms: (1) increased firing frequency of inspiratory cells, as the cycle progressed, depended on self-reexciting mechanisms within the inspiratory population; (2) concurrent decreased probability of expiratory cell firing was attributed

to reciprocal inhibition; (3) increased firing thresholds of inspiratory neurons explained transition from inspiration to expiration. This cyclic exchange between inspiratory and expiratory populations was expected to continue as long as the three postulated mechanisms were intact.

Although Waldron (174) has reported that distinct categories of activity patterns could not be distinguished within the inspiratory group, other investigators have described many respiratory cell subtypes. Cells have been classified into no less than eight categories based on phasing pattern differences with the respiratory cycle (14, 15, 40, 41, 42, 45, 128, 169, 173). It is interesting that cells do not change their phasing during CO2 administration, lung inflation or other procedures. Most workers, led by Cohen (43), have assumed that these different respiratory cell patterns reflected differences in function. Elaborate theories on the genesis of respiratory rhythm have subsequently been devised. Batsel (15) concluded that the bulbar respiratory center may exhibit rhythmicity due to the differences in onset time of discharges of the various early inspiratory cells. Temporal overlapping of different subgroups was believed to smooth the transition between respiratory phases.

Nesland and Plum (128) suggested that any hypothesis

on respiratory oscillation derived from the interrelationships among functionally different subgroups within the medullary inspiratory and expiratory populations required three assumptions. First, one active subgroup must activate another quiescent subgroup. Second, one active subgroup must inhibit another active subgroup. Third, activity must be found within at least one subgroup at any point in time. Cohen (42) used these criteria and proposed a model for genesis of respiratory rhythmicity based on respiratory cell subtype response to CO2, lung inflation and brainstem electrical stimulation. The schema was constructed around a master oscillatory loop which paralleled the inspiratory and expiratory neurons of Salmoiraghi and Burns (36, 155, 156). Three other loops had direct influence on the master loop. One, consisting of expiratory-inspiratory neurons, initiated inspiration. The other two loops inhibited inspiration and expiration respectively. Inspiratory units activated by lung inflation might function in the inspiratory inhibitory loop, but oscillation did not depend on vagal innervation.

### CHAPTER III

#### METHODS

## A. Surgical Preparation

Mongrel cats anesthetized intraperitoneally with 30 mg/Kg sodium pentobarbital (Nembutal, Abbott Laboratories) were used exclusively in this study. The cats had a mean weight of 2.7 Kg (range 1.6 to 4.9 Kg) and there was no sex discrimination. Cats were placed on a Gorman-Rupp Industries, Inc., Model Mll warm water circulated pad which was driven by a Model K-1-3 water heaterpump. Rectal temperatures, which were monitored with a Yellow Springs Instrument Company, Inc., Model 46 TUC Tele-thermometer, were maintained at  $37 \pm 2^{\circ}$ C. Surgical preparations and instrument calibrations were usually completed within 2 hours. Most cats remained remarkably stable for more than 8 hours and breathed spontaneously throughout the duration of the experiment.

Four surgical incisions were made. First, the femoral triangle was exposed to permit catheterization of the femoral artery and vein with PE100 polyethelene tubing. Catheter tips were advanced to the abdominal aorta for blood pressure recording and inferior vena cava for drug injections, respectively.

Second, a four or five centimeter midline incision was made through the ventral cervical neck skin and sternomastoid muscle. Reflection of the sternohyoid muscle exposed the trachea for intubation with a quarter-inch polypropylene (Nalgene) Y-tube. The cervical vagosympathetic nerves were isolated and loosely ligatured with umbilical tape. In some experiments loose triple zero silk ligatures were placed around each cervical carotid artery for bilateral carotid occlusions or tugs.

Third, after mounting the cat in David Kopf 1530 Stereotaxic Frame Assembly, a small incision was made through the skin of the left lateral thoracic cage and the pectoralis minor muscle was separated by blunt dissection. A transthoracic needle was inserted through the serratus ventralis and internal intercostal muscles at the fourth or fifth rib interspace. This probe was used for intrapleural pressure recording.

The last surgical procedure involved exposure of medullary brainstem structures. A dorsal midline incision was made through the skin of the head extending three to

four centimeters rostal and caudal to the occipital crest. The lambdoidal ridge was exposed by separation of the cut skin interfaces with retractors. A National cautery was used to separate neck muscles (clavotrapezius, levator auris longus, epicranius occipitalis, auricularis superior, abductor auris longus, abductor auris brevis and temporalis muscles). Some muscles were removed and other were retracted until the caudal interparietal and occipital bone surfaces were laid bare. The exposed dura mater between the occipital bone and the atlas vertebra was ruptured resulting in a free flow of cerebral spinal fluid. Portions of the occipital bone were removed with Rongeur forceps carefully inserted above but never touching the dorsal surface of the medulla. Medullary brainstem structures from the first cervical nerve to the cerebellar border were exposed. The posterior lobes of the cerebellum were also uncovered for suction removal of the whole cerebellum if necessary. In most experiments, however, the entire cerebellum was left intact. Frequent application of 0.9% saline solution prevented the brain tissue from drying out. In some cases, the spontaneous flow of cerebrospinal fluid provided satisfactory irrigation of the fourth ventricle.

# Data Acquisition

The interconnections of the electronic equipment used to monitor and store on-line analog data are presented schematically in Figure 1. A Grass Model 7 Polygraph strip chart recorder was used to record four physiiological parameters. In the first channel, airflow velocity was measured with a Fleisch pneumotachograph connected in series with one arm of the trachael Y-cannula. The opposite arm was blocked with U-screw clamp occlusion of a rubber tube extension. During movement of air through the pneumotachograph the small pressure gradient produced across a metal honeycomb grid was detected by a Grass Model PT5A differential volumetric pressure transducer. The device was calibrated and found to be linear with airflow velocities up to 110 cc/second in accordance with Poiseuille's Law. This was the upper limit for airflows in most experimental cases.

Intrapleural pressure was monitored on the second polygraph channel. A 15 gauge needle beveled at the tip with sideports along its shaft was inserted across the lateral thoracic wall at the fourth or fifth rib interspace. An elliptical copper plate attached to the needle shaft at a 45° angle limited the probe's insertion distance to 2.5 centimeters. Skin flaps were pulled



Figure 1. Instrumental schematic: A. polygraph; B. microelectrodes; C. preamplifier; D. 60 Hz filter; E. oscilloscope; F. audioamplifier; G. tape recorder; H. switching network; I. current amplifier.

together over this plate to seal any air leaks and maintain the needle in an approximate parallel apposition with the lung. Air pressure fluctuations were recorded with a Statham P23Dc pressure transducer which was initially calibrated with a water manometer.

The third polygraph channel monitored the end expiratory  $\[mathbb{S}\] CO_2$ . A short length of tygon tubing was attached to the exit port of the pneumotachograph to support a PE260 CO<sub>2</sub> sampling catheter in the center of the airflow profile. A Beckman microcatheter sample pump continuously drew a small fraction of the expired air through the detector head of a Beckman LB-1 Medical Gas Analyzer. Using an infrared absorption technique, a voltage signal related to the  $\[mathbb{S}\]$  CO<sub>2</sub> of the sample was obtained. This curvilinear signal was processed with a Beckman linearizer before going to the polygraph. At the beginning of each experiment the CO<sub>2</sub> channel was calibrated with a CO<sub>2</sub> reference gas (Matheson Gas Products). The linearizer was periodically adjusted for linearity.

Finally, the blood pressure was recorded on the fourth polygraph channel. A Statham PE23Gb pressure transducer attached to an intra-aortic PE100 catheter filled with 0.9% non-heprinized saline was used for this measurement. The catheter was kept clot-free by frequent

flushings with saline. The blood pressure transducer was initially calibrated with a mercury manometer.

The last physiologic parameter examined in this study was the extracellular electrical activity of single respiratory neurons in the medulla. As shown in Figure 1, potentials were recorded with microelectrodes, AC amplified (2 channel capacity) and filtered. In early experiments, glass micropipettes filled with 3 molar sodium chloride solution were used. With the exception of one cell, however, all single cell potentials analyzed in this study were recorded with Green's (78) metal microelectrodes. Steel insect pins were etched to fine tip diameters in 12 molar hydrochloric acid using a 6.3 volt A.C. source. The electrodes were insulated with clear Insl-X E33 solution and baked in an oven overnight. Tip dimensions were measured with a Carl Zeiss microscope (X10) and Vickers A.E.I. image splitting eyepiece (X10) and ranged from 1-5 microns. Corresponding electrical impedances, checked on a General Radio Company Type 1650-A impedance bridge, ranged from 80-5 megohms respectively.

Microelectrodes were mounted on a Kopf 1460 electrode carrier fitted with a Kopf 1206 reduction drive and were slowly advanced through medullary brain tissue in 10 micron steps. No attempt was made to cut away the pia

Single cell potentials picked up by the microelecmater. trodes were in the 200-800 microvolt range. These potentials were amplified about 2000 times with a Grass DP9B dual channel AC preamplifier (single-ended input, cathode follower mode). The signal-to-noise ratio was maximized by keeping input leads short, use of shielding, establishment of common grounds between the amplifier and cat, and signal filtering. The low and high half amplitude frequency filters on the amplifier were set at 0.1 and 40 K Hz respectively. A 60 Hz notch filter, shown in Figure 2A, was constructed to eliminate line noise. The frequency response curve of this filter, which is plotted on a log scale in Figure 2B, shows maximum attenuation at 60 Hz. Experimental tests demonstrated that peak-to-peak voltages of single respiratory spike potentials were not attenuated by filtering. Filtered waveforms were more biphasic than nonfiltered signals and the former displayed a small leading phase shift (less than 0.2 millisecond). Neither of these changes affected the validity of data collection or spike train analysis used in this study.

Amplified and filtered single cell discharges were monitored on-line. Potentials were displayed on a Tetronix type 502A dual-beam oscilloscope and were audio-amplified on a Grass AM7 audio-monitor as shown in Figure 1. Both



Figure 2. Parallel T notch filter: A. schematic diagram; B. frequency response curve.

of these instruments played important roles in the positive identification of single respiratory cell discharges.

Whenever a single respiratory cell potential of good amplitude was found, on line data from both this cell and from the polygraph were stored on a seven channel philips ANA-LOG 7 tape recorder as shown in Figure 1. The tape recorder was operated at 3-3/4 inches per second in the FM mode. During a recording procedure, single cell data were immediately played back to the oscilloscope and audio-monitor to determine the quality of the recorded signal. A switching network permitted various combinations of data review when recordings from two different cells were obtained at the same time.

Finally, a current amplifier was constructed which sensed current flow in the "record light" logic circuit of the tape recorder. Whenever the recorder was storing analog data, this device closed a relay which caused a downward identification mark to be placed on the polygraph strip chart. An upward deflection on the polygraph event marker channel was activated by a remote foot switch to identify experimental manipulations. Other features including voice description on the tape (channel 8) and digital tape counter were also useful in locating single cell discharges during data analysis.

## Experimental Manipulations

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After a cat was surgically prepared and all polygraph channels were calibrated, a microelectrode search for respiratory potentials was started. Strict stereotaxic coordinates were not used, but by following the map of Salmoiraghi and Burns (155) with the obex as a reference point, respiratory cells could be found. Care was taken in the identification of cells as primary respiratory neurons. Many types of potential discharges were found in the medulla, but only those showing an on-off firing pattern in phase with the respiratory cycle (airflow, intrapleural pressure and % CO, oscillations) were considered as primary respiratory cell candidates. Some of these potentials were rejected for various reasons. Potentials whose amplitude fluctuated as a function of the respiratory cycle were eliminated because of the possibility that they were generated by movement artifacts. Potentials with uniform spike height showing highly irregular or high frequency discharges (instantaneous frequencies over 200 Hz) were rejected since more than one cell was probably present. Finally, potentials showing phase-spanning patterns were rejected since they may have been vagal afferent in origin. Only those potentials of constant amplitude exhibiting pure inspiratory or pure expiratory phasings were recorded

as primary respiratory neurons. These potentials were believed to be derived from cell bodies since no respiratory discharges could be found from the lower medulla to the upper cord where respiratory efferents are known to pass.

When a respiratory cell was found and positively identified, a control record was stored on magnetic tape. Various manipulations of the respiratory system were then performed to induce alterations in the discharge pattern. In general, procedures were used which evoked changes in respiratory rate and depth. Single cell data were obtained in both vagi-intact and vagotomized preparations.

Increases in respiratory rate were induced by intravenous injection of doxapram hydrochloride (Dopram, A.H. Robins Company). Respiratory rate was readily depressed by sodium pentobarbital or sodium pentothal (Pentothal, Abbott Laboratories). In a few cases, high respiratory rates arose spontaneously during exposure of the medulla. This acceleration was probably due to warming of brainstem structures. Other procedures, including CO<sub>2</sub> administration, anterior hypothalamic heating and intravenous injections of morphine sulfate (U.S.P.) were tried in several cats, but associated rate changes, if any, were not consistent.

Respiration depth was increased by increasing airflow

resistance. For this procedure, the cross-sectional area of the pneumotachograph exit port was decreased by known fractions with calibrated resistance plugs. It was very difficult to retain single unit recordings during induced depth changes. Either the cell would be lost because of movement problems or other cells would be recruited, thus masking the original discharge. For this reason, data obtained with airflow resistance plugs will not be presented.

Finally, other studies were designed to examine the correlation between apneustic breaths and barbiturate level in the spontaneously breathing cat. This phenomenon was studied at the single cell level and apneustic thresholds were evaluated by cerebellectomy and bilateral carotid occlusion. Data obtained from this work was important for the interpretation of single cell discharge pattern changes during barbiturate titration.

#### CHAPTER IV

#### DATA ANALYSIS

## A. PDP-12 Overview

The general objective of this study was to investigate interspike interval distribution and sequencing of single respiratory cell discharges at various steady state breathing frequencies and depths. A Digital Equipment Corporation PDP-12 (Programmed Data Processor-12) general purpose laboratory computer was programmed to process offline analog tape data of single cell activity. For each steady state observation, thousands of interspike intervals were examined and manipulated to construct histogram and interspike interval modulation curves. The latter involved a new mathematical technique devised by the author to quantitate ordering of interspike intervals during burst discharges. In addition to powerful software capabilities, a full array of PDP-12 output options was available to the user: CRT display; LA-30 Decwriter (Digital Equipment Corporation) hard copy printing; DP-1 Complot

(Houston Instrument, Baush and Lomb) digital increment plotting; LINC magnetic tape storage.

Communication with the PDP-12 computer was accomplished with essentially three programming languages. The first two are machine language in format and actually represent the two mode operation capacity of the PDP-12. The first or LINC-8 (Laboratory INstrument Computer) mode activates peripherals including analog to digital conversion, sense switch lines, relay buffers, CRT display and auxiliary LINC tape storage. The second or PDP-8 mode provides for extended arithmetic element (EAE) operations, real-time clock programming, digital incremental plotting and Decwriter input-output. While each mode has its own complete instruction set, both modes are given equal status by the single central processor. This permits rapid switching between modes under program control. Also, the 1.6 micro-second memory access time of the PDP-12 permits fast execution of individual instructions. This speed is advantageous for rapid analog to digital conversions.

FOCAL (Formulating On-line Calculations in Algebraic Language) was the third programming language used. This is a conversational language that permits on-line user-machine interaction and resembles FORTRAN IV (FORmula TRANslation version IV) in power for calculation of complex

mathematical expressions. Two FOCAL systems, FOCAL-12 and FOCALPL (plot), were utilized respectively to retrieve and manipulate data stored on magnetic tape from machine language programs and to graphically plot calculated parameters located on digital tape.

Two major disadvantages are associated with FOCAL. First, FOCAL programs are limited in length since the FOCAL interpreter, a machine language program itself, takes up a large portion of the PDP-12 8K core memory. Second, execution of individual FOCAL program instructions is slow since each mnemonic code command must be interpreted into machine language binary each time it is performed. Under the conditions of this study, these disadvantages were by no means limiting.

## B. Machine Language Programs

## 1. ERASE

For convenience and speed of data handling, data were stored on LINC magnetic tape of standard format. Each tape was marked off into  $1000_8$  ( $512_{10}$ ) blocks, each block containing  $400_8$  ( $256_{10}$ ) 12-bit words. Prior to data storage, program ERASE was run to store a zero in each of the  $131,072_{10}$  ( $512_{10} \times 256_{10}$ ) 12-bit words. By this procedure, new and old tapes could be cleared of all digital values before proceeding with other programs. Program ERASE along

with the programs discussed below are listed in the Appendix for reference.

2. DATA

Program DATA was written in machine language making free use of both LINC and PDP-8 modes. As outlined in the Appendix (Table VII), program instructions were located in the lower 4K memory of the PDP-12 and data were stored in the upper 4K memory. An abbreviated logic flow diagram of the program instructions is presented in Figure 3. The logic is represented by three major loops (A,B,C) and calculation (CALC) procedures between loops B and C. To facilitate understanding of data handling by program DATA, each of these four program sections will be discussed in relation to a real physiological input signal. The reader should be able to trace data processing of the analog respiratory cell discharge input to the final digitalized output before proceeding to higher levels of data analysis.

Inspiratory and expiratory cell discharges were examined in this study, and two representative cells are shown in Figure 4A and 4B respectively (35 mm records from a Grass Kymograph Model C4N Camera). Both cells were obtained from different cats, each of which was breathing at a rate of 30 breaths per minute. It can be seen that the inspiratory cell is in phase with the fall in the intrapleural pressure



Figure 3. Program DATA flow chart. See text for details.



A

Figure 4. Representative examples of single cell analog data: A. inspiratory cell; B. expiratory cell. Lower tracing in each panel is intrapleural pressure (IPP).

while the expiratory cell is 180° out of phase. The inspiratory signal C29UI7R(2) of Figure 4A will be processed step by step in the discussion that follows.

The analog respiratory discharge was played back to the PDP-12 computer four times slower than record speed. In loop A of program DATA (Figure 3) the signal was digitalized and displayed on the CRT for assessment of signal quality. The sample rate was determined by the clock logic which halted program flow until a predetermined amount of time had elapsed. The KW12 real time clock, a crystalcontrolled pulse generator oscillating at 400K Hz, was programmed to give a basic clock overflow count rate of 0.4 millisecond. This rate, coupled with the fourfold slow-down of the tape transport, established a simulated sampling rate of 0.1 millisecond per sample or 10 samples per millisecond.

Loop A was programmed to sample and store  $1000_8$  points before displaying the stored data on the CRT. The display therefore corresponded to a 51.2 millisecond segment  $(1000_8 \text{ samples x } (512_{10}/1000_8) \times 0.1 \text{ msec/sample})$  of the respiratory cell discharge. The memory was constantly updated causing the CRT to flash at about 5 Hz ([0.0512 sec x 4]<sup>-1</sup>) although any segment could be frozen on the CRT for close analysis via sense switch control. After a signal

was judged to be satisfactory for computer analysis, exit from loop A was manually controlled under sense switch selection. Between loops A and B, the upper 4K of core memory was cleared along with various constants. Certain addresses were also reset to appropriate values.

The overall responsibility of loop B was to construct histogram and interspike interval modulation curves from the analog signal. The logic centered around detection of action potentials, measurement of interspike interval times and proper memory storage of interval times in various combinations for histogram and interval sequence analysis.

The PDP-12 computer is equipped with a Schmitt trigger. This device senses potentials whose amplitude exceed a manually set threshold and hence would appear ideal for action potential detection. The Schmitt trigger, however, has several disadvantages when used to detect the action potentials recorded in this study. For this reason a software rate-of-rise trigger was designed which proved highly reliable in action potential identification. The rate-ofrise trigger diagrammed in Figure 5 operated as follows. Analog sampling in loop B occurred at a constant simulated rate of 0.1 millisecond per sample as determined by the clock logic (CL). At this rate, action potentials



Figure 5. Technique for detection of action potentials. Dots represent digitalized 0.1 msec samples of analog signal. The change in voltage  $(\Delta S=S2-S1)$  per unit time represents a signal exceeding the trigger (TRG) level ( $\Delta S>TRG$ ). This identifies an action potential (A or B) and inactivates the trigger logic for the next 2 msec.

1 millisecond in duration could be sampled 10 times. Since the sample rate was constant, the vertical distance between samples was proportional to the rate of potential change. Therefore, by testing for vertical separation between successive samples, action potentials could easily be detected even when the signal to noise ratio was as low as 2:1 and when slow baseline shifts were present. The trigger level (TRG) was manually adjusted until a "T" flashed on the CRT in synchrony with the audio amplified action potentials. The trigger operated only on the rising phase of action potentials. After a trigger occurred, 2 milliseconds elapsed before the trigger was "activated" again. This eliminated the possibility of generating two trigger pulses from a single biphasic action potential.

Interspike interval times were calculated to the nearest 0.1 millisecond by counting the elapsed time between action potential triggers. In short, a trigger caused the accumulated time of the previous interval to be stored with subsequent resetting of the interval counter. In Figure 5, for example, action potential A resets the counter to 0.0 milliseconds. Detection of action potential B 5.0 milliseconds later terminates the accumulation of interval time. The A-B interspike interval is stored as 5.0 milliseconds and the counter is reset for the next interval.

Histogram analysis has been a popular approach to quantitation of electrophysiological data from single neurons (66, 67). In this study, a 100 millisecond interval histogram was constructed by accumulating 500-4000 intervals, the number under manual selection. The histogram had 125 bins each of 0.8 millisecond width. The histogram plot for inspiratory cell C29UI7R(2) is presented in Figure 6A in which the terminal 30 milliseconds have been deleted. In Figure 6B the same data are plotted on an expanded scale. As consistent with all units studied, the distribution of interspike intervals for this cell shows unimodal peaking and is skewed to the right, favoring longer intervals. Parrot and Fleming (139) attempted to associate this characteristic shape of the respiratory interspike interval histogram with random Poisson processes. Although this has been done for non-respiratory discharges of truly random patterns (68, 106, 165), it is difficult to assign such random mechanisms to respiratory cells which possess predictable discharges. Against the random approach, Marczynski and Sherry (119) suggested that time-locked patterns which repeat over and over again with a sequential arrangement of adjacent intervals can best be described by the autocorrelation function. High correlations for respiratory cells (R.A. Mitchell - unpublished



Figure 6. A. Interspike interval histogram derived from inspiratory cell C29UI7R(2) in Figure 4A. B. Same histogram on an expanded time scale showing mean (MEN), median (MED), mode (MOD) and number of intervals at the mode (MON). The histogram is made up of 2000 intervals.

observations) are certainly not indicative of random ordering of intervals. The interdependence series matrix method introduced by Sherry, Marczynski and Wolf (163) may also be useful in establishing a relationship between a specific interval and an interval removed by a fixed number of other intervals for respiratory train analysis.

A cumulative histogram or ogive curve is plotted in Figure 7 for inspiratory cell C29UI7R(2). The plot is linear on a log scale indicative of exponential processes operating in interval distribution. Similar plots are found for both Poisson and normal distribution functions. A horizontal line has been drawn at the 50% level and a vertical line intercepting the curve at this same level has been extended to the time scale. By definition, the interpolated time of 14.8 milliseconds corresponds to the median interval time. From Figure 6B, it can be seen that the median time is longer than the mode time. Also, the mean interval time is longer than median time. These relationships establish the skewing characteristics of the interspike interval histogram to the right.

For discharges that have random arrangement of intervals, quantification of cell output is satisfactorily completed by histogram analysis and measurement of standard



Figure 7. Ogive curve derived from histogram in Figure 6. Median (MED) interval time interpolated from 50% level.

statistical parameters such as the mean, median, mode and standard deviation (119). As reviewed in the Literature, however, respiratory discharges undergo characteristic frequency increase, plateauing and frequency decrease during their "on" phase. For this reason, accessment of respiratory cell output must involve description of sequential interval ordering, information that cannot be extracted from histogram interval distributions. Cohen (40) and Bertrand and Hugelin (24) approached this problem by using phase-triggered time histograms and cycletriggered spike-density histograms for analysis of respiratory discharges, respectively. Although qualitative accessment was achieved, these methods failed to quantitate dynamic changes in the interspike interval during respiratory cell discharge.

To study dynamic changes in the interspike interval during respiratory burst activity, a new statistical averaging technique was devised as diagrammed in Figure 8 with hypothetical data. Intervals were numbered consecutively (Figure 8A) and corresponding intervals were averaged to construct an idealized respiratory train (Figure 8B). Plotting the sequential interspike intervals of the idealized train as a function of time resulted in a smooth "U"-shaped interspike interval modulation curve (Figure 8C).


Figure 8. Generation of idealized interspike interval modulation curve from raw data: A. analog data; B. interval averaging; C. graphic display of averaged intervals. See text for details.

In Figure 9, similar plots for cell C29UI7R(2) are presented. For a single burst discharge (NT=1) a very rough curve was described reflecting non-smooth transition between consecutive interspike intervals as the train progressed (Figure 9A). An average of 44 sequential burst discharges (NT=44) eliminated the variability between adjacent intervals and resulted in a smooth interspike interval modulation curve (Figure 9B), readily accessible for mathematical analysis. This mathematical method differed from standard signal averaging techniques (164) which depend on external time references to recover repetitive waveforms from random noise. The analysis worked for both inspiratory and expiratory discharges (Figure 4) and was independent of cycle cues from peripheral respiratory parameters.

The computer techniques employed to generate interspike interval modulation curves can best be understood by paralleling the "S" (start of train), "T" (trigger on successive action potentials) and "R" (reset) designations over the action potentials in Figure 8A with the display "S", display "T" and display "R" commands of loop B in Figure 3. For example, loop B logic was manually entered from either loop A or loop C during the quiescent period of the respiratory discharge (interburst interval). This



Figure 9. Interspike interval modulation curves derived from inspiratory cell C29UI7R(2) in Figure 4A: A. single train; B. average of 44 trains. Derivation of parameters shown in B are described in text, pages 99-106.

caused an "R" to be flashed on the CRT indicating that appropriate addresses had been reset. Program flow was then delayed in the first trigger loop (TLl) until the first action potential was detected. At this time, an "S" was flashed on the CRT and program flow was then delayed in the second trigger loop (TL2). Starting with the second action potential, all the remaining action potentials in the train caused a "T" to be displayed on the In conjunction with the clock logic (CL), each of CRT. these successive action potentials defined an interspike interval which was stored in an incremental address. Thus, consecutive intervals were stored in consecutive addresses. When a predetermined amount of time (maximum of 4095 msec scaled time) elapsed without any action potentials being detected, it was assumed that the train discharge was terminated for that breath and reset procedures were automatically initiated as revealed by CRT display of the "R". The sequence started all over again when the first action potential (display "S") of the next burst discharge was detected.

By this iterative technique, the PDP-12 memory accumulated the sum of the first intervals, the sum of the second intervals and so forth. To handle large sums, double precision arithmetic was used. That is, two 12-bit registers were daisy-chained together to form a 24-bit register

(maximum value accepted =  $2^{23} = 8,388,608$ ). The idealized train was recovered after exit from loop B by dividing each accumulated interval sum by the number of intervals that contributed to that sum. Since the divisor N was variable, the analysis was not limited by the shortest train, a problem described by other workers (24, 40). However, commencing with the first interval after the shortest train and continuing until the last interval of the longest train, the divisor N decreased as fewer and fewer trains contributed to the idealized interspike interval average (Figure 8B). For this reason, a breakdown in the statistical averaging and hence poor curve smoothing was observed towards the end of the train (Figure 9B).

In addition to histogram and interspike interval modulation curve genesis, loop B also stored consecutive cycle times and first interval times during the complete analysis. Cycle time (CT) was defined as the time between first action potentials of consecutive burst discharges. The first interval (FI) was defined as the time between the first two action potentials of each train. This parameter is circled in Figure 9B at the beginning of the train.

Exit from loop B was under both manual and automatic control. During trial runs, output procedures could be initiated by sense switch selection. Also, if more than 510

burst discharges were accumulated, automatic transfer to loop C was performed. For final runs, however, exit from loop B occurred after the histogram N had been filled. If the histogram was filled during the middle of a burst discharge, intervals were still calculated to complete the interspike interval modulation curve for that burst, but the intervals were deleted from histogram construction. Exit proceeded with the first action potential of the very next train (Figure 8A). This permitted accurate measurement of the last cycle time.

Between loops B and C, a series of calculation (CALC) steps were performed (Figure 3). As already discussed, mean interspike intervals were recovered to generate the idealized train. Individual instantaneous respiratory rates were calculated from the reciprocal of each cycle time measurement and these rates were averaged to give a mean respiratory rate (RR) for the analysis period. Mean rates calculated in this manner were slightly higher than averages taken by dividing the number of respiratory cycles observed by the total analysis period. This was due to the hyperbolic relationship between the period and the reciprocal of the period. High and low rates were isolated to reveal the degree of steady-stateness of instantaneous frequencies.

The number of intervals in each train were calculated and the mean spikes per train (ST) were found by adding one to the mean number of intervals per train. By examination of each idealized interval, the minimum interval (MI) in the respiratory train was localized by a search technique. The minimum interval (MI) is circled in Figure 9B. Also, the mean (MEN) interval time was calculated from the idealized train taking into account the variable divisor N, for each interval. The mode (MOD) and median (MED) interval times were extracted from the histogram data and the number of intervals in the bin at the mode (MON) was found. The mean (MEN), median (MED), mode (MOD) and number of intervals at the mode (MON) are diagrammed in the histogram data of cell C29UI7R(2) in Figure 6B.

Finally, the following eleven values were stored in a specific portion of core memory to facilitate transfer to LINC magnetic tape: mean respiration rate (RR), number of trains averaged (NT), spikes per train (ST), first interval time (FI), minimum interval time (MI), number of intervals in the interspike interval modulation curve (FMN), number of intervals in the histogram (HSN), mean (MEN), median (MED) and mode (MOD) interval times, and number of intervals at the mode (MON).

After completion of the calculation procedures,

program flow proceeded to loop C instructions. Loop C (Figure 3) was an output loop responsible for retrieving calculated data. The CRT was used to continuously display the histogram or interspike interval modulation curve (sense switch selection) along with axes and appropriate scaling integers. Titles could be placed on the CRT from the Decwriter keyboard for photographic purposes.

Selection of sense switch W (write) caused the Decwriter to print a hard copy list of digitilized values stored in core memory. Table I is the output from cell C29UI7R(2). In A, the mean, high and low respiration rates (breaths/10 minutes) and instantaneous rates for each breath are given. The number of breaths averaged (N=NT) was 44. In B, the mean spikes per train and the number of intervals for each individual train are given. Concerning the latter, one train was 37 intervals long, six trains were 43 intervals long, five trains were 48 intervals long, etc. The N is repeated as an internal program check. In C, the individual first interval times for each breath are printed to nearest 0.1 millisecond and in D, the digitilized values for the idealized interspike interval curve are listed to nearest 0.1 millisecond in sequential order (e.g. first interval, second interval, etc.). An average of data in C equals the first value in D. Also in D, the mean (MEN),

Table	I.	Prog: spira	ram I atory	DATA v cel	compu 1 C29	ter p UI7R	orint (2) in	out đ n Fig	erive ure 4	ed fro 4A.	om in-
	C29UI7R(2)										
А	RRA	TE. N a	301	H 0317	L 028	37 N	8844				
	0295 0294 0297 0292 0288	0304 0304 0306 0291 0294	0298 0317 0312 0298 0301	0300 0309 0300 0312 0307	0266 0304 0294 0310	0304 0304 0292 0389	0303 0287 0314 0303	0301 0306 0310 0301	0303 0303 0297 0298	0301 0315 0318 0303	
В	TRAI	45 INT	57	0467	N 0044				- -		. <b>.</b>
	0001	003	7		. •.						
	0001	993 993	:9								
	_0002     0002		.ย .1	····-					· · · · · · ·	•	
	8001	004	2								
	0996	884	3								n
	0003	004	4								
	6993	004	5								
•	_ 8666 _ 8667	. 004 664	5		••••••••••••••••••••••••••••••••••••••		• · • ·				
	0005	004	8								
	0083	994	9								
	8002	005	Ð						•		
	0002	005	1								
	_8882_ 	. 885	2				• · · · · · •				
С	FIRST	ІНТ	·					·			
	0607	0506	0496	0414	0524	0482	0581	0574	0598	0661	
	0615 B645	0028 8519	0031	0479	8424	8789	8529	8578	0637 0606	8615	
	0507	0515	9611	0103	0423	9032 8127	8562	0014 0487	0505	0512 0548	
	0791	0459	0505	8657		·	0002	0.01	0000	00+0	·
D	M INT	ERVALS	MEN	9188	MI 012	9 N 2	911				
	0561	0419	0381	0354	0319	0280	8255	0239	R229	a231	• • •
	0221	0198	8197	0190	0181	0183	0169	0155	0162	0148	
	8145	0140	0140	0140	0129	8129	0123	0131	0127	0136	
	0120	8123	0126 0151	0123	0121	0129	0127	•0129	0137	0131	
	0155 8254	0141 8389	0104	0149 0147	0167	0185	8155	0186	0197	8168	
	_0204 _	0305	0134	0143	0211						• •••
E	ISIH	MOD 0:	132 N	ON 015	1 HED	0148	N 280	0			
	0999	5999	0001	0004	0001	0006	9993	8884	8911	0014	
	9953	8851	0086	0112	0140	0131	0161	0147	0117	0098	
	0076 8827	0007	8015	8854 8831	99977 99977	0045	0046	0338	8835	0039	
	0023	0019 0017	8813	0021 8818	ยย่ะเ คลลว	9893 9893	0017 8387	8895 9815	0012	001 <b>1</b> 0009	
	0005	0003	0013	9998	8884	00000	0007	0000	0007 8887	000 <del>3</del> 0802	
	0001	0002	0003	0005	0003	8863	0001	0002	0000	0003	
	0002	0901	0002	0000	0002	0005	0005	0000	9995	8801	
	0002	0001	9995	0001	9999	9999	8998	9991	0081	0000	
	0000 0004	8999	0000	0000	9001 0000	0000	0000	0000	0000	8888	
	99991 99991	8999 8999	<i>0000</i>	0000 0000	8889 8889	99999 99999	00000 0000	89998	8888	8999	
	<b>80</b> 00	00000	0000	0000	0000	0000	0000	0000	0000	0000	

minimum interval (MI) and number of intervals contributing to interspike interval modulation curve (N=FMN) are retrieved. Finally, in E, the contents of each of the 125 - 0.8 millisecond bins of the histogram are printed. The mode (MOD), number of intervals at the mode (MON), median (MED) and number of intervals in the histogram (N=HSN) are also given. It can be seen that the 17th bin contains the largest number of counts (MON=161). This by definition is the mode (e.g. 17 bins x 0.8 msec per bin = 13.6 msec or to place the peak at center of 0.8 msec bin, MOD = 13.6 msec - 0.4 msec = 13.2 msec). The reader should be able to correlate the digitalized values of Table 1-D with Figure 9B and Table 1-E with Figure 6.

Selection of sense switch P (plot) caused the Calcomp X-Y digital plotter to plot the histogram and interspike interval modulation data on paper from Table 1-E and 1-D data, respectively. These plots along with axes and scalings were identical to the CRT displays of the same data. Figures 6 and 9 are computer plots for cell C29UI7R(2) obtained from this output procedure.

Finally, selection of sense switch A (address) transfered data in core memory to a specified address of the LINC magnetic tape. Included in this transfer were the individual number of intervals per train and individual first

intervals, histogram and interspike interval modulation data, and the eleven constants mentioned previously (RR, NT, ST, FI, MI, FMN, HSN, MEN, MED, MOD, MON). A CRT display of "F" indicated that the tape contents at the selected address were full. This prohibited overwriting of stored data by mistake, although contents could be replaced if so desired. The tape-stored data were accessed via FOCAL programs for advanced mathematical analysis. In addition, other machine language programs could be run to replot histogram and interspike interval modulation data from the magnetic tape.

Exit from loop C (sense switch control) cleared the core memory and initiated loop B procedures (Figure 3). To examine the single cell input signal it was necessary to manually halt program flow and restart the program at \*20. 3. REPLT

Program REPLT permitted replotting of either 100 or 50 millisecond histogram and interspike interval modulation data from the LINC magnetic tape. Data from several steady state observations on the same cell or different cells could be superimposed for visual comparison. Since this program was a modification of the plot routine in program DATA, it is not listed in the Appendix.

#### FOCAL-12 Programs

## 1. \$CALC1

с.

Data stored on the LINC magnetic tape were accessed, manipulated and restored in columnar arrangement by this first calculation program. The following new eleven parameters were derived and added to the list of eleven parameters previously calculated by program DATA. The data from cell C29UI7R(2) found in Table I are used for all examples, which can be substantiated via hand calculations. This program along with all other FOCAL-12 programs are listed in the Appendix.

The train length (TL) was determined to the nearest millisecond by summing consecutive intervals of the idealized interspike interval modulation curve data until the mean number of intervals per train was reached. Mathematically,

```
n = integer(ST) - 1
f = ST - 1 - n
TL(msec) = \begin{bmatrix} \Sigma & int_{i} \end{bmatrix} + f[int_{n+1}]
i = 1
```

where ST is the mean spikes per train;  $\operatorname{int}_n$  is the last whole interval of the intervals contributing to the train length (TL) and "f" corrects for the fractional contribution from the very next interval,  $\operatorname{int}_{n+1}$ , for trains terminating between intervals  $\operatorname{int}_n$  and  $\operatorname{int}_{n+1}$ . For cell C29UI7R(2), n = 45, "f" = 0.7 and TL = 845.9 + 0.7(18.5) = 859 milliseconds. A vertical train length (TL) line has been drawn on the interspike interval modulation curve in Figure 9B corresponding to the above measurement for cell C29UI7R(2). It can be observed that the mean train length (TL) was reached before the curve lost the smooth transitions between intervals toward the end of the train. No measurements or interpolations were made past the mean train length (TL). This cutoff was observed for most cells.

The mean cycle time (CT) was calculated to the nearest 10 milliseconds by computing the reciprocal of the mean respiratory rate (RR). That is,

 $CT(msec) = 10 \cdot integer[(RR^{-1} \cdot 60000 msec/min)/10]$ For cell C29UI7R(2), CT = 10 · integer(6000/30.1) = 1990 milliseconds.

From program DATA, the number of intervals per individual train and individual first interval times contributing to single steady state averages were stored on LINC magnetic tape. These values were retrieved by program \$CALC1 for calculation of the standard deviation (SD) and standard error (SE) for each. These standard statistical measurements were made as follows:

$$SD = \sqrt{[\Sigma X^{2} - (\Sigma X)^{2}/N]/[N - 1]}$$
$$SE = SD/\sqrt{N}$$

where X represents the individual intervals for either case and N is the number of respiratory bursts averaged. For cell C29UI7R(2), N = 44 and  $SD_{ST} = 3.9$ ,  $SE_{ST} = 0.58$ ,  $SD_{FI} =$ 11.1 and  $SE_{FI} = 1.68$  milliseconds.

The plateau level (PL), defined as the length of time the interspike interval modulation curve was within 10% of the minimum interval (FI - MI difference = 100%), was measured to the nearest millisecond. That is,

> n = integer(ST) - 1K = 0.10(FI - MI) + MI

$$PL(msec) = \begin{bmatrix} \Sigma & int_{i} < K \end{bmatrix}$$
$$i=1$$

where ST is the mean spikes per train, FI is the first interval, MI is the minimum interval and int<sub>n</sub> is the last whole interval of the intervals contributing to the mean train length. The plateau level (PL) is drawn in Figure 9B as a horizontal line extending between two vertical lines which intercept the experimental interspike interval modulation curve at the 90% level. Intervals meeting the requirements, but falling after the mean train length (TL), were disregarded. The plateau level (PL) for cell C29UI7R(2) was 368 milliseconds.

The last interval (LI) was defined as the interspike interval time of the experimental curve at the end of the measured mean train length. This parameter was calculated to the nearest 0.1 millisecond and is circled in Figure 9B at the end of the train. Mathematically,

n = integer(ST) - 1

f = ST - 1 - n

 $LI(0.1 \text{ msec}) = f[int_{n+1} - int_n] + int_n$ 

where ST is the mean spikes per train,  $\operatorname{int}_n$  is the last whole interval of the intervals contributing to the mean train length (TL) and  $\operatorname{int}_{n+1}$  is the very next interval. The "f" measurement computes a linearly interpolated last interval (LI) correction for train lengths (TL) terminating between intervals  $\operatorname{int}_n$  and  $\operatorname{int}_{n+1}$ . For cell C29UI7R(2), LI(0.1 msec) = 0.7(18.5 - 16.7) + 16.7 = 18.0 milliseconds with the train terminating between the 45th and 46th intervals.

The slope (SL) was a measure of the initial rate of change in the interval time of the interspike interval modulation curve. The slope was defined as

SL = (SI - FI)/SI

where FI is the first interval and SI is the second interval. The slope of the dashed lined connecting the first two circled intervals in Figure 9B corresponds to this measurement. For cell C29UI7R(2), SL = (41.9 - 56.1)/41.9 = -0.34.

The plateau level percent (PLP) was defined as the ratio of the plateau level (PL) to the mean train length (TL). For example,

PLP(%) = (PL/TL) 100

This parameter was a normalized measure of the fraction of the cell's "on" time occupied by intervals within 10% of the minimum interval (MI). For cell C29UI7R(2), PLP = (368/859)100 = 42.8%.

The last measurement made by program \$CALC1 was the train legnth percent (TLP). This parameter was defined as the ratio of the mean train length (TL) to the cycle time (CT) or

TLP(%) = (TL/CT)100

This measurement normalized the fraction of the respiratory cycle occupied by respiratory cell activity (e.g. percent "on" time). For cell C29UI7R(2), TLP = (859/1990) 100 = 43.2%.

2. \$CALC2

Similar to program \$CALC1, this second calculation program derived the final twelve parameters from the LINC magnetic tape. These parameters were added to the columnar data previously calculated, thus completing the number of parameters measured for each steady state observation to thirty-four. The following new parameters were calculated. All examples are taken from cell C29UI7R(2) data listed in Table I permitting verification via hand calculations.

As illustrated by the horizontal lines traversing the interspike interval modulation curve in Figure 9B, the interspike interval times were normalized into percent levels. The range extended from the first interval (FI = 0%) to the minimum interval (MI = 100%) with additional horizontals drawn at the 50, 70 and 90% levels. Where these immaginary lines crossed the experimental curve, vertical lines corresponding to times to reach 50, 70, 90 and 100% levels (T50, T70, T90, T100) were constructed. Measurements of T values were carried out to the nearest millisecond. Linear interpolations were performed in cases where 50, 70, and 90% horizontal levels crossed the curve between two intervals. Associated with these four measurements (T50, T70, T90, T100) were four parameters (N50, N70, N90, N100) representing the number of intervals elapsed before each level was reached. The mathematical expressions used to calculate the T and N values are given below:

K = (1 - P/100) (FI - MI) + MI

$$T(msec) = \begin{bmatrix} \Sigma & int_{i} \end{bmatrix} + \begin{bmatrix} K - int_{n} \\ \vdots \end{bmatrix}$$

$$i=1 \qquad (int_{n+1} - int_{n})/int_{n+1}$$

 $N = n - (int_n - K) / (int_{n+1} - int_n)$ 

where P is the percent level and n is the sequence position of the interval preceeding the first interval less than K. For cell C29UI7R(2),

K50 = (1 - 50/100) (56.1 - 12.0) + 12.0 = 34.05T50 (msec) = (56.1 + 41.9 + 38.1 + 35.4) +

 $\frac{(34.05 - 35.4)}{(31.9 - 35.4)/31.9} = 184 \text{ msec}$ 

N50 = 4 - (35.4 - 34.05)/(31.9 - 35.4) =

4.4 intervals

Also for cell Ç29UI7R(2), T70 = 270, T90 = 467 and T100 = 655 milliseconds, and N70 = 7.5, N90 = 17.4 and N100 = 31.0 intervals. From Table 1-D, it can be seen that the minimum interval (MI = 12.0 msec) is the thirty-first interval in the train and corresponds to N100.

Four last parameters were derived by taking the ratio of the T values to the mean train length. That is,

T5P(\$) = (T50/TL)100 T7P(\$) = (T70/TL)100 T9P(\$) = (T90/TL)100T10P(\$) = (T100/TL)100 For example, for cell C29UI7R(2), T5P = (184/859)100 =
21.4%. Also, T7P = 31.4%, T9P = 54.4% and T10P = 76.2%.
3. \$READ

The thirty-four parameters calculated via programs pATA, \$CALC1 and \$CALC2 and stored on LINC magnetic tape were retrieved and printed out by program \$READ for each steady state respiratory discharge. The computer listing of these parameters for cell C29UI7R(2) is found in Table II. All time measurements (TL, CT, SD<sub>ST</sub>, SE<sub>ST</sub>, FI,  $SD_{FI}$ ,  $SE_{FI}$ , MI, MEN, MED, MOD, PL, LI, T50, T70, T90 and T100) are standardized in milliseconds. Parameters that count events (NT, ST, FMN, HSN, MON, N50, N70, N90 and N100) and parameters that are derived from the ratio of time measurements (SL, T5P, T7P, T10P, PLP and TLP) are all dimensionless. The respiratory rate (RR) is given in breaths per minute.

4.	\$SUM1
5.	\$SUM2
6.	\$SUM3
7.	\$SUM4

Similarly to program \$READ, these four programs printed out the thirty-four parameters calculated for each steady state observation, but in a modified format. That is, instead of lising the different parameters in one vertical column as in Table II, parameters were typed out in horizontal rows so that similar measurements from

τı	050	
	4000	
	. 78 4	
NT	44	
ST	46.7	
SD	3.9	
SE	Ð. 58	
FI	56.1	
SD	- 11.1	• .
SE	- 1.68	
NI	<u> </u>	
FMN	~ 2011	
K5N	2000	
NEN ·		
NDD	17.2	
MUN	151	
		an na sana sanna sa
LI	- 18.0	
SL	0.34	
T50	184	
T70	270	
TS0	467	
7100	655	
N50	4.4	
NYU Nga		
N188	21 B	
T5P	21 4	
T7P	- 31. 4	
TPP	54.4	
T10P	75.2	
PLP	42.8	
TLP	43.2	
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с. <b>е</b> — р	· · · · · · · · · · · · · · · · · · ·	

# Table II. Program \$READ computer printout derived from inspiratory cell C29UI7R(2) in Figure 4A.

consecutive steady state observations formed vertical columns. For example, parameters listed by programs \$SUM1 (RR, NT, ST, SD<sub>ST</sub>, SE<sub>ST</sub>, FI, SD<sub>FI</sub>, SE<sub>FI</sub>, MI), \$SUM2 (FMN, HSN, MEN, MED, MOD, MON, PL, LI), \$SUM3 (SL, T50, T70, T90, T100, N50, N70, N90, N100) and \$SUM4 (TL, CT, T5P, T7P, T9P, T10P, PLP, TLP) formed four tables of data. By following down any one of the thirty-four columns, alterations in a single parameter for any one cell could be traced and correlated with induced modifications of the breathing pattern.

#### 8. \$REORD

The thirty-four parameters associated with any one steady state observation were located in sequential addresses on LINC magentic tape. Since this was an inconvenient format for accessing similar parameter types in certain plotting procedures, program \$REORD was used to reorder all the parameters on new LINC magnetic tape. In effect, rows and columns were interchanged which placed similar parameter types in sequential addresses. Two recorded tapes containing inspiratory and expiratory cell data, respectively, were obtained by this procedure.

9.	\$IVO
10.	\$IVI
11.	\$EVO
12.	SEVI

The reordered inspiratory and expiratory tapes that

were constructed via program \$REORD contained steady state measurements from both vagotomized and vagi-intact preparations. The responsibility of these four programs was to divide vagi-intact (VI) from vagi-out (VO) data points for both inspiratory (I) and expiratory (E) cells. This data manipulation of the two reordered types produced four new LINC tapes including inspiratory vagi-out (I-VO), inspiratory vagi-intact (I-VI), expiratory vagiout (E-VO) and expiratory vagi-intact (E-VI) data groups. These four tapes were formated as the reordered tapes and were used for statistical computations and regression plotting of raw data.

### 13. \$ROWM

This program calculated the mean, standard deviation (SD), standard error (SE), high and low values and range for each parameter group stored on LINC tapes I-VO, I-VI, E-VO, and E-VI. The standard deviation (SD) and standard error (SE) calculations were identical to those described in program \$CALC1. One hundred and thirty-six sets of statistical data (4 tapes · 34 parameters types/ tape) were printed out by program \$ROWM.

14.	\$RLIN
15.	\$REXP
16.	\$RLOG
17.	\$RLLG

Linear and curvilinear regressions were obtained

between groups of similar parameter types taking two groups at a time. Excluding eight groups ( $SD_{ST}$ ,  $SE_{ST}$ ,  $SD_{FI}$ ,  $SE_{FI}$ , NT, FMN, HSN and MON), all possible combinations for the remaining twenty-six groups were examined using four different curve fits for each of the four tapes I-VO, I-VI, E-VO and E-VI ( $26^2 \cdot 4 \cdot 4 = 10,816$ regression comparisons). Coefficients for the four equations,

fit 1  $Y = B + X \cdot M + E$  (linear) fit 2  $Y = EXP(B + X \cdot M + E)$  (exponential) fit 3  $Y = B + \ln(X) \cdot M + E$  (logarithmic) fit 4  $Y = EXP(B + \ln(X) \cdot M + E)$  (log<sub>e</sub>-log<sub>e</sub>) along with the correlation coefficient "r" and other statistical computations were derived by transforming data for curvilinear regressions,

> Y = ln(Y) for exponential fit X = ln(X) for logarithmic fit Y = ln(Y) and X = ln(X) for  $\log_e -\log_e$  fit

and performing the following linear regression analysis:

$$DX = \Sigma X^{2} - (\Sigma X)^{2} / N$$

$$DY = \Sigma Y^{2} - (\Sigma Y)^{2} / N$$

$$M = [\Sigma XY - (\Sigma X) (\Sigma Y) / N] / DX$$

$$B = [\Sigma Y - (\Sigma X) M] / N$$

$$r = \frac{M \cdot DX}{\sqrt{(DX)(DY)}} = M(SD_{X} / SD_{Y})$$

$$S = DY - M2 \cdot DX$$
$$E = \sqrt{S/(N - 2)}$$
$$V = r2$$

where X and Y represent the independent and dependent variables, respectively, of the paired groups, N is the number of parameters in either group, M is the slope, B is the Y intercept, and "r" is the correlation coefficient ( $r \leq$ 1.00). Note that "r" can be defined as slope (M) times the ratio of X to Y standard deviations. The standard error of estimate (E) defined a range of regression curves including 68% of the individual observations of Y on X. Assuming that the distribution about the regression line was normal and of equal variance, this error term corresponded to one standard deviation unit on either side of the mean regression line. The V value ( $r^2$ ) described the proportion of the variance of Y that could be attributed to its linear regression on X.

18. \$REGSD

The significant difference between two regression slopes (M<sub>1</sub>, M<sub>2</sub>) was tested by this program. The following calculations applied only to regressions of the same fit (i.e. linear, exponential, logarithmic or log-log):

$$s = (S_{1} + S_{2}) / (N_{1} + N_{2} - 4)$$
  

$$DI = \sqrt{S / (DX_{1} + DX_{2})}$$
  

$$t = (M_{1} - M_{2}) / DI$$

where S, N, DX and M values were obtained from the regression programs and "t" is the standard Student "t" value with degrees of freedom equal to  $(N_1 + N_2 - 4)$ . The "t" values were converted into P coefficients in the program, eliminating the use of standard statistical tables.

19. \$RSIGD

This program calculated the significant difference between the regression coefficients of two regression equations independent of fit. The following calculations were made:

$$Z_{1} = [\ln(1 + r_{1}) - \ln(1 - r_{1})]/2$$

$$Z_{2} = [\ln(1 + r_{2}) - \ln(1 - r_{2})]/2$$

$$C = \frac{|Z_{1} - Z_{2}|}{\sqrt{\frac{1}{N_{1} - 3} + \frac{1}{N_{2} - 3}}}$$

where  $r_1$  and  $r_2$  are the two regression coefficients being compared,  $N_1$  and  $N_2$  are the number of X-Y pairs in fit<sub>1</sub> and fit<sub>2</sub>, respectively, and the C value is correlated with P levels of significance from the normal distribution curve (not the "t" distribution). The values for P were computed for the following levels: >0.05, <0.05, <0.04, <0.03, <0.02 and <0.01.

20. \$PVALR

Correlation coefficients were converted into P levels of significance by first computing Student "t" values.

For example,

$$t = r \sqrt{N - 2/1 - r^2}$$

where r is the correlation coefficient and N is the number of X-Y pairs correlated. As in program \$REGSD, "t" values were converted directly into P coefficients.

21. \$STTEST

The standard Student "t" test was programmed to calculate P values for miscellaneous paired or unpaired data. The "t" value was calculated as follows:

> $DM = \sqrt{(SE_1)^2 + (SE_2)^2 - 2r(SE_1)(SE_2)}$ t =  $|MN_1 - MN_2|/DM$ DF paired =  $(N_1 + N_2 - 2)/2 = N - 1$ DF unpaired =  $N_1 + N_2 - 2$

where  $SE_1$  and  $SE_2$  are the standard errors of the two sets of data,"r" is the regression coefficient for paired data (r = 0 for unpaired data),  $MN_1$  and  $MN_2$  are the means for each data set and N is the number of observations in each set ( $N_1 = N_2$  for paired data). The P values were computed automatically from the "t" values.

## 22. STIMFOL

This program was designed to compute the time elapsed between two digital tape counter values on the tape recorder. Since the tape counter was driven from the take-up reel, the digital read-out was a non-linear function of time. For this reason, a calibration curve was constructed in which the tape counter value was plotted as a function of time (0 - 100 minutes). This curvilinear plot was broken up into nine linear segments from which accurate time durations could be interpolated from two tape counter values. With this program, the length of time cells were recorded and the time between events could be computed, eliminating the need for hand computations from polygraph records.

### D. FOCALPL Programs

## 1. %PLOT

Groups of data, correlated via regression calculations (programs \$RLIN, \$REXP, \$LOG and \$LLG) from LINC magnetic tape data (I-VO, I-VI, E-VO and E-VI), were plotted in scattergram format on the Calcomp digital plotter by program %PLOT. The independent (X) and dependent (Y) variables plotted were under manual selection and scaling factors were determined on the basis of program \$ROWM range values for each data set. All regression plots were transformed to linear coordinates and six plots were placed on each page for space conservation. Program &PLOT is listed in the Appendix along with the other FOCALPL programs.

## 2. %REGP1

Program %REGP1 superimposed mean regression lines and standard error of estimate lines on the scattergram plots of program %PLOT. For any one plot, scaling factors and type of fit were identical. Coefficients for the linear, exponential, logarithmic and log<sub>e</sub>-log<sub>e</sub> equations (fit 1-fit 4) were obtained from the regression data of programs \$RLIN, \$REXP, \$RLOG and \$RLLG respectively. All equations were plotted on a linear scale thus rendering exponential, logarithmic and log<sub>e</sub>-log<sub>e</sub> fits curvilinear. Because of this, error lines above and below the mean regression line were not always parallel with or symmetrical to the latter as with linear regressions.

#### 3. %REGP2

This program was used to superimpose mean regression lines on the same graph for visual comparison. To avoid confusion, scattergram points of program %PLOT and error lines of program %REGP1 were omitted. Six sets of multiple graphs were condensed to one page. This plotting procedure facilitated data reduction and was useful for

## data summarization.

## 4. %LINEP

Induced changes in single unit parameters followed digitally by programs \$SUM1, \$SUM2, \$SUM3 and \$SUM4 were plotted in time sequence by program %LINEP (line plot) for each respiratory cell that was examined for more than one steady state period. With the exception of cycle time (CT), the twenty-five parameters from the regression analysis (T50, T70, T90, T100, PL, TL, FI, MI, LI, MEN, MED, MOD, RR, N50, N70, N90, N100, ST, SL, T5P, T7P, T9P, T10P, PLP and TLP) were plotted on nine graphs (three pages) for each cell. The X scaling was proportioned according to the number of different steady state observations made for each cell and was a non-linear function of time.

#### CHAPTER V

#### RESULTS

## A. Data Presentation

Single cell studies on the neural control of respiration have been organized into three categories which are presented in the following order. First, parameter measurements from similar cell types have been grouped from many cells for regression analysis. This was an attempt to describe general population characteristics of discharge patterns at different respiratory rates and depths. Second, changes in single unit parameters have been followed during induced modification of the spontaneous breathing pattern. Comparison of these single cell data with population regression data revealed the degree of discharge pattern heterogeneity among similar cell types. Third, the correlation between high barbiturate levels and apneusis has been examined at the single cell level. These data were important for interpretation of population and single cell data obtained after barbiturate

modification of the spontaneous breathing pattern.

## Population Data

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The general statistics of the single cell recordings attempted in 60 out of 85 cats used in this study are summarized in Table III. On the average, approximately three respiratory cells were recorded from each cat in a ratio of two inspiratory cells to one expiratory cell. Of these recorded cells, however, over fifty percent were rejected from final data compilation due to generation of uneven interspike interval modulation curves from poor signal-tonoise ratios or non-uniform breathing patterns.

Steady state computer averages were divided into four categories of inspiratory vagi-intact (I-VI), inspiratory vagi-out (I-VO), expiratory vagi-intact (E-VI) and expiratory vagi-out (E-VO) observations. Cells recorded during unilateral vagotomy were categorized with vagi-intact data, since no significant respiratory rate or depth changes were manifest after removal of one vagus nerve.

Each steady state average was identified by a data point number. There was a total of 333 data points each of which contributed 34 parameter measurements (333 X 34 = 11322 parameters) for regression analysis. An average of four data points (range = 1-17) was obtained from each Table III. General statistics of respiratory cells analyzed by computer techniques.

Cell# CellsTypeRecorded		<pre># Cells Analyzed</pre>	<u>State</u> of Vagi	# Data Points		<u>Analysis</u> Time (Min)		<u># Trains</u> (NT)		# Intervals (FMN)	
				Total	Mean	Total	Mean	Total	Mean	Total	Mean
I	T 125	57	VI	175	3.4	188.7	1.1	6079	34.7	256111	1463
			VO	50	5.0	78.0	1.6	1159	23.2	61329	1227
Е	57	26	VI	105	4.6	107.7	1.0	3776	36.0	119825	1141
_		20	VO	3	1.0	3.5	1.2	64	21.3	2543	848
Sum										ł	
Total	182	83		333		377.9		11078		439808	
Grand Mean					4.0		1.1		33.3		1321

respiratory cell. Respiratory cells were recorded for a period of time ranging from 30 seconds to three hours. Steady state averages were derived from mean breathing segments of 1.1 minutes. For all the cells, this analysis time represented more than six hours of spontaneous breathing or more than 25 hours of computer time taking into account the time scaling factor of 4. Derivation of the 333 data points involved over eleven thousand individual breaths and close to one half million interspike intervals. Average interspike interval modulation curves were generated from 33 burst discharges and more than thirteen hundred intervals.

As described in Data Analysis, similar parameter types were grouped together and all possible regression comparisons taking two groups at a time were performed. Interest centered around two regression types in which respiration rate (RR) and mode (MOD) parameters were selected as the independent variables. The respiration rate (RR) parameter, derived from the reciprocal of the cycle time, was a direct measurement of the spontaneous breathing frequency.

The mode (MOD) parameter reflected changes in respiratory depth (or tidal volume assuming constant airflow resistance) as illustrated in Figure 10 for an inspiratory



Figure 10. Idealized representation of airflow velocity (AFV), intrapleural pres-

cell. In Figure 10A, for example, a decrease in mode (MOD) time is associated with an increased intrapleural pressure and increased tidal volume (shaded area under airflow curve) with no change in respiratory rate (RR = k). Figure 10B diagrams a hypothetical situation where a rate (RR) change is observed in the absence of any depth or tidal volume change. In such a case, the mode (MOD) parameter can be shown to be independent of rate (RR) changes.

This reciprocal relationship between mode (MOD) time and depth or tidal volume (TV  $\propto$  1/MOD) is not unusual since it has been established for both phrenic (39, 50, 53, 58) and central inspiratory cells (72, 129), but does make the assumption that no recruitment of units takes place, at least at the central level. Nesland <u>et al</u>. (129) deny that respiratory neurons are recruited, but this can be debated. The mode (MOD) time was selected over the mean (MEN) or median (MED) times since the former falls within the 100 millisecond segment of the phrenic traffic coincident with the peak of inspiration, integration of which yields the best neural correlate of tidal volume (53). The mode (MOD) is also by definition the most common or frequent interval in the average respiratory train.

For expiratory cells, the reciprocal relationship

between mode (MOD) and tidal volume is more involved. Nevertheless, higher frequency discharges (lower mode times) are expected to be found at larger tidal volumes due to elevated afferent feedback, increased active expiratory movements and postulated higher inhibitory thresholds on inspiratory neurons.

The thirty four parameters defined and measured in this study successfully quantitated all phases of a respiratory neuronal spike discharge. The respiratory train or interspike interval modulation curve (Figure 9B) was segmented into initial (frequency increase), middle (frequency plateau) and terminal phases (frequency decrease). Examination of parameter changes during induced alterations in the spontaneous breathing pattern revealed selective modification of certain phases over others. For example, changes in SL, FI, T50, T70, N50, N70, T5P and T7P reflected changes in the initial phase. Changes in MI, T90, T100, N90, N100, T9P, T10P, PL and PLP reflected changes in the middle phase. Changes in LI, TL and TLP reflected changes in the terminal phase of spike activity. The reader should keep the parameters in this type of perspective when following parameter modification at different spontaneous respiratory rates (RR) and depths (1/MOD). The thirty four parameters have been
tabulated in Table IV for convenient reader reference. Both code identification and definition as used throughout the dissertation are listed for each parameter.

Regression plots of 25 dependent variables (\* Table IV) on respiration rate (RR) and mode (MOD) are presented in Figures 11-22 and Figures 23-34 respectively. Three plots for two dependent variables are organized from left to right in each figure for inspiratory vari-out (I-VO), inspiratory vagi-intact (I-VI) and expiratory vagi-intact (E-VI) data respectively. Expiratory vagi-out data (E-VO) have been deleted since only three data points from three expiratory cells were located in vagotomized preparations (cf. Table III). All scaling factors are given for X and Y axes which extend from border to border. The respiration rate (RR) scaling of Figures 11-22 and the mode (MOD) scaling of Figures 23-34 are consistent from plot to plot (X-axis). For any one figure, the scalings of dependent variables (Y-axis) are identical for each of the six plots. Exceptions are found in Figures 19, 28, and 31 where the different dependent parameters have different scaling factors. In these cases, the I-VO, I-VI and E-VI scalings are the same for any one parameter, however. Each axis is labeled with parameter type and appropriate dimension

Table IV. List of parameter abbreviations.

1	CT	Cycle Time
2	T50*	Time to 50%
3	<b>T70</b> *	Time to 70%
4	T90*	Time to 90%
5	T100*	Time to 100%
6	PL*	Plateau Level
7	TL*	Train Length
8	RR*	Respiration Rate
9	ST*	Spikes per Train
10	FI*	First Interval
11	MI*	Minimum Interval
12	LI*	Last Interval
13	MEN*	Mean
14	MED*	Median
15	MOD*	Mode
16	N50*	<pre># of Intervals to 50%</pre>
17	N70*	<pre># of Intervals to 70%</pre>
18	N90*	# of Intervals to 90%
19	N100*	# of Intervals to 100%
20	T5P*	T50 Percent
21	T7P*	T70 Percent
22	T9P*	T90 Percent
23	T10P*	T100 Percent
24	PLP*	Plateau Level Percent
25	TLP*	Train Length Percent
26	SL*	Slope
27	$SE_{ST}$	Standard Error (ST)
28	$\mathtt{SE}_{FI}$	Standard Error (FI)
29	${ m SD}_{ m ST}$	Standard Deviation (ST)
30	$\mathtt{SD}_{FI}$	Standard Deviation (FI)
31	NT	# of Trains
32	FMN	<pre># of Intervals in Interspike</pre>
		Interval Modulation Curve
33	HSN	<pre># of Intervals in Histogram</pre>
34	MON	# of Intervals at Mode

\*Parameter plotted in Figures 11-43.



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Figure 11. Regression of T50 and T70 on RR for I-VO, I-VI and E-VI cells.



Figure 12. Regression of T90 and T100 on RR for I-VO, I-VI and E-VI cells.

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Figure 13. Regression of PL and TL on RR for I-VO, I-VI and E-VI cells.



Figure 14. Regression of FI and MI on RR for I-VO, I-VI and E-VI cells.



Figure 15. Regression of LI and MEN on RR for I-VO, I-VI and E-VI cells.



Figure 16. Regression of MED and MOD on RR for I-VO, I-VI and E-VI cells.







Figure 18. Regression of N90 and N100 on RR for I-VO, I-VI and E-VI cells.



Figure 19. Regression of ST and SL on RR for I-VO, I-VI and E-VI cells.



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Figure 20. Regression of T5P and T7P on RR for I-VO, I-VI and E-VI cells.

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Figure 21. Regression of T9P and T10P on RR for I-VO, I-VI and E-VI cells.



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Figure 22. Regression of PLP and TLP on RR for I-VO, I-VI and E-VI cells.



Figure 23. Regression of T50 and T70 on MOD for I-VO, I-VI and E-VI cells.



Figure 24. Regression of T90 and T100 on MOD for I-VO, I-VI and E-VI cells.



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Figure 25. Regression of PL and TL on MOD for I-VO, I-VI and E-VI cells.



Figure 26. Regression of FI and MI on MOD for I-VO, I-VI and E-VI cells.



Figure 27. Regression of LI and MEN on MOD for I-VO, I-VI and E-VI cells.



Figure 28. Regression of MED and RR on MOD for I-VO, I-VI and E-VI cells.



Figure 29. Regression of N50 and N70 on MOD for I-VO, I-VI and E-VI cells.



Figure 30. Regression of N90 and N100 on MOD for I-VO, I-VI and E-VI cells.



Figure 31. Regression of ST and SL on MOD for I-VO, I-VI and E-VI cells.



Figure 32. Regression of T5P and T7P on MOD for I-VO, I-VI and E-VI cells.



Figure 33. Regression of T9P and T10P on MOD for I-VO, I-VI and E-VI cells.



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Figure 34. Regression of PLP and TLP on MOD for I-VO, I-VI and E-VI cells.

where applicable. Respiration rate (RR) is understood to be in breaths per minute.

The raw data points for each regression plot are placed in scattergram format. From Table III data, all I-VO plots contain 50 data points from 10 cells, all I-VI plots contain 175 data points from 51 cells and all E-VI plots contain 105 data points from 26 cells. In the regression analysis, each data point was considered as a new observation. No weighting factors were introduced to balance unequal data point contributions from various cells. The three lines drawn in each graph represent the mean regression line and error lines on either side of the mean for the best regression fit. The best fit was defined as that fit (linear, exponential, logarithmic or log-log) possessing the highest correlation coefficient for each set of data. The mean regression and error lines extend from low to high values of the independent variable which includes the entire rate or Mode range observed for each case (I-VO, I-VI, E-VI) in this study. All plots are on a linear scale which renders curvilinear fits non-linear. Transformation of curvilinear regressions back to linear coordinates also distorts the symmetry of error lines on either side of the mean regression line. Still, the error lines include

68% of the raw data points or one standard deviation on either side of the mean regression line. The equations for all regression plots in Figures 11-34 are listed in the Appendix (Tables VIII-XIII). These equations can be used for accurate interpolation of dependent variables from independent variables. The type of fit (linear, exponential, logarithmic or log-log) used to correlate X and Y data for each regression plot are also listed in the Appendix (Table XIV).

Correlation coefficients or "r" values ranged from 0.04 to 0.99 and are given for each regression plot. Steep slopes and/or narrow error bands are associated with large "r" values and good fits. Flat slopes and/or wide error bands are associated with low "r" values and poor fits. The significant difference between "r" values of adjacent horizontal panels is designated by a number sign (#) for P<0.05 or an asterisk (\*) for P<0.01. Blank panels indicate that the correlation coefficients between I-VO and I-VI or I-VI and E-VI plots are not significantly different at the 0.05 level.

In Figure 11, T50 is plotted as a function of RR. For I-VI and E-VI populations, T50 decreases as rates increase from 9.9 to 78.7 and 11.5 to 86.6 breaths per minute respectively. This indicates that at higher

breathing frequencies it takes less time on the average for inspiratory and expiratory trains to reach interspike intervals which are one half the difference between the first interval (FI) and minimum interval (MI). Comparison of I-VI and E-VI plots indicates that expiratory T50's are slightly longer in time than inspiratory T50's for equivalent respiratory rates. The expiratory regression has less scatter and a slightly greater slope as indicated by the significantly higher "r" value at the 0.05 level. For the I-VO population, respiration rate ranges from 7.9 to 30.9 breaths per minute. This decrease in rate response to drug stimulation or depression after vagotomy implicates the vagus in control of respiratory rate. For the T50 parameter, vagotomy significantly decreases the "r" value at the 0.05 level. That is, the correlation between T50 and RR is lost by cutting both vagus nerves (low slope, wide scatter). A similar analysis can be done by the reader for the remaining respiration rate regressions in Figures 11-22.

In Figure 23, T50 is plotted as a function of MOD. Mode ranges are approximately the same for I-VO, I-VI and E-VI populations and extend from 9.2 to 50.0, 5.2 to 43.6 and 5.2 to 42.0 milliseconds respectively. The plots show that T50 is directly related to the mode for

all populations. That is, as the mode decreases (increasing depth or tidal volume) it takes less time for respiratory trains to be activated. The inspiratory and expiratory populations are approximately the same and do not have significantly different "r" values at the 0.05 level. The relationship of T50 versus MOD is by far the best in the I-VO panel (highest "r" value) indicating that vagotomy significantly increases the correlation between T50 and MOD for inspiratory cells at the 0.01 level. Similar comparisons can be made by the reader for the remaining regressions in Figures 23-34.

Correlation coefficients ("r") are placed in rank order for the regression of I-VO, I-VI and E-VI cell discharge parameters on respiration rate and mode in Tables V and VI respectively. Correlations of inspiratory (I-VI) and expiratory (E-VI) parameters as a function of respiratory rate in Table V appear to parallel each other in rank order while vagotomy (I-VO) tends to invert the ordering for inspiratory (I-VI) cells. These same general relationships tend to hold for parameters plotted as a function of the mode in Table VI, but the I-VI - E-VI pairings and the I-VI - I-VO reciprocity are not as well defined. Comparison of respiration rate (Table V) and mode (Table VI) rankings for similar cell types reveals poor order

Table V. Rank ordering of correlation coefficients for the regression of 24 parameters on respiratory rate for I-VO, I-VI and E-VI cell types.

n - n le	T-VO		I-VI		E-VI	
Rank Order	Parameter	<u>"r"</u>	Parameter	<u>"r"</u>	Parameter	<u>"r"</u>
1	TL	.62	TL	.69	TL	.84
2	TLP	.59	T100	.68	T100	.79
3	T7P	.43	T90	.57	FI	.73
4	T5P	.39	<b>T70</b>	.55	Т90	. 72
5	T9P	.38	PL	.53	PL	.71
6	LI	.34	т50	.44	т70	.65
7	ST	.31	FI	.44	т50	.64
8	PL	.31	ST	.33	MEN	.62
9	$\operatorname{SL}$	.30	MEN	.31	MED	.60
10	FI	.30	MED	.30	MOD	.59
11	N 5 0	.27	MOD	.28	MI	.59
12	TlOP	.26	MI	.27	LI	.44
13	PLP	.25	N100	.24	TLP	.43
14	N70	.24	T9P	.21	T7P	.38
15	MEN	.21	$\operatorname{TLP}$	.21	N100	.38
16	N90	.18	LI	.20	T5P	.36
17	MED	.16	N70	.18	ST	.35
18	MI	.15	T5P	.16	PLP	.33
19	т70	.13	PLP	.15	TlOP	.29
20	TlOO	.13	TlOP	.12	N90	.24
21	MOD	.11	N90	.12	T9P	.17
22	N100	.10	T7P	.10	N70	.10
23	T50	.08	N 5 0	.08	SL	.09
24	Т90	.06	SL	.08	N50	.04

Table VI. Rank ordering of correlation coefficients for the regression of 24 parameters on mode for I-VO, I-VI and E-VI cell types.

Dank	I-VO		I-VI		E-VI	
Order	Parameter	<u>"r"</u>	Parameter	<u>"r"</u>	Parameter	<u>"r"</u>
1	MED	.99	MED	.99	MED	.99
2	MI	.99	MI	.99	MI	.99
3	MEN	.98	MEN	.97	MEN	.98
4	т50	.85	LI	.81	LI	.72
5	т70	.84	FI	.69	FI	.68
6	<b>T90</b>	.83	N100	.63	RR	•59 <sub>.</sub>
7	FI	.79	ST	.60	T90	.59
8	T100	.77	N 9 0	.53	Т50	.59
9	SL	.76	T50	.40	<b>T</b> 70	.54
10	T9P	.75	N70	.35	T100	.51
11	T7P	.74	TL	.33	ST	.49
12	T5P	.71	т70	.33	TLP	.47
13	ST	.71	T'90	.30	${ m TL}$	.46
14	TLOP	.67	RR	.28	N100	.35
15	N 70	.56	N50	.28	N 9 0	.30
16	N50	.53	1,100	.26	T9P	.28
17	${ m TL}$	.52	PL	.17	PL	.25
18	N90	.51	SL	.15	TlOP	.24
19	ΓI	.48	TLP	.15	N70	.21
20	$\operatorname{TLP}$	.43	T10P	.14	SL	.20
21	PL	.39	T5P	.13	T5P	.18
22	N100	.12	$\mathbf{P}\mathbf{L}\mathbf{P}$	.11	N50	.17
23	RR	.11	T9P	.07	PLP	.14
24	PLP	.10	T7P	.07	T7P	.13

correlations which may even approach randomization. The reader can use Tables V and VI as references relating to those parameters which are correlated best with either respiration rate (RR) or mode (MOD) for each cell type studied (I-VO, I-VI, E-VI).

The numerous regression plots presented in Figures 11-34 are condensed in Figures 35-43 for reader convenience. In these latter plots, cells are still separated into I-VO, I-VI and E-VI types, but different parameters are superimposed in individual plots. Only the mean regression lines are plotted to avoid confusion from overlapping error lines and raw data points. In each figure, the same parameters are plotted both as a function of respiration rate (RR) and mode (MOD) for easy comparison. The respiration rate (RR) and mode (MOD) scalings are identical to those used in Figures 11-34 and the data ranges are the same. The dependent variable scalings are equivalent for both rate and mode plots for any one figure and correspond to values selected in Figures 11-34 with a few appropriate exceptions. Each axis is labeled with time or percent scales where applicable. Respiration rate (RR) is given in breaths per minute.

In Figure 35, T50, T70, T90 and T100 are plotted



Figure 35. Regression of T100, T90, T70 and T50 on RR and MOD for I-VO, I-VI and E-VI cells.










Figure 38. Regression of MEN, MED and MOD on RR and MOD for I-VO, I-VI and E-VI cells.



Figure 39. Regression of N100, N90, N70 and N50 on RR and MOD for I-VO, I-VI and E-VI cells.







Figure 41. Regression of SL on RR and MOD for I-VO, I-VI and E-VI cells.

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Figure 42. Regression of T10P, T9P, T7P and T5P on RR and MOD for I-VO, I-VI and E-VI cells.



as a function of both respiration rate (RR) and mode (MOD) for I-VO, I-VI and E-VI cells. In accordance with the definition of each parameter, T50 < T70 < T90 < T100 for each of the six plots. Seven comparisons can be made between the six panels (e.g., I-VI to I-VO and I-VI to E-VI for RR and MOD plots and RR to MOD for I-VO, I-VI and E-VI plots). For example, the following observations can be made by comparing adjacent panels in the horizontal plane. Times to reach fractions of the way to the minimum interval (T50, T70, T90, T100) decrease as the respiration rate (RR) increases for both inspiratory and expiratory cells. Vagotomy abolishes this relationship for inspiratory cells. For inspiratory cells, T parameters are almost independent of changes in the mode (MOD) when the vagi are intact (I-VI), but become positively correlated when the vagal influence is removed (I-VO). For expiratory cells, T parameters follow changes in the mode (MOD).

Comparison of adjacent panels in the vertical plane reveals that T50, T70, T90 and T100 parameters for expiratory cells (E-VI) correlate with either respiration rate (RR) or mode (MOD), but parameter correlations for inspiratory cells (I-VI, I-VO) depend on the state of vagal innervation. That is, when the vagi are intact (I-VI),

T parameters correlate best with the respiration rate (RR). When the vagi are cut, the T parameters correlate best with the mode (MOD). This reversal is of importance to consider when comparing rate and depth outputs of the respiratory system. The reader can make similar comparisons between other cell and parameter types from the rest of the superimposed regression plots in Figures 36-43. Major findings from the population data will be elaborated in the Discussion.

## C. Single Cell Data

From the 83 cells (Table III) contributing to the I-VO, I-VI and E-VI population data (Figures 11-43), 14 cells have been selected to illustrate single unit responses to induced or spontaneous changes in respiratory rate and/or depth. The reader should make careful comparisons between the single cell data presented and the population plots of Figures 35-43.

One of the important questions to consider in this study is how well do mode (MOD) interval times of single cells correlate with the depth of respiration. The theoretical reasoning diagrammed in Figure 10 predicts that for any one inspiratory cell, the mode (MOD) should be reciprocally related to the depth of respiration and independent of changes in spontaneous respiratory rate.

Examples from six inspiratory cells (I-VI) are presented to qualitatively establish the mode-depth relationship, point out quantitative cell-to-cell differences and suggest that mode interval times can fluctuate with the spontaneous respiratory rate in some circumstances. For each example, the depth of respiration is defined in relative terms as the average end inspiratory to end expiratory intrapleural pressure difference ( $\Delta$ IPP).

Three histograms and interspike interval modulation curves for inspiratory cell C32UIIR are superimposed in Figure 44A and B respectively. The curves are numbered consecutively, denoting a chronological data point acquisition sequence. Corresponding absolute and percent changes in the respiratory rate (RR), mode (MOD) and respiratory depth ( $\Delta$ IPP) measurements are listed for each data point in tabular format. In this series, there was a substantial spontaneous increase in the depth of respiration (73.1%) with only a small rate decrease (11.9%). The single unit response was one of activation. That is, the histogram interval distribution was shifted to the left (Figure 44A) resulting in a decreased mode time (34.5%) and the interspike interval modulation curve was shifted downward in a parallel fashion (Figure 44B). Rate and mode interaction, if any, cannot be ascertained



Figure 44. C32UIIR. Effect of spontaneous increase in respiratory depth on histogram (A) and interspike interval modulation curve (B). Data points numbered in time sequence. Vagi intact.

from these data. If one assumes that this cell possesses characteristics similar to the population data of Figure 16 where mode and rate are reciprocally related, the rate slowing observed in Figure 44 may limit the mode decrease during an increase in respiratory depth. From the data presented in Figure 44 it is reasonable to conclude that mode time and respiratory depth have a reciprocal relationship.

Figure 45 shows single cell data for cell C80UIIR obtained during a spontaneous decrease in respiratory depth (AIPP). In this case, the depth decreases proportionately more than the rate increases (28.0% versus 13.8% respectively) suggesting that the mode increase (54.5%) is associated with the former. The cell displays a typical deactivation pattern in which the histogram interval distribution shifts to the right and the interspike interval modulation curve is shifted upward. In another cell, not pictured, C29UI7R, the increase in the mode from 10.8 to 13.2 milliseconds (22.2%) was associated with a depth change from 4.4 to 3.7 centimeters of water (-15.9%). The rate change was minimal from 30.7 to 29.7 breaths per minute (-3.3%). These single cell examples suggest that mode time and respiratory depth are reciprocally related.



Figure 45. C80UIIR. Effect of spontaneous decrease in respiratory depth on histogram (A) and interspike interval modulation curve (B). Vagi intact.

Careful inspection of tabular data in Figures 44 and 45 shows that an absolute depth (AIPP) of about 5.2 to 5.0 centimeters of water is paralleled by mode times of 11.6 and 22.0 milliseconds respectively. These differences in single cell firing frequencies at equivalent depths can be explained in two ways. First, the two cats may have had different (and unknown) compliances. Mode time may be directly related to compliance for any given volume or depth. Second, the difference may be attributed to characteristic variations among central inspiratory neurons. Both phenomena are probably operative in the respiratory control system, but the following experiment was addressed to the latter point.

In one cat breathing spontaneously, two inspiratory cells were recorded simultaneously with two separate microelectrodes inserted on opposite sides of the medulla. As shown in Figure 46A, the left cell (I2L) had a higher discharge frequency than the right cell (I3R). The histogram plots and frequency modulation curves of Figure 46B and C, respectively, show firing pattern differences between the fast (I2L) and slow (I3R) cells. Since both cells were recorded at the same time in the same animal, differences in mode time cannot be attributed to variations in mechanical or chemical



Figure 46.

Two simultaneously recorded inspiratory cells from right and left medulla (A), their histograms (B) and interspike interval modulation curves (C). Vagi intact.

factors. Rather, it is suggested that inherent variability exists at the cellular level presumably due to differences in cell size, membrane characteristics and interneurone connections. This reasoning explains the scatter of mode (MOD) values plotted as a function of respiratory rate (RR) in Figure 16 and probably is a factor causing scatter of data points in all the regression plots (Figures 11-34). Because of these cell-to-cell differences, quantitation of parameter interactions (e.g., MOD versus 1/depth) cannot be done at the single cell level. That is, quantitation of one cell's characteristics represents a specific individual case. Quantitation of the whole population requires sufficient sampling of all representative cell types in the respiratory complex and statistical averaging of cell discharges in time and space. The latter is probably handled physiologically at several synaptic levels in the efferent pathway.

Although Figures 44 and 45 suggest that mode changes are associated with modifications in respiratory depth, Figure 47 presents evidence that this is not always the case. Here, a spontaneous increase in the respiratory rate occurs (40.8%) which is accompanied by an increase in the mode (MOD) interval time (31.6%). Since the maximal change in respiratory depth is at best



Figure 47. C28UI5. Effect of spontaneous increase in respiratory rate on histogram (A) and interspike interval modulation curve (B). Vagi intact.

only minimal (2.9%), the cellular depression must have been due to other factors. It is interesting to note that the histogram shift to the right (Figure 47A) is not a smooth transition as seen for the rate elevation. Also, the interspike interval modulation curve shift is not parallel (Figure 47B) as observed for other inspiratory cells (Figures 44-45). That is, the latter part of the train is affected to a larger extent than the initial phase of unit activity. These variations may explain the abnormal mode modification during spontaneous changes in breathing patterns involving rate, but not depth.

Seven cells have been selected to demonstrate the effects of certain drugs on discharge patterns. The pharmacologic agents (pentobarbital sodium, thiopental sodium, doxapram hydrochloride and morphine sulphate) were chosen because of their known effects on gross respiratory function. For example, Figures 48 and 49 illustrate the quantitative responses of cell C62UI3R to two injections of doxapram. Before discussing the physiological responses, however, the format of Figure 49 is described to facilitate reader comprehension of the data presentation. The data from the six remaining cells in this section have identical formats.

In Figure 49, the twenty five parameters examined



Figure 48. C62UI3R. Effect of doxapram on interspike interval modulation curve: A. 1.6 mg/Kg doxapram given between Curves 2 and 3; B. 1.6 mg/Kg doxapram given between Curves 5 and 6. Vagi intact.



Figure 49A. C62UI3R. Effect of doxapram on parameters of inspiratory cell discharge. See text for details.





Figure 49B. C62UI3R. Effect of doxapram on parameters of inspiratory cell discharge. See text for details.



Figure 49C. C62UI3R. Effect of doxapram on parameters of inspiratory cell discharge. See text for details.

by regression analysis (Figures 11-43) are plotted as a function of time in nine panels on three pages. All parameters are identified according to the abbreviations listed in Table IV. By examination of mode and respiration rate trends in the upper and lower panels of Figure 49B, respectively, comparison of single cell characteristics with the mean population data is possible.

Each steady state measurement is marked off by a vertical line which is identified by a data point number at the top and a time measurement to the nearest tenth of a minute at the bottom. The uniformly spaced data points form a non-linear time function on the X-axis. Scaling of dependent variables is given for each group of parameters and appropriate dimensions are supplied. Respiration rate is in breaths per minute. Timings of doxapram injections are identified by inverted triangles with superscript numbers denoting drug dose in milligrams per kilo-1.6 gram (e.g.  $\nabla$ ).

Changes in interspike interval modulation curves for inspiratory cell C62UI3R following two separate injections of doxapram are shown in Figure 48A and B respectively. Superimposed Curves 1 and 2 in Figure 48A are pre-injection controls. Curve 3 represents the discharge pattern change shortly after injection of doxapram

(1.6 mg/kg) and Curve 4 shows partial recovery from drug activation. In Figure 48B, the series is continued using Curve 5 as the new control. The second doxapram injection (1.6 mg/kg) caused a pattern shift to Curve 6, but this activation level was not as high as in Curve 3, possibly due to tachyphylaxis. Curves 7 and 8 are recovery patterns.

Doxapram effects on the individual parameters for cell C62UI3R are shown in Figure 49. Doxapram accelerates the respiration rate (RR) and decreases the mode (MOD) interval time. Corresponding decreases in the first interval (FI), minimal interval (MI), times to reach portions of the way to the minimal interval (T50, T70, T90, T100), plateau level (PL), train length (TL), mean (MEN) and median (MED) times all parallel predicted parameter responses to increased rates and decreased modes from the mean population data (Figures 35-43). The last interval (LI) has an inconsistent biphasic response while the N50, N70, N90, N100 and ST parameters follow predicted changes in the mode but not the rate. The spikes per train response indicates that the mode time is decreasing faster than the train length. The slope (SL) has a very unpredictable pattern which must be associated with the poor correlation coefficients for

regressions of slope on rate (Figure 19, I-VI) and slope on mode (Figure 31, I-VI). Variable responses are seen for the normalized parameters (T5P, T7P, T9P, T10P, PLP) while the percent time the cell fires during the respiratory cycle (TLP) appears to be independent of rate and mode changes induced by doxapram.

Variations occur in the characteristics of single unit patterns in response to barbiturate administration. These are illustrated in the following two sets of data derived from two different cells. The vagus nerves were intact in each case which permits comparison of these single cell data with the mean I-VI population data in Figures 35-43. Data from the first inspiratory cell, C63UI4R, are presented in Figures 50 and 51. Identical doses of pentobarbital (1.5 mg/kg) were injected between each data point. With increasing accumulated dosage of pentobarbital it can be seen that respiration rate decreases from 44.7 to 24.0 breaths per minute (Figure 51B). The mode (MOD) time, however, only slightly increases from 14.0 to 13.8 milliseconds as illustrated in Figure 50A, where histogram distributions fall in overlapping populations. In contrast to the response of cell C62UI3R (Figure 49B) where both spikes per train (ST) and respiration rate (RR) showed parallel increases after doxapram



Figure 50. C63UI4R. Effect of cumulative doses of pentobarbital on histogram (A) and interspike interval modulation curve (B). Vagi intact.











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Figure 51C. C63UI4R. Effect of pentobarbital on parameters of inspiratory cell discharge. See text for details.

injections, ST and RR for cell C63UI4R change in opposite directions during barbiturate depression. This is due to the dramatic increase in train length (TL) following respiratory rate slowing with only a small decrease in the discharge frequency (Figure 50B). Parameters T50, T70, T90, T100 and PL show little change except for T100, which increases abruptly after the sixth injection of pentobarbital (Figure 51A). These observations, coupled with the longer train lengths, explain the decrease in the T5P, T7P, T9P, T10P and PLP measurements (Figure 51C). Vertical shifts of the interspike interval modulation curves are small as shown by the relatively small changes in first interval (FI), minimum interval (MI) and last interval (LI) during drug depression (Figure 51A). Similarly, N50, N70, N90 and N100 parameters show little change until high nembutal levels are reached (Figure 51B). In general, the slope (SL) tends to increase as a function of drug depression, but individual directional changes are not predictable. Finally, pentobarbital causes inspiratory train discharge to occupy more of the respiratory cycle time as indicated by the increase in TLP (Figure 51C). This is due to a greater increase in train length than in cycle time during the slowing of respiratory rate. Most of these pattern changes are consistent

with those predicted from the mean population data (Figures 35-43).

Data from the second inspiratory cell, C83UILL, are presented in Figures 52 and 53. In this case, consecutive equal doses of pentobarbital (1.7 mg/kg) decreases both respiration rate from 71.8 to 29.9 breaths per minute and mode interval time from 21.2 to 14.8 millisec-The latter is illustrated in Figure 52A by a sigonds. nificant shift of the histogram interval distributions to the left. This mode response, which is quite different from that for cell C63UI4R (Figures 50 and 51), is indicative of unit activation (increased firing frequency). This presents an apparent paradox in which increased unit activity occurs during depression of respiratory rate. Data bearing specifically on this problem will be presented in the last part of Results. Similar to cell C63UI4R, the train length of cell C83UI1L was greatly increased by pentobarbital as shown in Figure 52B. The increasing train length and decreasing mode both contribute to an increase in spikes per train, and again the mode is inversely related to respiration rate. While the T50, T70, T90, T100 and PL parameters show predicted responses, an interesting inversion of first and last interval times is seen. That is, with accumulating doses



Figure 52.

C83UIIL. Effect of cumulative doses of pentobarbital on histogram (A) and interspike interval modulation curve (B). Vagi intact.



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of pentobarbital, the first interval and the last interval change in opposite directions (Figures 52B and 53A). The slope again shows tendencies to increase at higher barbiturate doses. This is due mainly to first interval lengthening. Finally, the TLP remains independent of either rate or mode changes induced by pentobarbital depression. Single cell data and mean population data (Figures 35-43) are generally consistent for all parameters plotted as a function of rate, but not as a function of mode. The two significant exceptions are the regression of mode and last interval on respiratory rate.

The next inspiratory cell, C81UI5L, was selected to show single unit response to barbiturate depression in the absence of vagal afferent feedback. The data are shown in Figures 54 and 55 which can be correlated with the mean I-VO population data trends in Figures 35-43. Data point 1 represents a prevagotomy control. Data points 2 and 3 show parameter responses to section LV RV of the left ( $\nabla$ ) and right ( $\nabla$ ) vagus nerves respectively. Most parameter responses appear independent of unilateral vagotomy and become evident only after section of the second vagus nerve. The immediate effect of severing the left vagus on firing frequency is most likely related to the fact that this unit was located in the left medulla.



Figure 54. C81UI5L. Effect of cumulative doses of pentobarbital on histogram (A) and interspike interval modulation curve (B). Left vagus sectioned after #1; right vagus sectioned after #2.










Figure 55C. C8lUI5L. Effect of pentobarbital on parameters of inspiratory cell discharge. See text for details.

Starting with data point 3 as the vagotomized control, the parameters are plotted as a function of pentobarbital dose in Figure 55. Respiration rate decreases from 21.1 to 8.1 breaths per minute and mode time increases from 18.0 to 30.0 milliseconds. This is a typical depression response with the characteristic shift in the histogram to the right (Figure 54A) and an upward shift of the interspike interval modulation curve (Figure 54B). The train length increases, but due to the depression in firing frequency, the spikes per train remains relatively constant. The reciprocal relationship between ST and RR seems to be lost when the vagi are cut, at least for this cell. All other parameters follow predicted directional changes during rate and firing frequency depression when compared to the mean population data (Figures 35-43). It can be noted that the slope data are very unpredictable.

The responses of two expiratory cells during barbiturate accumulation are presented to show not only individual characteristics, but to reveal pattern similarities to inspiratory cells already discussed. The vagi are intact for each expiratory cell, which allows comparisons to be made with the mean E-VI population data in Figures 35-43. The data from the first expiratory

cell, C64UE4R, are plotted in Figures 56 and 57. Respiration rate decreases from 86.6 to 40.5 breaths per minute during pentobarbital depression while the mode shows little change except for a significant decrease from 17.2 to 12.4 milliseconds at data point 4. This single shift in the histogram can be seen in Figure 56A. As with inspiratory cells, the train length greatly increases (Figures 56B and 57A) which causes an increase in the spikes per train. An inverse relationship between ST and RR is thus established. A small increase in the plateau level is also observed. The T50, T70, T90 and T100 parameters tend to increase indicating that pentobarbital modifies the expiratory discharge pattern such that it takes more time to reach portions of the way to the minimum interval. These increases parallel train length increase since T5P, T7P, T9P and T10P measurements remain approximately constant for most of the drug range. The first, last and minimum intervals increase significantly, slightly and not at all as a function of accumulated drug respectively. The N parameters appear to be independent of drug modification except for N100 which increases after three pentobarbital injections. The slope response appears randomized as in other cells. Finally, TLP remains relatively constant indicating that this expiratory cell always fires



Figure 56. C64UE4R. Effect of cumulative doses of pentobarbital on histogram (A) and interspike interval modulation curve (B). Vagi intact.











Figure 57C. C64UE4R. Effect of pentobarbital on parameters of expiratory cell discharge. See text for details.

for the same fraction of the respiratory cycle, regardless of the respiratory rate. All of these single cell observations on expiratory cell C64UE4R follow the mean E-VI population trends in Figures 35-43. It is significant that no outstanding differences between expiratory and inspiratory single cell responses to barbiturate depression can be observed.

Data from the second expiratory cell, C71UE2R, are presented in Figures 58 and 59. Successive barbiturate injections depressed the respiratory rate from 21.6 to 11.5 breaths per minute, but produced a triphasic shift in the mode. The mode first increased from 14.0 to 40.4 milliseconds, then decreased to 26.8 milliseconds and finally increased to 42.0 milliseconds. This can be seen as an inflection in the mode, median and mean curves between data points 9 and 12 in Figure 59B. Every other data point is plotted in Figure 58 to clarify histogram and interspike interval modulation curve shifts. This effect is best seen in Figure 58B. Increasing dosage of pentobarbital first causes an upward shift in the interspike interval modulation curve (data points 1, 3, 5, 7, 9), then a downward shift occurs (data point 11) followed by a final upward shift (data point 13). This pattern resembles the activation of



Figure 58. C71UE2R. Effect of cumulative doses of pentobarbital on histogram (A) and interspike interval modulation curve (B). Vagi intact.













inspiratory cell C83UILL (Figures 50 and 51) during barbiturate administration and will be examined later.

Expiratory cell C71UE2R exhibits several atypical parameter responses during barbiturate depression. For example, pentobarbital has no effect on modifying the train length, a response which was observed consistently for other cells. For this reason, spikes per train mirror changes in the mode and the inverse relationship with respiratory rate is lost. Also, for the first time, the plateau level is seen to decrease as a function of barbiturate dose. Since the train length is not changing, PLP parallels the plateau level decrease and TLP decreases due to a lengthening of the respiratory cycle. The first, minimum and last intervals show variable fluctuations while N50, N70 and N90 parameters appear to be independent of pentobarbital effects. The N100 measurement, however, parallels the spikes per train and generally decreases at higher drug levels. A similar directional change for N100 is observed for inspiratory cell, C81UI5L (Figures 54 and 55) recorded when vagal afferents were removed. The slope pattern for this expiratory cell is very irregular and yields no useful information. Comparison of these parameter responses to the mean population data in Figures 35-43 reveals many

individual differences.

Another expiratory cell, C82UE3R, was examined during morphine administration as shown in Figures 60 and 61. Pattern shifts induced with morphine were considerably different from those seen in expiratory cells during barbiturate administration (Figures 56-59). After a small decrease in respiration rate from 29.4 to 24.0 breaths per minute, the rate was facilitated up to 53.8 with cumulative doses of morphine. This unexpected species-specific result may be attributed to sensitization of pulmonary receptors. A true depression of the discharge frequency is observed as shown by the shift to the right in the histogram distribution (Figure 60A) and the increased mean, median and mode times (Figure 61B). Figure 61 shows that most parameters are decreased by morphine. These effects are in direct opposition to those seen during pentobarbital depression of expiratory cells, but strict comparisons must be avoided since respiration rate alterations with each drug are going in reverse directions. These data indirectly demonstrate that morphine and pentobarbital probably act via different mechanisms. This is a significant observation worthy of further exploration.

Finally, the quantitative effects of vagotomy on



Figure 60. C82UE3R. Effect of cumulative doses of morphine sulphate on histogram (A) and interspike interval modulation curve (B). Vagi intact.



ters of expiratory cell discharge.

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Figure 61B. C82UE3R. Effect of morphine on parameters of expiratory cell discharge. See text for details.



Figure 61C. C82UE3R. Effect of morphine on parameters of expiratory cell discharge. See text for details.

expiratory cell C68UE6R are shown in Figure 62. The first steady state measurement (Curve 1) is a prevagotomized control. One half a minute after cutting the left vagus nerve, a new steady state discharge was attained. The histogram was shifted to the right (Figure 62A) and the modulation curve shifted upward (Curve 2). After an additional 1.7 minutes, the curves assumed position 3. These shifts corresponded to an increase in the mode time from 10.8 to 19.6 to 30.8 milliseconds. This was associated with small respiratory rate decreases from 65.3 to 59.4 to 57.0 breaths per minute. The discharge pattern was analyzed up to 4.8 minutes after the initial unilateral vagotomy, but did not differ significantly from Curve 3. However, subsequent sectioning of the right vagus immediately terminated the expiratory discharge. Since the cell was anatomically located in the right medulla, it is postulated that the right vagal afferents were responsible for the activation of this expiratory unit. Removal of these afferents inhibited unit discharge. These vagotomy effects on an expiratory cell can be compared to the response of inspiratory cell C8lUI5L in Figures 54 and 55 subjected to similar procedures.



Figure 62. C68UE6R. Histogram (A) and interspike interval modulation curves (B) before (Curve 1) and after (Curves 2 and 3) unilateral left vagotomy.

## Barbiturate Apneusis

D.

During single cell depression studies, it was frequently observed that apneustic breathing patterns could be induced after summation of several serial injections of a barbiturate (pentobarbital or thiopental sodium). This well documented phenomenon (cf. Literature Review) was further investigated to facilitate interpretation of the mean population regressions (Figures 11-43) and single cell data (Figures 50-59) previously presented.

Classically, apneusis in the cat can be produced by surgical removal of the rostral pons (pneumotaxic area) coupled with bilateral vagotomy. This is illustrated in Figure 63. Previous to this record, the cerebellum of cat 12 was removed and the brainstem was transected at the level of the inferior colliculi. The cat continued to breathe rhythmically at about five breaths per minute and this breathing pattern was not altered significantly by unilateral vagotomy on the left side. Subsequent section of the right vagus nerve, however, initiated a sustained inspiratory effort as seen in the intrapleural pressure tracing (IPP). Clearly, pneumotaxic and vagal mechanisms play important roles in the maintenance of eupneic respiration. The literature also implicates the cerebellum as an additional source of inspiratory inhibition.





Figure 63. Genesis of classical apneusis in the cat. Prior to the beginning of record an inferior collicular transection was made. The left (LV) and right (RV) vagus nerves were sectioned at times indicated by arrows. Tracings top to bottom: air flow velocity (AFV), intrapleural pressure (IPP) and systemic blood pressure (BP).

Figure 64 shows a representative example of barbiturate induced apneusis in a cat with intact brainstem, cerebellum and vagi. At the arrow, 3.4 mg/kg pentobarbital was injected intravenously, raising the total dosage of barbiturate to 57.6 mg/kg, including the initial anesthetic dose of 30.0 mg/kg. After a short circulation delay, a prolonged inspiratory hold of more than 30 seconds was observed. A normal respiratory pattern then emerged, but the system was operating at a higher end-expiratory % CO, level. It is possible that this elevated CO, drive was responsible for the return to cyclicity. This example illustrates that pentobarbital can in some way block pneumotaxic, vagal and cerebellar inhibitions on inspiratory drive with the resultant genesis of apneusis. Similar results were found using thiopental.

Supportive evidence that the cerebellum is inhibitory to inspiration is given in Figure 65. The control respiratory pattern in panel A was obtained from cat 49 which had brainstem, cerebellum and vagi all intact. Between panels A and B the cerebellum was quickly removed by suction with very little blood loss. Immediately after cerebellectomy the eupneic respiration was transformed into one of apneusis with elevated end-expiratory % CO<sub>2</sub> values (panel B). Eight minutes later (panel C) the



Figure 64. Pentobarbital apneusis. Cerebellum and vagi intact. Injection of 3.4 mg/Kg pentobarbital (arrow) induced a prolonged apneustic breath. Tracings as in Figure 63 with the addition of end-expiratory % CO2 recording in third panel from top.



Figure 65. Appeustic pattern produced by acute cerebellectomy: A. control; B. three minutes later after cerebellectomy; C. recovery after eight minutes. Tracings as in Figure 64.

apneustic breaths were replaced by a normal respiratory pattern and the % CO<sub>2</sub> returned to control levels. Evidently the system is capable of readjustment, suggesting that cerebellar inhibition is of secondary importance (76).

Figure 66 summarizes apneustic threshold data for four different procedures. The apneustic threshold was defined as the amount of barbiturate required to induce the first apneustic breath under various experimental conditions. The total accumulated dose was expressed as the incremental amount over and above the initial anesthetic level of 30 mg/kg pentobarbital. For example, successive small increments of thiopental (A) and pentobarbital (B) were administered until the first apneustic breath was produced (cf. Figure 64). Approximately twice the dosage of pentobarbital was required to reach the apneustic threshold in cats with brainstem, cerebellum and vagi intact. The difference between pentobarbital and thiopental threshold doses was significant at the 0.04 level. This was probably due to the fast acting characteristics of thiopental, a short acting barbiturate that is rapidly absorbed.

In C, drug data are pooled for apneustic breaths induced by vagotomy at low pentobarbital levels and from



Figure 66. Mean and SEM of barbiturate dosage at apneustic threshold: A. thiopental; B. pentobarbital; C. pentobarbital after vagotomy only; D. pentobarbital after cerebellectomy only. Levels of significance: A vs. B, P<0.04; B vs. C, p<0.0005; C vs. D, p>0.4; B vs. D, p<0.03. Ordinate expressed as cumulative dosage over and above initial anesthetic dose of 30 mg/Kg pentobarbital.

pentobarbital titration studies in vagotomized cats failing to show long inspiratory holds following vagal section. In the former group, the apneustic breath observed was not believed to be due to mechanical stimulation of the vagus, since this generally leads to expiratory apnea. Comparison of B and C shows that it was significantly easier (p<0.0005) to induce apneusis at lower pentobarbital levels when vagal inhibition was absent.

Finally, the cerebellum was removed in a group of cats with intact brainstem and vagi. The pentobarbital level to induce apneustic breaths (cf. Figure 65) in this group is shown in D. Comparison of B and D shows that cerebellectomy significantly decreased (p<0.03) the amount of pentobarbital required to induce sustained inspiratory holds in brainstem and vagi intact cats. Although there is no significant difference (p>0.4) between C and D, it cannot be concluded that vagal and cerebellar inhibitions are of equal strength because of the nature of these experiments. That is, apneusis often resulted immediately after vagotomy or cerebellectomy procedures indicating that the apneustic threshold was already exceeded by an unknown amount of barbiturate.

In conclusion, these results show that relatively large doses of barbiturate are required to block major

inhibitions on inspiration before apneusis is produced. However, partial reduction of inhibitory input (vagotomy or cerebellectomy) significantly decreases this barbiturate dose requirement. This implies that apneusis depends on the relative balance between excitatory and inhibitory inputs to the brainstem inspiratory cells.

Figure 67 shows the effect of vagotomy on cat 63 previously subjected to pentobarbital apneusis (17.8 mg/kg incremental dose) and cerebellectomy (22.2 mg/kg pentobarbital level). Thirty minutes after the latter procedure, the cat had recovered to the prevagotomy control pattern in Figure 67. At this point, section of the left vagus immediately prolonged the average inspiratory to expiratory time ratio and subsequent section of the right vagus further increased this ratio. At least two conclusions can be drawn from these results. First, the length of apneustic holds is directly related to the degree of blockade of inspiratory inhibitory systems. Second, a high pentobarbital level may block brainstem interconnections, since the control pattern was lost after unilateral vagotomy on the left side, a response which did not occur at lower pentobarbital levels (Figure 63).

Barbiturate induced apneusis was examined at the



Figure 67. Effect of sequential left (LV) and right (RV) vagotomy on respiratory patterns. Cat previously subjected to cerebellectomy and high doses of pentobarbital. Tracings as in Figure 64.

single cell level. In Figure 68, an inspiratory cell was found to fire continuously during a sustained inspiratory hold induced by pentobarbital administration. An expiratory cell subjected to a similar procedure was inhibited throughout the apneustic breath as shown in Figure 69. These observations support the idea that inspiratory and expiratory cells are reciprocally inhibitory.

In another study, shifts in the histogram interspike interval distribution of a single inspiratory cell were followed after several thiopental injections as shown in Figure 70. In this preparation, which had intact brainstem, cerebellum and vagi, there was a consistent decrease in the respiration rate from 57 to 15 breaths per minute. However, an interesting triphasic shift in the histogram was observed as previously shown for another inspiratory cell during pentobarbital accumulation in Figures 52 and 53. For example, at low incremental thiopental doses (0-4 mg/kg) the histogram was first shifted to the right as the unit was deactivated (Figure 70, top panel). At medium thiopental levels (4-7 mg/kg), the unit became activated causing a shift in the histogram to the left (Figure 70, middle panel). Finally, at high thiopental levels (7-9 mg/kg), the inspiratory cell experienced a second depression



Figure 68. C50UI5R. Single inspiratory cell recording during induction of apneusis after administration of 1.0 mg/Kg pentobarbital (arrow). Tracings top to bottom: unit activity, air flow, intrapleural pressure and end-expiratory % CO<sub>2</sub>.



Figure 69. C64UE5R. Single expiratory cell recording during induction of apneusis after administration of 3.0 mg/Kg pentobarbital (arrow). Tracings as in Figure 68.



Figure 70. Changes in single inspiratory cell histogram during progressive depression of respiration rate (RR) produced by serial thiopental injections. Corresponding respiration rates and histogram modes are indicated by arrows.
trend and the histogram shifted back to the right (Figure 70, bottom panel). Apneusis was never produced.

Explanation of this response most likely involves differential thiopental depression of inhibitory versus excitatory inputs to the medullary inspiratory mechanism. That is, at medium thiopental levels (4-7 mg/kg), a significant fraction of total inhibition could be sufficiently depressed by the barbiturate, thereby allowing inspiratory unit activation. This would result from pneumotaxic, cerebellar or vagal blockade, or partial depression of each by thiopental.

The mode, median and mean interval times from each histogram distribution in Figure 70 are plotted as a function of thicpental dose and respiration rate in Figure 71A and B respectively. The dose is expressed as the incremental level over the initial anesthetic dose of 30 mg/kg pentobarbital. Similar data from expiratory cell C47UE10R are included for comparison. The triphasic shift in interval times for inspiratory cell C41UI2R are clearly seen in each plot. Qualitatively speaking, a mirror image triphasic shift can also be observed for expiratory cell C47UE10R. This was previously seen for expiratory cell C71UE2R (Figures 58 and 59). For example, when the inspiratory unit was depressed, the expiratory



Figure 71.

 Histogram data for cell C41UI2R (Figure 70) replotted to show changes in mean (MEN), median (MED) and mode (MOD) as a function of thiopental dosage (A) and respiration rate (B). Expiratory cell C47UE10R plotted for comparison. unit was activated and vice versa. This implies a negative reciprocal relationship between firing frequencies of inspiratory and expiratory cells.

An attempt was made to determine if pentobarbital could differentially block pneumotaxic regions before medullary areas. The cerebellum was removed from cat 65 and an electrode was inserted into the classical pneumotaxic region of the rostral pons. The vagi were intact. Figure 72 shows the frequency discharge response of three constantly firing (non-respiratory) cells plotted as a function of time before and after pentobarbital administration. Cell Kl, the first cell found, was completely inhibited by a 2.7 mg/kg injection of pentobarbital which brought the total sum dose over the anesthetic level to 4.0 mg/kg. Another cell, K2 was soon found which had a discharge frequency approximately half that of cell Kl. After a 2.7 mg/kg pentobarbital injection, the discharge frequency was sharply inhibited, but rebounded back to the control level in less than a minute. This unit could not be completely inhibited by two additional pentobarbital injections (3.3 and 2.7 mg/kg). Finally, a third constantly firing cell (K3) was located in the upper pons. The firing frequency of this unit was very low presumably due to the high pentobarbital



Figure 72.

Effect of pentobarbital (arrows) on discharge frequency of three non-respiratory pontine cells. See text for details.

level (12.7 mg/kg). When 3.3 mg/kg pentobarbital was given, this cell was completely inhibited like cell Kl and a tendency toward apneusis was observed. Subsequent searching for non-specific units in the rostral pons was not successful and it was concluded that this region of the brainstem was deeply depressed by the total sum level of pentobarbital present (16.0 mg/kg). Replacement of the same recording electrode in the medullary architecture, however, immediately yielded unit activity. Soon an inspiratory cell was located which correlated with the oscillating peripheral parameters. This demonstrated two points. First, the failure to find single cell discharges in the pons could not be attributed to microelectrode failure. Second, the medulla was not as highly depressed as the rostral pons at an incremental pentobarbital level of 16.0 mg/kg. This information suggests that the inflection of the mode curve for inspiratory cell C41UI2R in Figure 71 may be due to depression of pneumotaxic circuits by pentobarbital.

In final studies, miscellaneous procedures were performed to induce apneusis in the spontaneously breathing cat. Figure 73 illustrates the effect of bilateral carotid occlusion (BCO) on modification of the breathing pattern at different pentobarbital levels. In this



Figure 73. Changes in respiratory patterns during bilateral carotid occlusion (BCO) in a vagotomized cat with increasing pentobarbital dosage: A. after 31.0 mg/Kg; B. after 32.8 mg/Kg; C. after 34.5 mg/Kg. Tracings as in Figure 64.

preparation, vagi were cut but the cerebellum was still intact. As the total barbiturate level was elevated from 31.0 to 32.8 to 34.5 mg/kg in panels A, B and C, respectively, there was an increased tendency toward apneusis during each BCO procedure. This demonstrates that a change in inhibitory input to respiratory centers over carotid sinus afferents (baroreceptor or chemoreceptor) can induce apneusis provided the barbiturate depression is at an appropriate level.

Similar results were found in another cat in which carotid sinus pressure was decreased via intravenous administration of histamine as shown in Figure 74. The vagi were cut and the cerebellum was intact as in Figure 73. The accumulated total dose of thiopental over the initial anesthetic dose of pentobarbital was 34.4 mg/kg. The effective dose was lower, since thiopental injections were given over a five hour period. After histamine injection there was a precipitous fall in systemic blood pressure from about 150 to 85 millimeters mercury due to peripheral vasomotor dilatation. A corresponding modification in the breathing pattern resulted with prolongation of the inspiratory duration tesembling apneusis. As the blood pressure returned to a pre-injection control level over the following five



Figure 74.

Changes in respiratory pattern produced by 17.0 µgm histamine phosphate (arrow) in a vagotomized cat. Tracings as in Figure 64.

minutes, the respiratory pattern lost its apneustic form. These results substantiate the conclusions made for Figure 73; namely, a decrease in the inhibitions to the inspiratory mechanism can lead to apneusis when other inhibitory systems are partially blocked by barbiturate depression.

A final attempt was made to induce apneusis by facilitating excitatory inputs to the inspiratory complex. In Figure 75, doxapram, a respiratory stimulant, was given intravenously to a cat with severed vagi and intact cerebellum. The pentobarbital level was at 4.4 mg/kg over the initial anesthetic dose. Following a transient dip in the blood pressure, two prolonged apneustic breaths were produced. This response is consistent with the concept that inspiratory duration is a "simple" algebraic summation function of all excitatory and inhibitory inputs impinging on inspiratory cells in the medulla at any given point in time.



Figure 75. Changes in respiratory pattern produced by 4.4 mg/Kg doxapram (arrow) in a vagotomized cat. Tracings as in Figure 63.

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## CHAPTER VI

## DISCUSSION

## A. Population Modeling

In assessing the experimental data presented in this dissertation, two crucial questions arise: first, how are the limits of a cell population determined, and second, how many single cell elements need to be combined to represent physiological response characteristics of the defined population?

Concerning the first question, the assumption must be made that "singular" biological populations possess inherent variability. Population characteristics may follow normal or skewed distributions, but in either case, variations are present. Recognition of this fact is important, since it may prevent establishment of such rigid criteria for a population (minimization of variability) that only a few elements are eligible. This, by necessity, requires the postulation of a number of other so-called populations. Cohen (40, 41, 42, 43, 45) and others (14, 15, 128, 169, 173), in describing no less than eight different

respiratory phasing patterns, may have failed to recognize inherent biological variability. If so, the elaborate theories on rate and depth control proposed by different individuals (15, 42) are highly questionable. Under these conditions, the experimental analysis no longer deals with real biological entities, but with artifactual systems whose parameters are mere functions of the experimental techniques employed.

A second, but less common error, is the tendency to be over-inclusive when defining the limits of a population. In this case, cells rightfully belonging to separate populations are included within the same category. Subsequent averaging of data results in the masking of real and important physiological trends. Obviously, a balance between over and under selectivity should be sought when attempting to assign single cell observations into appropriate groups. As a guideline, it is suggested that population limits be set such that standard deviations of individual elements approach predictable magnitudes as determined from statistical theory.

Assuming that real physiological populations can be defined, the second question posed above seeks realistic means whereby population characteristics can be accurately assessed. Since it is unlikely that all components

in a population can be sampled, functional description of many systems, notably CNS subsystems, must rely on approximation techniques (31, 41, 51, 101, 102, 127, 129). Two powerful techniques stand out in importance. First, Knight (101, 102) has stressed the importance of averaging repetitive observations from a single cell when describing activity in a population of neurons. In his own words (101), "While at present it is not feasible to record individually from a uniform population of neurons, it is possible to do something equivalent: to record from a single member over repeated stimuli." That is, processes spacially distributed over many components, but occurring at the same point in time, can be approximated by temporal summation of a single component's output at one point in space. Second, Nelson (127) has emphasized the importance of grouping characteristics of individual cells for accurate population description. He writes, "Ideally, the electrode records from but a single element in the system; with data from a large number of such elements it is possible to 'resynthesize' the total population and draw conclusions about the location of units having similar temporal patterns of firing." These two mutually interactive techniques can be coupled as follows in population description studies:

Population	Single Cell Discharge Pattern	# Cells	<u># Cycles</u>
Homogeneous	Smooth	1	1
Homogeneous	Rough	1	N
Heterogeneous	Smooth	N	1
Heterogeneous	Rough	N	N

The number of cells and number of cycles averaged for each cell are listed as either 1 or N (arbitrary large number) in specific combination pairs depending on the type of population and type of single cell discharge pattern. For example, if all the components of a population are identical (homogeneous) and if each discharge is not subject to change fluctuations (smooth), population characteristics can be identified by examination of a single burst discharge from one cell in the population. If all the cells are identical (homogeneous), but are subject to change fluctuations (rough), then it is necessary to average many output cycles from one cell before description of population characteristics is possible. In situations where the population contains a variety of cellular individuality (heterogeneous), it is necessary to sample from a large representative fraction of the population for accurate description. Considering the argument of inherent biological variability presented above, the

first three cases possessing population homogeniety and/or single cell regularity must be rejected as untenable. For the respiratory system, this is confirmed by the rough interspike interval modulation curves for single burst discharges (Figure 9A) and the presence of error lines (standard deviation) in all regression plots (Figures 11-34). This leaves the fourth case which demands that many cycles from single cells and repeated observations on different cells be averaged for population assessment. Description errors are, of course, minimized by maximizing the N values.

In this study, four respiratory neuron populations were defined which subdivided inspiratory and expiratory cell types into vagi-intact and vagotomized groups (I-VO, I-VI, E-VO, E-VI). The limits of each population were inclusive enough to allow for inherent variability, but exclusive enough to avoid masking of important physiological data (determined via range of error lines in Figures 11-34). Data analysis of single cell discharges included generation of common histogram interval distributions (66, 67, 68, 106, 139, 165 and Figure 6) and the new interspike interval modulation curve (Figure 9). The latter quantitatively defined the average interval ordering for a single respiratory cell discharging under

steady state conditions. This technique proved superior to those of Cohen (40) and Bertrand and Hugelin (24) who used modified histogram techniques. From the histogram (Figure 6) and interspike interval modulation curve (Figure 9B), 34 parameters were defined (Table IV) which successfully quantitated all phases of spike activity (initial, middle, terminal). This analysis compares favorably with other work published in the literature in which only a few parameter measurements were made in any one study. For example, the following parameters form an almost complete list of measurements made on single respiratory discharges (listed in decreasing frequency of occurrence - author references not exhaustive): ST (31, 40, 41, 51, 63, 91, 97, 127, 129); TL (31, 41, 51, 63, 91, 97, 127, 129); mean discharge frequency or 1/MEN (31, 40, 51, 69, 72, 91, 97); RR (31, 127, 129); CT (127, 129); peak discharge frequency or 1/MI (40, 97); T100 (97); TLP (129).

Discharge characteristics of the I-VO, I-VI, and E-VI populations were determined by regression analysis of 24 parameter groups on respiration rate and mode (Figures 11-43). The E-VO population data were not reported since only three cells contributed to this group (cf. Table III). Before discussing the parameter trends observed, it is important to consider the degree to which

separate populations have been sampled.

Waldron (174) has estimated that at any one time there are at least 2000 respiratory (inspiratory and expiratory) neurons in the total respiratory complex of the rostral medulla. Assuming this to be a reasonable estimate and assuming an inspiratory to expiratory cell ratio of 2:1 (155), there must be at least 1333 inspiratory and 667 expiratory cells involved in respiratory function (cf. Table III). In this study, only 10 I-VO, 51 I-VI and 23 E-VI cells were analyzed (Table III) which corresponds to 0.8%, 3.8% and 3.4% of each respective population. However, assuming that each burst discharge in time represents one cell in space (101), corrections can be made for the repetitive observations on single cells during curve smoothing procedures. For example, 1159 I-VO, 6079 I-VI and 3776 E-VI trains (Table III) or simulated cell samples contributed 86.9%, 456.0% and 566.1%, respectively, to each population. Within the constraints of these assumptions, the mathematical analysis used in this study has provided an excellent estimate of the inspiratory (I-VO, I-VI) and expiratory (E-VI) populations. Data interpretation should be weighed accordingly.

Parameter regressions plotted in Figures 11-43 represent specific population trends during barbiturate

and doxapram induced modifications in the spontaneous respiration rate and mode interval time. If it can be assumed that mode and tidal volume are reciprocally related as the rationale in Results proposes, specific characteristics in respiratory cell discharge patterns can be correlated with the two major outputs of the respiratory system namely, respiration rate and depth. Both rate and mode curves (Figures 11-43) can be viewed as barbiturate depression curves since pentobarbital or thiopental administration leads to decreased rates and tidal volumes (82, 131). Relatively speaking, the contribution from doxapram-facilitated data points is minimal.

Two series of figures are presented to summarize I-VO, I-VI and E-VI population characteristics. In the first series, Figures 76-80, regression correlation coefficients ("r" values) are plotted in bar graph format for each parameter as a function of either respiration rate or mode. All populations are represented. The "r" value reveals the degree of population homogeniety toward any one parameter. For example, as "r" values range from 0.00 to 1.00, there is a population trend or shift from complete heterogeniety to complete homogeniety. By definition, all parameters fall with these limits. For specific respiration rate or mode plots, different populations



igure 76. Comparison of correlation coefficients for 24 parameters on respiration rate for I-VO (solid), I-VI (open) and E-VI (striped) cells: # = P<0.05; \* = P<0.01.





Figure 78. Comparison of correlation coefficients for 24 parameters on respiration rate (open) and mode (striped) for I-VO cells: # = P < 0.05; \* = P < 0.01.







Figure 80. Comparison of correlation coefficients for 24 parameters on respiration rate (open) and mode (striped) for E-VI cells: \* = P<0.01.

exhibit different "r" values. Also, any one parameter usually correlates better with respiration rate than mode and vice versa. In such cases, the significant difference between "r" values is indicated by a number sign (#) for P<0.05 and an asterisk (\*) for P<0.01. Lack of a symbol designates that "r" values are not significantly different at the 0.05 level.

Figure 76 shows that for the first 12 parameters (T50 - MOD) expiratory cells have a higher degree of correlation with respiration rate than do inspiratory cells. This indicates that for these parameters, the expiratory population possesses less individual cell-tocell differences and is relatively more homogeneous than either inspiratory population. Comparison of I-VO and I-VI data for the first 12 parameters shows that vagotomy usually decreases the correlation coefficients of inspiratory cell characteristics on rate. This evidence supports the concept that the control of respiratory rate operates through vagal afferent feedback (55, 57, 73, 129, 161, 162, 171). None of the latter 12 parameters (N50 - TLP) for any cell type in Figure 76 display high "r" values, illustrating that these measurements are relatively independent of rate changes.

Figure 77 shows that I-VO parameters usually correlate

best with mode, indicating that vagotomy significantly entrains many inspiratory discharge characteristics with alterations in respiratory depth. The expiratory and I-VI orderings are fairly consistent with rate data (Figure 76), with E-VI cells showing higher correlations on mode than I-VI cells. Also, the last 12 parameters for these two populations correlate very poorly with mode suggesting that, with the exception of I-VO parameters on mode, these parameters are poor indicators of either rate or depth changes.

In Figure 78, I-VO parameter "r" values are presented for both rate and mode regressions. Similar plots are found in Figure 79 for I-VI cells. When the vagi are intact (Figure 79), parameters derived from the summation of intervals (T50 - TL) correlate best with respiration rate, while individual interspike intervals (FI -MOD) correlate best with the mode. Parameters N50 - ST show an increased tendency to correlate with the mode, but the latter parameters (SL - TLP) fail to correlate with either rate or mode for I-VI cells. Sectioning of the Vagi (Figure 78) significantly alters the correlation pairing for inspiratory T50 - PL parameters from rate to mode. The significant TL correlation with rate when the Vagi are intact is reduced to no significant difference

from the mode regression after cutting both vagi. The FI - MOD parameters retain their strong mode correlations after vagal section. Finally, vagotomy tends to increase all mode correlations for the last 12 parameters (N50 - TLP) in the inspiratory population. These results show that, with the exception of parameters T50 - TL when the vagi are intact, most parameters correlate best with fluctuations in the mode irrespective of the presence or absence of vagal afferents. In general, this indicates that vertical ordering of the interspike interval modulation curve is more sensitive to depth changes, while horizontal interval ordering ( $\Sigma$  intervals) varies with respiration rate changes. The latter reverts to mode correlations after vagal section.

Figure 80 presents similar data for E-VI cells. Expiratory cells tend to show the same qualitative "r" value pattern as I-VI cells for most parameters (compare with Figure 79). This includes a respiratory rate coupling for horizontal time measurements (T50 - TL) and mode coupling for vertical time measurements (LI - MOD) with the exception of FI. As with I-VI cells, the last 12 E-VI parameters (N50 - TLP) show poor correlations with either rate or mode.

It has been indicated previously that correlation

coefficients or "r" values reveal the degree of homogeniety or degree of fit. This concept of correlation also involves the type of fit since population data were represented by the best of four different regression equations; namely, linear, exponential, logarithmic or loglog. The best type of equation fits for all cell type parameters are listed in the Appendix (Table XIV) for both respiration rate and mode regressions. Taking all 24 parameters at a time for each cell type reveals that 16 I-VO, 11 I-VI, and 13 E-VI parameters are fit best with logarithmic, exponential and logarithmic equations, respectively, as a function of respiration rate. For mode regressions, 19 I-VO, 11 I-VI and 12 E-VI parameters fit best with logarithmic and linear equations respectively. The interpretations of these data are highly speculative but they are suggestive of different processes in operation for different cell populations as a function of either rate or mode.

The second series of summarization data for population studies are presented in Figures 81-83. For each cell type, I-VO, I-VI and E-VI, a family of theoretical interspike interval modulation curves were reconstructed by interpolation of parameter values from regression equations in the Appendix (Tables VIII-XIII) at five



Figure 81.

Theoretical reconstruction of interspike interval modulation curves for I-VO cells. Pattern shifts are shown for increasing respiration rate (A) and for decreasing mode (B). Tabular data is given for selected parameters.



Figure 82.

Theoretical reconstruction of interspike interval modulation curves for I-VI cells. Pattern shifts are shown for increasing respiration rate (A) and for decreasing mode (B). Tabular data is given for selected parameters.



Figure 83.

Theoretical reconstruction of interspike interval modulation curves for E-VI cells. Pattern shifts are shown for increasing respiration rate (A) and for decreasing mode (B). Tabular data is given for selected parameters. different rates and five different modes. Each theoretical curve consists of seven points with the following coordinates:

#	<u>x</u>	<u>Y</u>
1	FI	FI
2	т50	0.5(FI - MI) + MI
3	т70	0.3(FI - MI) + MI
4	Т90	0.1(FI - MI) + MI
5	<b>T100</b>	MI
б	T90 + PL	0.1(FI - MI) + MI
7	TL	LI

Corresponding respiration rate, mode, spikes per train and train length parameters are identified for each curve in tabular format. Consistently, the first parameter is the independent variable and the remaining three are dependent variables. For respiration rate plots, MOD  $\propto$ TL/(ST-1)  $\sim$  k. For mode plots, TL  $\propto$  MOD(ST-1)  $\sim$  k. Rate and mode curves are plotted in the same figures for each cell population. Panel A represents the projected population response to increasing rates. Panel B predicts the population response to decreasing modes (increasing depths). All plots in Figures 81-83 have identical scalings for easy comparison.

Theoretical interspike interval modulation curves

from I-VO population data are plotted in Figure 81. Panel A shows that the family of curves form a tight distribution group, differing significantly only in train length and possibly first interval as the respiration rate is increased. Only a small decrease in mode is observed due to a simultaneous proportional decrease in train length and spikes per train. Panel B shows significant pattern changes in both horizontal (X-axis) and vertical (Y-axis) interval ordering during decrease in mode time (increase in depth). This is due to the high correlation of many I-VO parameters on mode (Figure 78). As the mode decreases, a minimal increase in respiration rate occurs, presumably due to the simultaneous decrease in train length (TLP  $\sim$  k). The latter results from a decrease in mode which is faster than the increase in spikes per train.

Data from the I-VI population are plotted in Figure 82. The curves in panel A show a downward shift as the respiratory rate is increased. Disproportionate decreases in spikes per train and train length produce moderate mode interval shortening. Panel B shows theoretical parallel shifts of the I-VI curves as a function of decreasing mode. The reduction in train length (and, therefore, the increase in respiration rate) follows predicted mode and spikes per train combinations. Comparison of Figures 82 and 81 reveals interesting inspiratory cell pattern differences when the vagi are intact and severed.

The last set of theoretical interspike interval modulation curves are plotted in Figure 83 for E-VI cells. In panel A, an increase in respiration rate is accompanied by a decrease in mode due to a faster decrease in train length than spikes per train. As the mode decreases in panel B, the modulation curve shifts downward in a characteristic activation pattern. Unlike I-VI curves in Figure 82B, E-VI curve shifts are not parallel since a simultaneous decrease in train length occurs. This results from a decreasing mode - spikes per train product as the respiratory depth is increased. Presumably this explains the simultaneous increase in respiration rate as a function of mode. Comparison of E-VI and I-VI patterns in Figures 83 and 82, respectively, demonstrates qualitative similarities between corresponding curves. Quantitatively, however, expiratory cells consistently have lower discharge frequencies than inspiratory cells at equivalent respiratory rates (panel A) as shown by the higher modulation curves for E-VI cells. In mode plots (panel B), expiratory first interval times are significantly longer than those for inspiratory cells.

In summary, the reconstructed discharge patterns

for I-VO, I-VI and E-VI cell groups in Figures 81-83 constitute specific population characteristics corresponding to medullary outputs of respiration rate (panel A) and respiratory depth (1/MOD, panel B). A major conclusion from these data is that respiratory cell discharge patterns have a two-fold dynamic response. In one sense, individual curves represent dynamic modulation of the interspike interval during the train progression as indicated by the "U" shaped quality of all curves. This property of discharge has been recognized by many investigators (51, 69, 72, 74, 91) who have described frequency modulation curves for single respiratory cells. In a second sense, however, respiratory discharge patterns are dynamically locked to the respiration rate and mode outputs. Only a few workers have realized this for rate (31, 127, 129) and depth changes (129). From the data presented in this dissertation, it is suggested that the interpretation of single respiratory cell discharge characteristics must incorporate respiration rate and depth modifications. This suggests that single cell data acquired under differing rate and depth conditions should not be averaged together as Nesland et al. (129) failed to recognize.

## Single Cell Elements

As previously discussed, all regression plots (Figures 11-34) characteristically possessed standard deviations (error lines) from the mean regression line, indicative of inherent biological variation within each defined population of cells. Selected single cell responses to induced or spontaneous modifications in the breathing pattern were presented in Results to illustrate this cell to cell variability in otherwise homogeneous neuron populations. Figure 46, for example, presents evidence that two cells recorded at the same time can exhibit wide variation in discharge frequency. To summarize single cell differences from and similarities to population characteristics, interspike interval modulation curves for individual units (Figures 44-62) and theoretical units (Figures 81-83) can be compared for corresponding cell types.

Deviations from I-VO population predictions (Figure 81) are seen for inspiratory cell C81UI5L in Figure 54B. After severing both vagi (data points 1 and 2) data points 3-10 represent interspike interval modulation curve response to cummulative doses of pentobarbital. A simultaneous decrease in respiration rate and increase in mode interval time resulted in a predicted increase in train length, although no overall change in spikes per train was observed. Induced modifications in the latter parameter were masked by significant depression of both rate and depth components by the barbiturate (82, 131).

Many single cell comparisons can be made with the theoretical I-VI population data (Figure 82). Inspiratory pattern responses for two cells, C32UIIR (Figure 44B) and C80UI1R (Figure 45B), show parallel shifts during spontaneous depth increase and decrease, respectively. since respiration rate modification in each case was at best only minimal, both modulation curve sets match predicted I-VI population patterns as a function of mode (Figure 82B). During a spontaneous increase in respiratory rate with minimal depth change, inspiratory cell C28UI5 (Figure 47B) showed a simultaneous increase in mode interval time. This rendered the single unit pattern response atypical compared to I-VI population characteristics as a function of rate (Figure 82A). For another inspiratory cell, C62UI3R (Figure 48), doxapraminduced increases in respiratory rate revealed typical discharge pattern responses. That is, the interspike interval shifted downward as the mode interval time decreased with a simultaneous decrease in train length and
spikes per train. This response paralleled I-VI population predictions during rate increase (Figure 82A). Finally, inspiratory cells C63UI4R (Figure 50B) and C83UI1L (Figure 52B) were followed during pentobarbital administration. The response pattern of cell C63UI4R during respiration rate decrease closely followed population trends (Figure 82A) with increases in mode, spikes per train and train length. The response pattern of cell C83UI1L, was atypical. In this case, respiration rate was decreased and train length was lengthened, but a significant decrease in the mode interval time caused an exaggerated increase in spikes per train. The modulation curve shift (Figure 52B) appeared to possess characteristics of theoretical I-VI population curves as a function of both rate and mode.

A few single expiratory cell examples can be compared with E-VI population predictions in Figure 83. Cell C64UE4R (Figure 56B) and cell C71UE2R (Figure 58B) were subjected to cumulative doses of pentobarbital. In the former case, only a slight decrease in the mode was observed as the rate was significantly decreased. There was a corresponding increase in spikes per train and train length. With the exception of a peculiar inflection in the interspike interval modulation curve

for the first three data points (Figure 56B), this pattern response resembled theoretical E-VI population trends during rate decrease (Figure 83A). In general, cell C71UE2R pattern shifts paralleled E-VI population constructions as a function of mode (Figure 83B). During pentobarbital accumulation, there was only a slight respiration rate decrease while the mode was significantly increased. The train length was not lengthened as predicted, but spikes per train decreased nevertheless. In Figure 60B, expiratory cell C82UE3R was depressed by cumulative doses of morphine sulphate. With the exception of the control pattern at data point 1, successive injections of morphine produced atypical interspike interval modulation curve shifts which did not correlate with E-VI population projections related to either respiration rate or mode changes (Figure 83). Morphine caused a slight increase in respiration rate which was inconsistent with Ngai's (132) observations. Also, the mode was increased while the spikes per train decreased, producing a significant shortening in the train length. Examination of Figure 60B reveals that morphine, in this case, exerts its greatest effect on the latter portion of the interspike interval modulation curve. Finally, expiratory cell C68UE6R (Figure 62B) was analyzed before (Curve 1)

and after (Curves 2 and 3) unilateral left vagotomy. The mode interval time and spikes per train changed in opposite directions so that train length, and therefore respiration rate, remained relatively constant. Disregarding the latter two characteristics, the single cell pattern shifts resembled E-VI population data as a function of mode (Figure 83B).

From the comparison of inspiratory (I-VI) and expiratory (E-VI) single cell data and population responses, it is difficult to find major differences between these two neuron groups. Both cell types possess indistinguishable variability during barbiturate depression, and interspike interval modulation curves (Figures 82 and 83) reveal distinct similarities as a function of either respiration rate or mode. Interpretation of these data is consistent with the hypothesis that inspiratory and expiratory neurons are functionally similar. It is possible that these cell types belong to a similar reticular formation cell class, differing only in intercellular connections.

Gross characterizations of respiratory cell discharge patterns include assessment of spike frequency, burst duration and phasing with the respiratory cycle. Variations in the first two parameters throughout the

respiratory complex can be explained on the basis of threshold differences among cells (91) and/or differing combinations of neuronal connections (36). The pairing of cell inputs (excitatory and inhibitory) with threshold characteristics of the membrane defines the level of excitability for any given respiratory neuron. This excitability level for individual respiratory cells and grouped neuron populations fluctuates in phase with the respiratory cycle due to oscillating inputs (156) and variations in threshold values (18, 154).

The data presented in this dissertation indicate that expiratory cells have lower discharge frequencies than inspiratory cells at equivalent respiratory rates and modes (compare Figures 82 and 83) suggesting that the former have less excitatory inputs and/or higher firing thresholds than the latter. Also, the observation that expiratory cell parameters correlate better with rate and mode (cf. Figures 76 and 77) indicates that the E-VI population is relatively more homogeneous than the I-VI cell group. This decreased variability in the expiratory population may be indicative of fewer modulatory inputs to these cells, or of the dominance of one or more inputs with relatively lower variability.

Finally, both inspiratory and expiratory cells

tend to fire for a constant fraction of the respiratory cycle (TLP  $\sim$  k) irrespective of respiration rate or depth changes (Figures 49-61). A wide variety of percentages are found for I-VO, I-VI and E-VI cell groups (Figures 22, 34 and 43) indicating that all cells in any defined population do not have identical starting and stopping times. Further study into this phenomenon, preferably at the intracellular level, should provide important data on single cell inputs and threshold characteristics.

## C. Respiratory Complex Organization

The most consistent definition of apneusis refers to the situation where inspiratory mechanisms are locked in a hold position for an extended period of time. This respiratory pattern can be induced either by appropriate neural transections (112, 113, 114, 116, 117, 136, 167, 176 and Figure 63) or high barbiturate levels (31, 82, 131, 151 and Figure 64). Although both techniques result in prolonged inspiratory times, significant differences occur in the depth of inspiration. Neural transections produce near maximal inspiratory efforts while barbiturate administration produces a prolonged, but shallower inspiratory hold. Although this difference cannot be seen by comparing Figures 63 and 64, this result is presumably due to partial depression of the

inspiratory mechanism by barbiturate.

The production and abolition of apneusis has been useful in modeling the organization of brainstem respiratory mechanisms. For example, localized lesions in the rostral pons in vagotomized prepartions have resulted in apneusis (22, 93, 134, 147, 151, 152, 170, 172). Investigators have suggested that this pneumotaxic area is inhibitory to inspiration. Transection between the medullary-pontine border in apneustically breathing animals converts this pattern into one of gasping (26, 87, 112, 133, 136, 167, 170). Coupled with the former data, this suggests that the lower pons contains a constantly discharging cell population which is excitatory to rhythmically active medullary inspiratory neurons. From this work and similar studies, a general concept of respiratory organization developed which suggested that medullary inspiratory neurons are inhibited by vagal, pneumotaxic, cerebellar and expiratory cell connections and are facilitated by apneustic drives.

The fact that barbiturates can induce apneusis suggests that respiratory inhibitory mechanisms are differentially more susceptible to pharmacologic blockade than facilitatory systems. If this were not the case, barbiturate administration should result in apnea or expiratory holds as seen with morphine (132). Figure 72 implies that rostral pontine cells are depressed before medullary cells at equivalent barbiturate levels in the same cat. This finding is consistent with the observation that barbiturates act at high levels of the CNS and then work their way down the neuraxis as the dose is increased. Anatomically speaking, then, the pneumotaxic region may be depressed before the apneustic or medullary areas with cumulative barbiturate administration.

When the vagi are intact, it takes a higher dose of barbiturate to induce apneusis than when the vagi are severed (Figure 66). Assuming that pneumotaxic circuits are the first to be blocked as discussed above, this drug level difference suggests that either vagal influences or inspiratory mechanisms are mediated at sub-pneumotaxic stations (lower pons) or inhibitory synapses are more susceptible to barbiturate blockade than facilitatory synapses. In either case, high barbiturate levels appear to disrupt brainstem connections so that unilateral vagal influence cannot cross over to the opposite brainstem side (compare Figures 63 and 67).

The notion that apneusis results from a preponderant influence of facilitatory versus inhibitory drives on inspiration was introduced in Results. This concept

is actually a combination of Gray's (77) multiple factor theory ( $\Sigma$  chemical factors) and Gesell's <u>et al</u>. (71) reflexogenic components ( $\Sigma$  neural factors). For example, removal of inhibition via cerebellectomy (76, 83 and Figure 65), vagotomy (Figure 67) or decreasing carotid sinus pressure (BCO, Figure 73; histamine, Figure 74) all produced apneustic breaths. Similarly, increased facilitatory drive via doxapram (Figure 75) produced identical pattern changes. These results could only be observed when the barbiturate level was significantly higher than the initial anesthetic dosage (30 mg/kg pentobarbital). At lower levels, cerebellectomy, showed little, and vagotomy showed marked rate and depth changes, while decreased sinus pressure (86) and doxapram produced definite rate acceleration and depth increase. From these data it is suggested that pneumotaxic inhibitors must be blocked by barbiturate before apneusis can be induced by various experimental procedures. Krieger, Christensen, Sapru and Wang (105) have recently postulated the presence of another inhibitory afferent pathway in the cervical cord, which modulates pontine apneustic mechanisms. If this is a real entity, it represents another inhibitory input to the inspiratory system.

Results derived from single cell studies support

the conclusion that barbiturates differentially block inhibitory before facilitatory inputs. Figure 68 shows that inspiratory cells fire continuously during apneusis indicating that they are not depressed to an appreciable extent by barbiturate. Expiratory cells, on the other hand, are completely inhibited during the apneustic breath (Figure 69) due to direct barbiturate depression or more probably to reciprocal inhibition from constantly active inspiratory cells. Robson <u>et al</u>. (148) found similar results, but also described constant expiratory activity in some circumstances.

An interesting exception was observed for inspiratory cell C54UI13L as shown in Figure 84. A prolonged apneustic breath was produced one and one-half minutes after pentobarbital injection (new incremental dose level at 19.6 mg/kg). Unlike the inspiratory cell response in Figure 68, cell C54UI13L failed to fire continuously during the inspiratory hold. Rather, the unit turned off at a train length that was not significantly different from control. The cell recording was not lost at this time since the cell fired during succeeding breaths. This atypical unit discharge could arise from an inspiratory cell on the fringe of the I-VO population that was blocked by barbiturate or from a starter neuron



Figure 84.

C54UI13L. Single inspiratory cell recording during induction of apneustic breath (arrow) 90 seconds after administration of 1.8 mg/Kg pentobarbital. Note failure of unit to maintain discharge for duration of the inspiratory hold as in Figure 68. Vagi sectioned.

or pacemaker cell responsible for activating the inspiratory complex. The latter speculation is an exciting possibility which merits further investigation.

The triphasic shift in the histogram distribution in Figures 70 and 71 shows that an inspiratory cell with vagi intact can, in fact, be activated during barbiturate accumulation. Since the respiration rate was consistently depressed, the coupling between rate and unit discharge frequency was destroyed. In normal cases, rate and cell discharge frequency change in the same direction (31). Therefore, this uncoupling at medium barbiturate levels represents a significant change in brainstem functional activity during drug depression. More specifically, by comparison of Figures 66 and 71, the inflection in the inspiratory curves in the latter figure can be attributed to pneumotaxic blockade. That is, the inflection occurred at a low barbiturate level (4-7 mg/kg thiopental) not sufficient to block vagal inhibitory feedback (Figure 66). Also, apneusis was not seen at this drug level.

Following apneustic breaths there is usually an elevated end-expiratory % CO<sub>2</sub> (Figures 64, 65, 67, 68, 69, 73, 74). It was suggested that this central chemodrive was of sufficient magnitude to periodically interrupt inspiratory holds. This view is inconsistent with Stella's (168) data, which showed prolonged apneustic breaths induced by either  $CO_2$  administration or rebreathing. On the other hand, Ngai (130) showed that 10%  $CO_2$  accelerated the apneustic cycling, a response independent of peripheral chemoreceptor drives. Aström (9) has published excellent work on the combined action of  $CO_2$  excess and  $O_2$  deficiency in the regulation of breathing. The work of Mitchell and Herbert (123) should also be considered. These workers showed that  $CO_2$  does have a direct effect on central inspiratory neurons in terms of rhythm generation (increased frequency discharge) although  $CO_2$  does not change the resting membrane potential.

D. Information Transfer

The data presented in this dissertation have established certain quantitative relationships between respiratory cell discharge characteristics and medullary outputs of respiration rate and depth (1/MOD). It is suggested that if this study were repeated at the phrenic motoneuron or vagal afferent level, valuable information on gross properties of intersystem information transfer could be evaluated.

In a control systems approach, it would be ideal to derive transfer functions (ratio of output to input)

relating discharge pattern differences to synaptic processes intervening between successive stations of the respiratory arc. Due to numerous complexities inherent in the system, including proprioceptive modulation of rate and depth outputs at the spinal cord level (7, 54, 159, 160) and rate and depth interactions (37), the application of rigid mathematical criteria in transfer function derivation is quite difficult. Nevertheless, by comparison of idealized interspike interval modulation curves from various respiratory populations (expiratory, inspiratory, internuncial, phrenic, vagal afferent) it may be possible to initiate quantitative description of system couplings.

Gesell <u>et al</u>. (72) studied frequency modulation patterns of respiratory cells and found similar discharge patterns along major arcs of the respiratory system. For two of these components, interspike interval modulation curves for a vagal afferent and phrenic motoneuron were reconstructed in Figure 85A and B from the data of Adrian (2) and Pitts (142), respectively. These curves, generated from single train discharges, have a relatively smooth "U" shaped form which is characteristic of inspiratory and expiratory cells only after averaging of many successive bursts (cf. Figure 9). The regularity



Figure 85.

Interspike interval modulation curves for single train of vagal afferent (A) and phrenic motoneuron (B).

in vagal afferent interval ordering for a single burst (Figure 85A) derives from the highly predictable relationships between lung volume and vagal afferent discharge frequency (2). The regular phrenic pattern (Figure 85B) for a single burst indicates that this motoneuron is acting as a physiological integrator. Spatial summation of several respiratory neurons and/or spinal neurons arriving at phrenic cell bodies results in transformation of the variable medullary output into a smoothed pattern before preceeding to the respiratory musculature (75, 143). Comparison of Figure 85B (RR  $\sim$ 15) with Figure 82A (Curve 1) shows that average medullary outputs also undergo frequency depression as they are converted into phrenic outputs. The phrenic motoneuron may act as a frequency converter to provide suitable impulse frequency to muscles of respiration for tidal volume control (144).

Dirken and Woldring (51) suggested that expiratory cells were activated by vagal afferents. If this is so, the inflation reflex which inhibits inspiration may be mediated through expiratory cells which have inhibitory inputs to inspiratory neurons. The data in Table III shows that only a few expiratory cells could be located when the vagus nerves were sectioned. Moreover,

Figure 62 shows that an expiratory discharge could be inhibited by vagotomy, suggesting that some kind of functional connection exists between vagal afferents and expiratory neurons. Assuming this to be true, the greater homogeniety of expiratory than inspiratory cells may be due to the dominence of highly regular input signals carried over vagal afferents (Figure 85A).

If one studies the respiratory system in terms of respiratory rate and depth outputs, it should be recognized that the transfer function for rate is equal to unity between serially-linked components. This is true since all components of the respiratory arc oscillate at the same frequency. The transfer function for depth, however, remains undefined since it is coded and recoded at each level of the respiratory system.

# CHAPTER VII

## CONCLUSION

1. The experiments presented in this dissertation were designed to investigate three aspects of central respiratory control utilizing computer techniques: (a) population characteristics of inspiratory and expiratory cells in the medulla; (b) characteristics of single elements in the above populations; (c) genesis of apneustic breathing by barbiturate administration and other experimental procedures.

2. The cells examined in these experiments comprised three neuronal populations: inspiratory, vagus nerves sectioned; inspiratory, vagus nerves intact; and expiratory, vagus nerves intact.

3. A new mathematical technique was devised to describe average interspike interval ordering of respiratory trains (interspike interval modulation curves) by temporal summation of consecutive trains discharging under steady state conditions. This technique provides

a capability for detailed analysis of the respiratory train, not possible by histogram analysis.

4. Twenty-five parameters, most of which have not been reported in the literature, were derived from the modulation curves. These parameters describe specific characteristics of the initial, middle and terminal phases of a respiratory train.

5. All parameters for similar populations were correlated with two functional respiratory outputs, rate and depth («1/mode interval time) using regression analyses. The implications of similarities and dissimilarities in the response of inspiratory and expiratory cells were discussed.

6. Theoretical modulation curves were reconstruted from regression equations for each population. These curves predict characteristic alterations in respiratory cell discharge patterns as a function of rate and mode.

7. Single cell parameter responses were analyzed during experimental manipulations designed to modify respiratory rate and depth. Variations in discharge patterns, observed among many single units, were consistent with the expected variation within population distributions.

8. Various experimental procedures were found to

elicit apneustic breathing in cats under pentobarbital anesthesia. Additional doses of depressant drugs appeared to induce apneusis by differential inhibition of negative feedback loops in the brainstem. At appropriate barbiturate levels, decreasing carotid sinus pressure or doxapram administration elicited apneustic breathing, presumably by activation of facilitatory input. In other cases, vagotomy and cerebellectomy also produced apneusis.

9. The data in this study were discussed in the context of possible interneuronal connections within the brainstem respiratory complex.

### CHAPTER VIII

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	4141	2225	5224		JAP .	-2	
	4142	2227	1336		TAD B	ASE	
	4143	2230	3733		DCA I	RL	
	44.4.4	2271	4384	HPDATE.	JH5 5	01.98	
	4445	2220	7774		000 1	01.04	
	4145	2232	2121		TOP 1		
	4146	2233	1734		THD 1	KY/IY I	
	4147	2234	3732		DCA I	OLDY	
	4159	2235	4735		JMS I	RHOVE	, ,
	4454	2276	4794		JHS S	CI 99	
	4151	2220	70/14		010		
	4132	2221	1331		700 1	AL NU	n na na manana kanang kana aka kanana na na na kanana kanana na na na na na na na na kananga persebuah kanana K
	4155	2240	1731		180 1	ULUA	
	4154	2241	1327		THD C	ULUX	المتحافظ المتحدة المحجم والمراجع والمراجع والمرد والمراجع والا
	4155	2242	- 3327-		DCA C	OLDX	
	4156	2243	1734		TAD 1	RYNYT	the state of an and the state of the state o
	41.57	2244	7941		613		
	44.60	2245	4772		TOD I	01.04	
	4100	2240	4770				a a na an an ann a marta. An 1970 - a' ann ann
	4161	2240	1330				
	4162	2247	5550		ULH L	ULUY	
	4163	2250	1321	RDFK4,	TAD 5	- H V	
	4164	2251	2320	· ·	15Z H	11260	and a second a second
	4165	2252	521.6		JHP R	DPK3	
	4166	2253	7200		CLA		ու է այս է երկությունը կարող արաց բարում մինչ պատունը և տարությունը է ունել արող։
	4167	2254	2317		15Z 5	TRADD	
	4128	2255	5286		J'MP R	DPACK	
	44.74	2200	7288	TUPETN.			
	4470	2250	1200	1 1 / 1 4 11/	700 C	01.07	
	4172	. 2231	1321				
	4173	2260	5131	•	DCH I	ULUA	
	4174	2251	1330		THD C	ULDY	د المعادية ا
	4175	2262	3732		DCA I	OLDY ·	
	4176	2263	5600		JMP I	PLTSTG	
	4177			1			
	4288	2264	6666	PNUPDN.	8		
	4281	2265	1724		TAD N	112	
	4000	2200	23640		670 0	1.0	
	42.02	2200	1640		52n C		ta in an
	4203	2267	5215		JHP .	+4	
	4204	2270	1390		THD D	H .	
	4205	2271	3702		DCA I	RPNSTA	
	4296	2272	5275		JMP .	+3	
	4297	2273	4 2 0 4		TAD P	HP	
	4240	2074	7797		DCA I	- EPNCTE	
	4210	2075	2102		705 1	POLDEV	
	4211	2213	1705		700 4	RULUKA	
	4212	2276	1326		THD N	145	· · · · ·
	4213	2277	5664		JMP I	PNUPDN	
	4214	2389	7200	DN,	CLA		
	4215	2381	7201	PUP,	CLA I	AC	
	4216	2782	21.95	RENSTR	PUSTA	Т	
	404.7	2202	2024	00100	01 204		
	4217 4000	2303	SOLT	KULPRAI	ULUKA		
	4229			r 	•		
	4221	2304	9999	5CL00,	0		
	4222	2305	<b>7</b> 288		CLA		
	4223	2306	3713		DCA I	RRAWX	
	-			1.1			•
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	224		2387	3714	DC	A I	RRAHY			•.		100 A.	
4	227		2718	4715	JP	15 1	RSCLPI	E S					
4	225		2310	4716	TE	AD I	RXHVT	1. A.					
4	226		2311	6794	.11	IP I	SCL00		د هند با بریا ہے۔	والمراجع فيتحدث والمحاد وروان		and the second	
4	227	-	2312	3704	DEBUY, PRI	1X -							
4	230		2313	2004		10 10							
- 4	231		2314	2065	NEANTH RAP		т						
4	232		2315	2113	RSULPLI SI								
۵	233		2316	2107	RXNYT, XM	¥ 1 		**					
ר ג	274				/YARIABLE:	5 FO	R PEIS	16					
	075		2317	8888	STRADD, 0							and a second	
	233	-	2728	8868	ми260, <del>0</del>								
4	230		2724	6666	584.8								
- 4	237		2321	0000	CODE B								
4	240		2322	0000	CUVE/U								
4	241		2323	0000	UNIRZIU	- 2							
· 4	242		2324	7776	nnz,	-2							·
4	1243		2325	0077	LL77,	~~				an anna channa anna an			
	1244		2326	7773	ин5,	-5							
	1245		2327	0000	COLDX, Ə								
•	1245		2778	6666	COLDY, 0								
"	1240		2771	7562	DI DX.	PLO	TX+162	2					
	4241		2331	2562	01.04	FLO	TX+163	\$					
4	4250		2552	2002							منديني للترويل		
4	4251		2333	2012	RLIL	UMU	т	and the standard stan					
	4252	•	2334	2110	KYNYI)	- 1111 MOU	 						
	4253		2335	2000	RHOYE,	104							
	4254		2336	2332	BASE,	4	ł						
	4255				1				IODOCTE	-0		and any set of the set	
	4256				ZHOVEMENT	000	ES FOR	S EHCH CI	HKHLIC	. K			
	4057				1							a anti-called a manager of antipartities and the second second second second second second second second second	-
<b></b>	4236		2777	1778	1379;								
	9260	• •	22331	4777	1777;							a ser a companya da la serie da companya da serie da ser	
	4260		2340	1333	4826:								
	4268		2341	4020	40207				_				
	4260		2342	4040	4040,	20							
	4260		2343	4040	4049	7.0						and the participant state and the second state of the second state of the second state of the second state of t	-
	4261		2344	4676	4676)		and the second	******					
	4261		2345	3343	33437								
	4261		2346	3393	3303/								
•···	4251		2347	4042	4042;								
	4261		2359	4889	4000	7B							
	4060		2754	4660	4669;								
	4202		2301	1676	1676;							المتر تعويه عمرت الماريون بالاراعية المر	
	4262		2332	0105	8185.			•					
	4262		2333	0100	4648:							and a second	
	4262		2354	4010	1010	26							
	4262		2355	4840	4040	10						and a subsection of the second se	
	4263		2356	3676	30101		· · · · ·						
	4263		2357	4145	4145;								
	4263		2360	0030	0030;				· · · · · · · · · · · · · ·				
	4263		2361	9399	0000;								
	4267		2362	8888	0000	2 D		1					
	4003		2763	4676	4676;								
	4204		2764	8786	83861								
	4204		2307	0300	:5778								
	4264		2300	1000	10095							and an an experimental second s	
	4264		2366	4000	40000	75							
	4264		2367	4040	4040	12							
	4265		2370	4676	46r6i								
	4265		2371	0306	0306;								
	4265		2372	0333	0333;								
	4265		2777	0000	0000;								
	4505 4505		2724	อกคล	8988	2F							
	4203		5775	4669	4560,								
	4266		2212	, 4000 1272	1676								
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	4267	2402	0376	8376;						• ·
	4267	2403	4543	4643;				. بېلورىن		
	4267	2404	4040	4848;						
	4267	2405	4040	4040;						
- ····	1767	2496	4848	4849	2 H					
	4279	2487	7818	7818.						
	4210	2419	2070	2979:						
	4270	2410	1676	1575:						
	4270	2442	2620	7676					· · · ·	
	4270	2412	2020	20201						
	4270		6، 50 ک	3636	71	an annan ann an an an an an an an an an				
	4271	2414	9972	9972;						
	4271	2415	3630	3630;						
	4271	2416	4626	4626;						
	4271	2417	4646	4646;						
	4271	2420	4646	4646	2J					
	4272	2421	Ð276	0276;						-
	4272	2422	4913	4013;						
	4272	2423	4613	4613;						
	4272	2424	4646	4646;						
	4272	2425	4646	4646	2K					
	4277	2426	8876	8876						
	4272	2427	4848	4848:						
a.c	4022	2478	4649	4848:			a af strandard and a second			
	ペピイン	2420	4848	40407						
	4213	0470	4040	4349	л				· · · · · · · · · · · · · · · ·	
	4273	2432	4040	4040	72					
	4274	2433	2310	23161			······		· · · · · · · · · · · · · · · ·	
	4274	2434	4046	4046;						
	4274	2435	4040	4848;						
	4274	- 2436	4040	4849;						
	4274	2437	4040	4040	2 M					
	4275	2449	4076	4076;						
	4275	2441	4646	4646;		· · · · · · ·				
	4275	2442	4646	4646;						
	4275	2443	4646	4646;		an and a second age of a second second second				
	4275	2444	4646-	4646	2 N					
	4276	2445	.7561	7561;						
	4276	2446	3616	3616;						
	4276	2447	4145	4145;						
	4276	2456	1838	1838;						
	4276	2451	8581	8581	20					
	4277	2452	4676	4676;		•				
	4222	2452	8742	8747:		·.				
	4977	2454	4547	4647:		· ·				
	4211 1077	2455	0005	10737 888 <i>6</i> 3						
	4677	2433	00000	00000	20		· ·			
	4211	24.55	0000	0000	~ ~					
·····	4300	2437	1045	10437				· · · · · · · · · · · ·		
	4300	2458	4140	41407						
	4300	2461	8838	00307						
	4300	2462	2262	22621						
	4300	2463	4872	4072	70					
	4301	2464	4676	4676;				•		
	4301	2465	0343	8343;		· · · · · · · · · · · · · · ·			and a second second	
	4301	2466	4013	4013;						
	4301	2467	4040	4040;						
	4301	2479	4040	4848	2 R					
	4302	2471	3070	3070;						
	4382	2472	4241	4241;						
	4302	2473	1333	1333;						
	4382	2474	0504	0504;					-	
	4385	2475	4616	4616	25					
	4702	2413	7600	7629:						
	4202	2410	BEAE	UEDE:						
	4303	2411 3800	0040	0040) 0404:						
	4303	2000	0000	00001						
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 4797	2581	8685	8686;			a na canada a canada
4303	2502	9595	8686	21		
4303	2583	7601	7691:			
4704	2594	1991	1991:			
 A704	2585	4179	4178:	-		
4304	2586	4130	4646:			
4504	2000	- +0+0 - AEAE	46461	211		
4304	2307	4040 7606	7696	70		
4300	2310	4000	10001		u.	
4380	2511	4020	46201			
 4395	2512	4646	4545			
43-05	2513	4646	4646;			
4305	2514	4646	4646	2¥		
4306	2515	7606	7696;			
4396	2516	2310	2310;			· · · · · · · · · · · · · · · · · · ·
4386	2517	4630	4630;			
4306	2528	4646	4646;			
 4386	2521	4646	4646	28		
4307	2522	4670	4678;			<u>.</u>
4397	2523	0666	8666;		· · ·	
4307	2524	4076	4876;			
4387	2525	4040	4040;			
4387	2526	4848	4848	28		
 4318	2527	7320	7329;			
4319	2538	2386	2386;			•
 4248	2571	4646	4646;		and a second rest of the second rest of the second s	
474.0	2572	4646	4646:			
 4740	2032	4040	46467	20	1 State and the second state of the second state and the second state of the second	
4310	5574	7696	7696.	~ `		
 4311	2334	0000	10001		a na ana ana amin'ny faritr'o ana amin'ny tanàna mandritry mandritry amin'ny tanàna amin'ny faritr'o amin'ny fa	Agen party - and Agent for the standard agent data is an and the standard agent of the standard agent of the st
4311	2030	0045	40401		•	
 4311	2030	4040	40407			
4311	2031	4040	40407			
 4311	2540	4040	4849	72		
4312	2541	7830	78381			
 4312	2542	1510	1610;	· · · ·		
4312	2543	3636-	3636;			,
 4312	2544	3636	3636;			
4312	2545	-3636	3636	- 73		
4313	- 2546	7592	7592;			
4313	2547	0105	0105;			
 4313	: 2558	4341	4341;		المتحافظ والمراجع وال	
4313	2551	4303	4303;			
4313	2552	2545	2545	- ZN		, որություն ու ուսություն արդադարությունը, ու ու ուսում հետել են ու ու են են ու ու են են ու ու են են են են են ե
4314	2553	7010	7010;			
4314	2554	3630	3630,			
4314	2555	1616	1616;			
4314	2556	1616	1616;			
 4314	2557	1616	1616	1)		
4315	2560	7303	7393;			
4315	2561	4325	4325;			
4315	2562	8321	0321:			
4715	2567	8787	8787.		· · · · · · · · · · · · · · · · · ·	
4215	2554	5979	8383	22		
 4315	2504	7041	7941:	•		
4216	2000	7700	2288:			
4240	2000	- 3200 - 8606	1696-			
4310	2331	4000	40000			
4310	2079	4040	キンキンバ スピメピ	2000		
4316	2571	4545	4343	7640		
 4317	2572	0000	6000 66861			
4317	2573	89999	00000			
4317	2574	8899	89897			
4317	2575	0000	0000;			
4317	2576	0000	0000	75PA	CE	
4320	2577	7101	7101;			

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	4228	2699	6441	6441;	
	4220	2681	0474	8474;	
	4778	2682	3664	3664;	~
	4728	2683	2276	2276	
	4320	2604	7510	7510;	
	4721	2695	2213	2213;	
	4321	2686	4332	4332;	
	4221 -	2687	4444	4444;	and the second
	4721	2610	4444 *	4444	/*
	4722 .	· 2511	7501	7501;	
	4322	2612	4145	4145;	
	4322	2613	8191	0101;	
	4322	2614	0101	0101;	
	4322	2615	0101	0101	/NUMBER SIGN
	4323	2616	7521	7521;	,
	4323	2517	3424	3424;	от проволини и слово, воло с настоя на наколикание и сили на стор солоно соло страта имариал с наримала на стра П
<b>2</b>	4323	2620	1314	1314;	
	4323	2621	3233	3233;	
	4323	2622	1212	1212	/\$
	4324	2623	7525	7525;	, manta a a construinte, es a sugargenera a se a se a se a se a serviciente ante en de matematica de de marcos
	4324	2624	1514	1514;	
	4324	2625	1135	1135;	ու է է պա տարությունը տարարությունը անությունը տարությունը համարը է հերու է։ Այս տարարութագրության համարտը է է Դ
	43-24	2626	3231	3231;	
	4324	2627	2121	2121	
	4325	2630	7521	7521;	*
	4325	2631	3424	34241	
	4325	2632	2314	23141	and the second
	4325	2633	3212	32121	
	4325	2634	3232	2222	n for each and the second s
	4326	2030	1223	2615:	
	4320	2030	2010	2010/	and the manufacture of the second
	4320	2031	2330	2727;	
	4220	. 2641	2727	2723	ZAPOSTROPHY
	4222	2642	2636	7636;	
	4321	2643	1325	1325;	and the second
	4227	2644	3821	3021;	
	4327	2645	3939	3030;	and the second
	4327	2646	3030	3939	76
	4336	2647	7010	7010;	e a companya na sange angena angena na kanangena na kanangena na sangena angena kanangena kanangena kanangena a
	4330	2650	3321	3321;	
	433Ð	2651	1625	1625;	
	4330	2652	1616	1616;	
	4330	2653	1616	1616	A) A set of the set
	4331	2654	7521	7521;	,
** * **	4331	2655	1423	1423;	ал так так ал ал ал так так так жана какала какала жана жана жана жана жана катана какала <del>шана</del> на алу баранда жана так ж
	4331	2656	2332	2332;	
	4331	2657	3412	3412;	
	4331	2660	2323	2323	/*
	4332	2661	7521	(521)	
	4332	- 2662	0323	ロンビント	
	. 4332	2663	2343	23431	
	4332	2004	2121	2121	2+
	4552	2000	7011	2211:	
	4333	2000	2122	2122;	
	4272	2679	2111	2111;	
	4222	2671	1618	1010;	and the second
	4333	2672	1010	1010	1.
	4224	2672	7313	7313;	
	4224	2673	6333	6333,	
	4774	2675	3333	3333;	
	4224	2676	3333	3333;	
		2010			;
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4351 4351 4352 4352 4352 4352	2776 2777 3000 3001	6411 2575 1424	6411; 2575; 1424		
4351 4351 4352 4352 4352 4352	2777 3000 3001	2575 1424	2575; 1424		
4351 4352 4352 4352	3000	1424	1424		
4352 4352 4352 4352	3001	1454		<u>, , , , , , , , , , , , , , , , , , , </u>	
4352 4352 4352			7040.	<i>r</i> .	
4352		7210	7210;	in a chairmana s	
4352	2005	2122	2122;		
1757	3003	6410	6410;		
5.72	3994	2575	2575;		
4352	3995	1424	1424	1;	
4752	3886	7545	2545:		
4333	2000	4487	4487.		
4333		4163	47671	· · · · · · · · · · ·	nan kana na mananan kana mananan mananan mananan mananan kanan ka
4353	3010	4141	4141;		
4353	3011	4141	4141;		
4353	3012	4141	4141	74	
4354	3013	7202	7202;		
4754	3914	6342	6342;		
4758	2015	8777	8777:		
4334	2010	0202	03031	• • • • •	
4354	3016	0303	02020		
4354	3017	0303	8383	7=	and the second
4355	3020	7191	7101;		
4355	3021	0543	0543;		No. I we have a second second as a second way of the second s
4355	3922	0505	0505;		
4755	7927	0595	8585		a su
4765	2023	0505	6505, 6565	15	
4333	2024	7505	7505.		•
4356	3023	1203	12025	· · · · -	- A set of the set
4356	3026	3616	3616;		
4356	3027	4445	4445;		الم المحمد الذي الم المحمد التي المحمد ا
4356	3030	2123	2123;		
4255	7871	2868	7868	12	a a secondar and a second a second and a second and a second second a second and a second and
4757			,	•••	•
4331		• •	r	BOCE	
4360				rnuc 0	a na ana ao amin'ny faritr'i Andrea. Ny faritr'i Andrea. Ny faritr'i Andrea. Ny faritr'i Andrea. Ny faritr'i An
4361	3200	2966	DECPLIS	0	
4362	3201	7500		SMA	(1,2,2,2,3,3,3,3,3,3,3,3,3,3,3,3,3,3,3,3,
4363	3202	5207		JHP PLUS	
4364	3203	7041		CIA	ана странски странар ил пола странски странски страний и има и странски силонали и протоком протоком и има странском п
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4371	3210	1274		THD L40	
4372	. 3211	4276		JMS FLT1	a and an
4373	3212	3270		DCA SKPF	
4374	3213	1253		TAD N7	
4225	3214	3221		DCA CNT4	
1212	2015	7762		DCA DIGIT	
1.31 D 4377	2010	1050		TON CHITOTO	
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4400	3217	3263		DCH UNIRZE	ց երքում երկերությունը հետ կարող առու արտարարությունը տեսարեցությունը հետ
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4492	3221	3226		DCA ARRON	
4482	2222	7410		SKP	
4404	2007	3261		DCA VALUE	
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4483	5224	1100		TON DOLDE	
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4497	3226	1254	ARRON,	TAD TENFUR	
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	5993	0231	4114		JMS TYP	
	5004	0232	1854		TAD K310	ZH
	5005	0233	4154		JMS TYPE	
	5006	0234	1066		TRD K240	/SPACE
	5882	0235	4154		JMS TYPE	
	5810	8276	1427		TAD I PR2	ZHIGH
	5011	8237	4114		JHS TYP	
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	5015		0244	1420		THE TUD	/ LON
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	5021		0247	4154		JAS ITE	
	5922		0250	1966		IND K240	25FRUE
	5023		0251	4154		JAS IYPE	
	5824		0252	1431		TAD I PR4	ZNUMBER IRHINS
	5025		0253	4114		JNS TYP	
	5026		Ø254	6211		CDF 10	
	5027		0255	1045		TAD K5800	/INDIVID RATES
	5030		0256	4423		JM5 I T01	
	5071		0257	6281		CDF 8	
	5022		8268	1964		TAD K324	/1
	5032		0200	4154		JMS TVPF	
	5033		0201	4967		TON 2772	2D
	2034		0202	1002			7 K
	5835		0263	4154		JAS IYPE	A second s
	5936		0264	1628		THD KJU1	7H
	5937		0265	4154		JMS TYPE	المعالية المعالم المعالية المحالية المحالية المحالية المحالية المحالية المحالية المحالية المحالية المحالية الم
	5040		0266	1055		TAD K311	21
	5041		0267	4154		JMS TYPE	
	5942		0270	1060		TRD K316	2N
	5943		8271	4154		JMS TYPE	
	5644		0272	1963		TAD K323	25 25
	5045		0272	A154		JMC TVPF	
	5045		0273	4154			ZCPACE
	2046		0214	1000		INC TUDE	7 DI NOL
	5047		0273	4134		JAS ITE	ACDOCE
	5050		9276	1066		1HD K240	/SPACE
	5951		0277	4154		JHS TYPE	ուսույթը, այս երկրությունները տարությունները տեղելությունը, այց արդել տարությունը, որոն համան հետ հայտական համ Դուն է
	5052		0300	1055	· ·	TAD K311	21
	5053		0301	4154		JHS TYPE	2. Construction of the second s second second se second second s second second se
	5054		0302	1060		TAD K316	2N *
	5955		0303	4154	•	JMS TYPE	
	5956		9394	1064		TRD K324	2T
	5057		8785	4154		JHS TYPE	
	5060		8786	1855		TAD K248	/SPACE
	5000		0207	4154		JMS TYPE	
· - · ·	5001		0301	-1955		TAD 1248	JSPACE
	2052		0310	1454		100 N240	7 DI NOL
	5865		0311	4134		JN5 1175	2. Compared ways to an extension of the second sec second second sec
	5864		0312	1963		THU KJZJ	75
	5965		0313	4154		JHS TYPE	յ այլ – ու ուսերին երկլացիալ շարձան երև շահ համան հրամուսը ու հարուսել տարութերիացի երելներին է աներադարեցի տո Համա
	5966		0314	1964		TAD K324	71
	5067		0315	4154		JHS TYPE	and the second of the second o
	5070		0316	1066		TAD K240	/SPACE
	5071		0317	4154		JHS TYPE	
	5972		0320	1432		TAD I PR5	/ST
	5973		0321	4114		JNS TYP	
	5874		0322	1969		TAD K316	/N
	5025		9323	4154		JHS TYPE	
	5076		8724	1.266		TAD K240	/SPACE
	5077		0327	4154		JHS TVPF	
	JUCC EXOD		0325	2014		CDE 10	and the second
	5100		0320	0211		- CPF 10 - TOP 1 20000	ANIMOED TODING
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	5102		0330	4114		JUS INP	
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	5104		0332	4425		JNS I TO3	
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	5106		0334	1053		TAD K306	/F
	5107		0335	4154		JNS TYPE	
•	5119		0336	1055		TAD K311	/1
	5111		8777	4154		JNS TYPE	
	5440		8740	1057		TAD K722	/R
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	5115		U341 D340	40/77		TOD 1772	72
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	5116	Ð344	1064		HD K324	~				
	5117	0345	4154	J	MS TYPE					
	5129	0346	1966		RD K248	758	HUE			
	5121	0347	4154	J	NS TYPE					
	5122	0350	1855	T:	AD K311	21				•
	5107	8351	4154	3.	MS TYPE					
	5124	0752	1868	T	RD K316	2 N				•
	5475	8757	4154	J	MS TYPE				•	
	5125	0353	4064	T	AD K724	21				· · · · · · · · · · · · · · · · · · ·
	5126	0334	1004	Ţ	MC TUPF					
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	5135	0363	4154	- J	NS TYPE					
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	51.48	0366	1055	Т	AD K311	. 21				
	5141	9367	4154	J	MS TYPE					
	5141	9779	1969	T	AD K316	2N				
	3142	9774	4154		NS TYPE					
	5145	0272	4364	- T	AD K324	21				
	5144	0372	1004	1	MC TUPE	• •				
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	5151	· 0377	4154	J	HS INFE	20				
	5152	9499	1065	1	HD K326	24				
	5152	0401	4154	J	HS INPE					
	5154	0402	1050	. T	AD K391	71				
	5155	0403	4154	J	NS TYPE					
	5156	0404	1856	T	AD K314					••••••
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	5160	0406	1063	ד	AD K323	75			•	
	5161	8407	4154	J	INS TYPE	·				
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	5187	8415	4154		INS TYPE					
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	5172	8428	1.050	-	TAD K316	2 N	متنصب والمراجع والرا			· · · · · · · · · · · · · · · · · · ·
	5172	3424	4154		JNS TYPE					
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	5174	0425	2454		THS TYPE					
	5175	0423	4114		TRD 1 PT2	28	ERN			
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	5201	0427	4724		TAD K311	21				
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	5216	0444	6211		CDF	10	
	5217	0445	1047 -		TRD	K7777	
	5220	0446	4423		JHS	I T01	
	5221	8447	6291		CDF	0	
	5222	8458	1055		TAD	K311	
	5223	0451	4154		JMS	TYPE	
	5224	0452	1063		TRD	K323	
	5225	8453-	4154		JMS	TYPE	
	5226	0454	1055		TAD	K311	
	5227	0455	4154		JHS	TYPE	
	5230	0456	1054		TRD	K310	
	5231	0457	4154		JMS	TYPE	
	5232	0460	1066		TRD	K240	
	5233	9461	4154		JNS	TYPE	
	5234	0462	1966 -		TAD	K240	
	5235	0463	4154	-	JMS	TYPE	
	5236	0464	1057		TAD	K315	
	5237	0465	4154 -	-	JMS	TYPE	
	5240	0466	1061		TAD	K317	
	5241	0467	4154		JNS	TYPE	
	5242	0470	1051		TAD	K304	
	5243	0471	4154		J145	TYPE	
	5244	0472	1066-	· ·	TAD	K248	
	5245	0473	4154		JMS	TYPE	
	5246	0474	1435		TRD	1 P82	
	5247	0475	4114		J # 5	ITE	
	5250	8476	1057 -		THD	K310 TUDE	
	5251	8477	4134		J/15	11755	
	5252	0500	1001		TMC	TUDE	
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	3234 5355	0302	1000		.145	TVPF	
	5256	0505 0594	1966		TRD	K248	
	5257	8585	4154		JMS	TYPE	
	5268	0506	1440		TRD	I PT1	
	5261	0507	4114		JH5	TYP	
	5262	0510	1057		TAD	K315	
	5263	0511	4154		JHS	TYPE	
	5264	0512	1052		TAD	K305	
	5265	0513	4154		JHS	TYPE	
	5266	0514	1051		TAD	K304	
	5267	0515	4154		JHS	TYPE	
	5270	0516	1066		TAD	K240	
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	5272	0520	1437		TAD	1 PH4	
	5273	0521	4114		J 115	198	
	5274	8522	1060		THO	K316	
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	5285	0532 8577	6291		CDF	0	
	5386	8574	4162		JMS	CRLF	
	5307	8535	4162		JHS	CRLF	
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	5314	8542	4162		JMS CRLF	an a
-	5315	0543	4162		JMS CRLF	
	5316	0544	4162		JHS CRLF	
	5317	8545	4162		JMS CRLF	
	5320	9546	4162		JMS CRLF	
	5321	9547	5577		JMP I OUTO	ZEXIT
	5322			1 .		
	5323			-	<b>*608</b>	
	5324	0600	0000	OUT1,	8	ZTELETYPE OUT
	5325	0601	3012		DCR 12	
	5326	0602	6046	•	TLS	ZROUTINE
	5327	0603	7300		CLA CLL	
	5330	0604	4162		JMS CRLF	• • • • • • • • • • • • • •
	5331	9695	4162		JHS CRLF	
	5332	8686	7208		CLA	
	5333	. 8687	1972		TAD M12	
	5334	0610	3073		DCA DON	
	5335	9611	7288	HX,	CLR	
	5336	0612	1412		TAD 1 12	
	5337	0517	7440		SZR	
	5348	9614	5220		JMP . +4	
	5341	9615	4162		JMS CRLF	
	5342	9616	4162		JNS CRLF	•
	5747	9617	5600		JNP I OUT1	
	5344	0620	4114		JNS TYP	
	5345	8621	2973		ISZ DON	
	5346	8622	5227		JMP DB	
	5347	8623	4162		JMS CRLF	
	5359	8624	7288		CLR	·
	5251	9625	1972		TRD M12	•
	5252	8626	3973		DCA DON	
	5252	8627	4101	DB.	JHS KEY	
	5754		7449	5.5.	528	
anda alfi i "	5355	8631	5211		JMP AX	
	5256	8672	1979		TAD K260	
	5357	8633	3074		908 CP	
	5368	8534	4162		JMS CRLF	· · · · · · · · · · · · · · · · · · ·
	5361	8635	4162		JMS CRLF	
	5362	0636	5600		JMP I OUT1	·
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	5364	8637	8999	DUT2,	8	
	5365	0640	3012		DCR 12	
	5366	0641	6046		TLS	
	5367	9642	7300		CLA CLL	
	5379	0643	4162		JMS CRLF	ու ու չու հայտերական հանդեպեսին ենքան պաշտպես բություրացել ու ու չել է այնպեսնացեն ընտրոնացել համանքան գնդելու է է հետ
	5371	0644	4162		JMS CRLF	
	5372	0645	7289		CLA	
	5373	0646	1072		TAD M12	
	5374	0647	3073		DCA DON	
	5375	0659	1076		TRD N175	
	5376	0651	3077		DCA CNT	
	5377	0652	7200	8X2,	CLA	
	5400	0653	1412		TRD I 12	- · · · ·
	5491	8654	4114		JMS TYP	
	5482	0655	2077		15Z CNT	
	5402	9656	5260		JMP .+2	
	5404	8657	5637		JMP 1 OUT2	
•	5405	8669	2073		ISZ DON	
	5486	8661	5266		JMP DE2	
	5407	8662	4162		JMS CRLF	
	5410	9002	7288		CLA	
	5411	8664 8664	1972		TAD M12	
	-	0004	2 V I E			
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	5443		9665	7877		<b>DC8 DON</b>	an a
	5412 5413		<del>0</del> 666	4101	DB2,	JHS KEY	, , , , , , , , , , , , , , , , , , ,
	5414		9667	7440		SZA	
. :	5415		0670	5252		JNP AX2	
	5416		0671	1070		1HD K260	
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	5424		0676	6046	<b>.</b>		
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	5430		0702	7200		CLA	
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:	5432		0704	3073		DCA DON	
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1	3433 5436		8718	5717		JMP +3	<ul> <li>Колиский с Поладилары украсно столика, налада сайско сара констранта 2 к.н. наказания на паланарально и бало за кара на акто констранции и полькования и полькования и палана сара констранта 2 к.н. наказания на паланарально и бало за кара на кара на кара</li> </ul>
Ì	5432		0711	4162		JMS CRLF	
	5440		0712	5674		JHP I OUT3	
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5	5442		0714	1066		TAD K240	/SPHCE
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	5446		0720	2973	•	ISZ DON	
	5447		0721	5305		JMP AX3	
;	5450		0722	4162		JH5 CRLF	
-	5451		0723	7200	1	CLA Top No	
-	5452		0724	1071		180 NZ	
	3433 5454		0725 8726	4101		JMS KEY	
	5455		0727	7440		SZA	
1	5456		0730	5305		JHP AX3	
1	5457		0731	1978		TAD K260	
-	5469		0732	3074		DCR CP	
	5461		8733	4162 5674		JHS CKLF	ւ չ չ՝ չ՝ չունի չափերիները, տարերը հարությունը հետ է հետությունը։ Աներան հարձապես հետությունը հետությունը է հետ Դուսի է չ՝ չունի չափերիները, հարերը հարձակությունը է հետությունը հետությունը հետությունը հետությունը է հետությունը է չ
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	5467	· ·	0024 0025	8637 0774	102,	0012	
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	5581		0030	5779	РИЗ,	НЗ	
	5592		0037	5771	PH4,	И4	
1	5593		8049	5772	PT1,	T1 .	
1	5594		8941	5773	PT2,	T2	
	5505		0042	9777	K777,	777	
	5596		0043 0044	2000	K2000, K7777.	2000 3777	
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5512	0047	7777	K7777,	7777		
5513	0050	0391	K301,	301	2 <b>R</b>	
5514	0051	0304	K304,	394		
5515	8852	0305	K303,	202	75	
5516	8823	0240	K2001	740	2 F	
5517	0034	0711	N310)	310	21	
JJ20 5524	0055	0311	K311/	714	21	· -
5522	9957	0314	K315.	315	21	
5522	9950	0310 0316	K316.	316	2N	
5524	8861	0317	K317,	317	10	
5525	0062	0322	K322,	322	2R	
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5530	0065	0326	K326,	326	<b>/ Y</b>	
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Name of Contraction of Contraction

\*L L, \$CALC2, 8 ... \*₩ C FOCAL-12 . . . . . 01.10 L 0, F1, U, #0, 1 81. 20 A !!, "FDP", PF, "LDP", PL 01.30 F DF=PF, FL; D 2 01. 40 T 11; L C, F1; Q 02.10 5 J=(DP+5+4)+256+221 02.20 5 MI=F1(J+11);5 D=F1(J+8)-MI 02.30 5 K5=.5\*D+H1;5 K7=.3\*D+H1;5 K9=.1\*D+N1 02.40 D 4 82.50 D 6 04.10 5 K=0; 5 T=0; 5 J=DP\*5\*256; 5 L=K5; D 5 04.20 5 T5=D; 5 N5=N; 5 L=K7; D 5 04.30 5 17=0; 5 N7=N; 5 L=K9; 0 5 04.40 5 T9=D; S N9=N; S L=MI; D 5 04.50 5 T1=D; 5 N1=N 85.10 I (F1(J+K)-L)5.3,5.3,5.2 05.20 5 T=T+F1(J+K); 5 K=K+1; 6 5.1 05.30 5 M=(F1(J+K)-F1(J+K-1))/F1(J+K) 05.40 S D=T+(L-F1(J+K-1))/H 05.50 5 N=K-(F1(J+K-1)-L)/(F1(J+K)-F1(J+K-1)) 06.10 5 J=(DF\*5+4)\*256+221 06.20 5 F1(J+21)=T5/10+.5;5 F1(J+22)=T7/10+.5 06.30 5 F1(J+23)=T9/10+.5; 5 F1(J+24)=T1/10+.5 06, 40 5 F1(J+25)=N5\*18+. 5; 5 F1(J+26)=N7\*10+. 5 05.50 5 F1(J+27)=N9\*10+.5;5 F1(J+28)=N1\*18+.5 06.60 5 D=F1(J+1)/100;5 F1(J+29)=T5/D+.5 06.70 5 F1(J+30)=T7/0+.5;5 F1(J+31)=T9/D+.5 86.88 5 F1(J+32)=T1/D+.5 \* . . . - -٩.

+L L, \$READ, 0 \*₩ C FOCAL-12 - + 81.10 L 0, F1, U, #9, 1 01.20 A !!, "TAPE", T, "FDP", PF, "LDP", PL 01.30 F DP=PF, PL; D 2 01. 40 D 2. 05; T %8. 04; L C, F1; Q 02.05 5 J=(DP\*5+4)\*256+221; F I=1,31; T " \*, ! T %3, "DATA POINT", DP+(T-1)+100 02.10 02.15 T !!, %11, "TL", F1(J+1), !, "CT", F1(J+2)\*18 02.20 T !, 210.01, "RR", F1(J+3)/10, !, 211, "NT", F1(J+4) 02.25 T !, %10.01, "ST", F1(J+5)/10, !, "SD", F1(J+6)/18 : !, %11.02, "5E", F1(J+7)/100, !, %10.01, "FI", F1(J+8)/10 02,30 T !, "5D", F1(J+9)/18, !, %11.02, "5E", F1(J+18)/188 92:35 T 02.40 T !, %10.01, "HI", F1(J+11)/10, !, %10, "FMN", F1(J+12) 02.45 T !, "H5N", F1(J+13), !, 29.01, "MEN", F1(J+14)/10 !, "MED", F1(J+15)/10, !, "MOD", F1(J+16)/10 02.50 T 02.55 T !, %10, "HON", F1(J+17), !, %11, "PL", F1(J+18) \*.-F1(J+28)/188 1, %10.01, "LI", F1(J+19)/10, 1, %4.02, "SL 02.60 T 1, %10, "T50", F1(J+21), 1, "T70", F1(J+22) 02.65 T 1, "T90", F1(J+23), 1, 29. 0, "T100", F1(J+24) 02.70 T !, %5. 01, "N50", F1(J+25)/10, !, "N70", F1(J+26)/18 62.75 T !, "N90", F1(J+27)/10, !, %8. 01, "N100", F1(J+28)/10 02.80 T 1, %9. 01, "T5P", F1(J+29)/10, 1, "T7P", F1(J+30)/10 02.85 Т 02.90 T !, "T9P", F1(J+31)/10, !, %8.01, "T10P", F1(J+32)/10 02.95 T !,%9.01,"FLP",F1(J+33)/10,!,"TLP",F1(J+34)/10 \* t t

369 \*L.L, \$50H1, 0 \*# C FOCAL-12 01.10 L D, F1, U, #0, 1 01. 20 A "TAPE", T, "FDP", PF, "LDP", PL SD\* ST 01.30 T !!." DP 01.40 T " SE NT RR M1\* SE 5E FI SÐ 01.50 F DP=PF, PL; D 2 81.60 T !!, 28.04; L C, F1; Q 02.10 5 J=(DP\*5+4)\*256+221 02.20 T !, %3, DF+(T-1)\*100 02.30 T %6.01, F1(J+3)/10, %7, F1(J+4), %6.01, F1(J+5)/10 02.40 T F1(J+6)/10,%6.02,F1(J+7)/100,%6.01,F1(J+8)/10 02: 50 T F1(J+9)/10, %6. 02, F1(J+10)/100, %6. 01, F1(J+11)/18 \* \*L L.\$50H2.0 \*N C FOCAL-12 01.10 L 0, F1, U, #0, 1 01.20 A "TAPE", T, "FDP", PF, "LDP", PL MED" 01.30 T !!," 01.40 T " HSN MEN FHN DP LI" FL MON HOD 01.50 F DP=PF, PL; D 2 01.60 T !!, %8.04; L C, F1; Q 02.10 5 J=(DP\*5+4)\*256+221 02.20 T 1,23,DP+(T-1)\*100 02.30 T %7, F1(J+12), F1(J+13), %6.01, F1(J+14)/18 82.48 T F1(J+15)/18,F1(J+16)/18,%7,F1(J+17) 02.50 T F1(J+18),26.01,F1(J+19)/10 ×.

+L L, \$50M3, 0 \*₩ C FOCAL-12 01. 10 L 0, F1, U, #0, 1 81. 20 A "TAPE", T, "FDP", PF, "LDP", PL !!." DP SL T50 170 T90" 01.30 T N180\* 01.40 T " T100 N90 N50 N70 01. 50 F DP=PF, PL; D 2 01.60 T 11,28.04; L C, F1; Q 02.10 5 J=(DP\*5+4)\*256+221 02.20 T !, %3, DP+(T-1)\*100, " . 02.30 T %3.02, -F1(J+20)/100, %7, F1(J+21), F1(J+22) 82.48 T F1(J+23), F1(J+24), %6.81, F1(J+25)/18 02.50 T F1(J+26)/10,F1(J+27)/10,F1(J+28)/10 \* \*L L, \$5UN4, 8 \*N C FOCAL-12 . . . 01.10 L 0,F1,U,#0,1 01. 20 A "TAPE", T, "FDP", FF, "LDP", PL 01. 30 T !!," DP TL CT CT ..... T5P 01.30 T !!," DP 01.40 T " T9P T7P\* T9P TLP\* T10P PLP 01.59 F DP=PF, PL; D 2 01.60 T 11,28.04; L C, F1; Q 02.10 5 J=(DP\*5+4)\*256+221 . 02.20 T 1,%3,DP+(T-1)\*100 02.30 T %7,F1(J+1),F1(J+2)\*10,%6.01,F1(J+29)/10,F1(J+30)/10 02.40 T F1(J+31)/10,F1(J+32)/10,F1(J+33)/10,F1(J+34)/10 \* ŧ

. . . . . \*L L, \$REORD, 0 .... +₩ C FOCAL-12 and the second · • • . 01.10 L 0, F0, U, #0, 0 01.20 A !!, "TAPE", T, "FDP", PF, "LDP", PL; S T=(T-1)\*100 81.30 D 2 01. 40 F R=1, 34; 5 L=R\*1000; F DP=PF, PL; D 3 01. 50 T !!:L C.F0:Q 82.10 5 A(1)=2;5 A(2)=21;5 A(3)=22;5 A(4)=23 02.20 5 A(5)=24;5 A(6)=18;5 A(7)=1;5 A(8)=3 02.30 5 A(9)=5;5 A(10)=8;5 A(11)=11;5 A(12)=19 02.40 5 A(13)=14;5 A(14)=15;5 A(15)=16;5 A(16)=25 . 02.50 5 8(17)=26;5 8(18)=27;5 8(19)=28;5 8(20)=29 \_\_\_\_\_ 02.60 5 A(21)=30;5 A(22)=31;5 A(23)=32;5 A(24)=33 02.70 5 A(25)=34; 5 A(26)=20; 5 A(27)=7; 5 A(28)=10 02.80 5 A(29)=6;5 A(30)=9;5 A(31)=4;5 A(32)=12 02.90 5 A(33)=13;5 A(34)=17 03.10 L 0.F1.U.#0.1 -----83.20 5 J=(0F\*5+4)\*256+221 03.30 5 F1(L+DP+T)=F0(J+A(R)) . 03.40 L C.F1 \* and a subset of a second second second second second second second and second s ٩. ţ

+L L, \$IVD, 0 \_\_\_\_\_ ≠N C FOCAL-12 -. . . . . 01.10 L 0, F0, U, #9, 0 . . . . . . . . . 01.20 F J=1,34;5 N=0;5 L=J\*1000;F K=1,50;5 N=N+1;D 2;D 3 a second a s 01.30 T !!!;L C F0;Q 02.10 I (N-2)2.2,2.15,2.2 02.15 5 N=N+41; R 82, 28 I (N-58)2. 3, 2. 25, 2. 3 the state of the state of the matter of the state of the 82. 25 5 N=N+32; R 02.30 I (N-85)2.4,2.35,2.4 02.35 5 N=N+10; R 82, 49 I (N-112)2, 5, 2, 45, 2, 5 02.45 5 N=N+6; R 02.50 I (N-120)2.6,2.55,2.6 02.55 5 N=N+11; R (N-148)2. 7, 2. 65, 2. 7 82.60 I ----02.65 5 N=N+37; R 82,78 I (N-179)2.8,2.75,2.8 02.75 5 N=N+11; R 02, 80 I (N-191)2, 9, 2, 85, 2, 9 02.85 5 N=N+7 02.90 R 03.10 L 0, F1, U, #0, 1 and a second state of the 03.20 5 F1(L+K)=F0(L+N) 03.30 L C.F1 \* \_\_\_\_\_ and an and a second . . . . . . . . . . . 

ί.

..... . . ... ... +L L, \$IVI, 0 ... \*N سائد دامان C FOCAL-12 . . . 01.10 L 0, F0, U,#0,0 01. 20 F J=1, 34; 5 H=0; 5 L=J\*1000; F K=1, 175; 5 N=N+1; D 2; D 3 01. 30 T !!!; L C, F0; Q .... 02, 05 I (N-1)2, 15, 2, 1, 2, 15 and the second 02.10 5 N=N+1; R 02.15 I (N-43)2.25,2.2,2.25 a construction of the second of the second s 02. 20 5 N=N+7; R ner a ser se ser se se se se se se anno a se a anno assessa de se sa santa a santa a anno se se se sa sa sa an 82.25 I (N-82)2.35,2.3,2.35 02. 30 5 -N=N+3; R 82.35 I (N-95)2.45,2.4,2.45 02.40 5 N=N+17; R 02.45 I (N-118)2.55,2.5,2.55 02. 50 5 N=N+2; R 82.55 I (N-131)2.65,2.6,2.65 02.60 5 N=N+9; R 02.65 I (N-177)2.75,2.7,2.75 82.78 5 N=N+2; R (N-190)2.85,2.8,2.85 82.75 I 02.80 5 N=N+1; R 82. 85 I (N-198)2. 95, 2. 9, 2. 95 02.90 5 N=N+8 82.95 R a a se a construction e el construction de la construction de la constructión de la construction de 03.10 L D, E1, U, #0, 1 03.20 5 F1(L+K)=F0(L+N) 03.30 L C.F1 \* and and a second provide the second ..... . . . . . . . . . an and a manager second data to a survey second المراجعة ومرورون ووالمراجعين المتعوم والمرور الإراري الروار ١

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\*L L, \$EV0, 0 ÷H C FOCAL-12 01. 10 L 0, F0, U, #0, 0 01. 20 F J=1, 34; 5 N=0; 5 L=J+1000; F K=1, 3; 5 N=N+1; D 2; D 3 01. 30 T !!!; L C, F0; Q ...... -----02.10 I (N-1>2.3,2.2,2.3 02.20 5 N=N+19; R 82.30 I (N-21)2.5,2.4,2.5 a a company of a second company of the second company of the second company 02.40 5 N=N+45; R 02.50 I (N-67)2.7,2.5,2.7 02.60 5 N=N+15 82.78 R 03.10 L D, F1, U, #0, 1 83.20 5 F1(L+K)=F0(L+N) 03.30 L C, F1 ..... \_\_\_\_ +L L. \$EVI, 0 \*1 C FOCAL-12 31 01. 10 L D, F0, U, #0, 0 01. 20 F J=1, 34; 5 N=0; 5 L=J\*1000; F K=1, 105; 5 N=N+1; D 2; D 3 01. 30 T !!!;L C, F0; Q 02.10 I (N~29)2.3,2.2,2.3 02.20 5 N=N+1; R 02.30 I (N-66)2.5,2.4,2.5 02.40 5 N=N+1; R 02.58 I (N-82)2.7.2.6.2.7 02.69 5 N=N+1 02.70 R and a construction of the second s 03. 10 L 0, F1, U, #0, 1 the state of the s 03.20 5 F1(L+K)=F0(L+N) 03.30 L C.F1 \*

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<pre>*L L. \$RDHM. 8 *N C FOCAL-12 1.19 L 0, F1. U, #0.1 1.20 A 11, FC*, CF *LC*, CL DL 20 F U+CF, CL: 0 2: D 3: D 4 21.49 T 113 L C, F1.4 22.45 L 2, L5, 2.2 23.45 L 2, L5, 2.2 24.45 L 2, L5, 2.2 25.45 L 2, L5, 2.5 25.45 L 2, L5, 2, L5, 2.5 25.45 L 2, L5, 2, L5,</pre>						
<pre>+L L.\$FDOMH.8 +H C FOCRL-12 81.10 L 0, F1.U, #0.1 20 R 11.*FC*.CC, FL*.C*, CL 91.30 F U=CF.CL:D 2:D 3:D 4 21.45 5 D = 1.6 22.45 5 D = 1.6 22.45 5 D = 1.6 22.55 D = 1.6 23.55 C 1=0.5 C 2=0.5 H=0 23.55 C 1=0.5 C 1=0.5 C 2=0.5 H=0 23.55 C 1=0.7 S C 2=0.5 H=0 23.55 S H=X 23.55 D = 1.6 23.55 C 1=0.7 S C 2=0.5 H=0 23.55 S H=X 24.55 D = 1.6 24.55 D = 1.6 25.55 D = 1.6 25.55</pre>					· · · · · · · · · · · · · · · · · · ·	
*L L.\$RDAH.0 H CODEL-12 31.10 L D.F.J., H&D.1 31.20 R U.F.F.Y.CF.*(C.*, CL 31.20 R U.F.F.Y.CF.*(C.*, CL 31.20 R U.F.F.Y.CF.*(C.*, CL 31.20 R U.F.F.Y.CF.*(C.*, CL 31.20 R U.F.F.Y.CF.*(C.*, CL 31.40 T U.F.Y.C, F.F.Y.C.*, CL 32.40 I (U.F.Y.2, 25.2, 25.2, 2 32.25 S D=1.R 32.30 I (U.F.Y.2, 25.2, 25.2, 2 32.35 D=1.R 32.35 D=1.R 32.35 D=1.R 32.35 D=1.R 32.35 D=1.R 32.40 I (U.F.Y.2, 25.2, 25.2, 2 32.41 U.F.Y.2, 25.2, 25.2, 2 32.45 S D=1.R 32.50 S D=1.R 32.50 S D=1.R 32.50 S D=1.R 33.10 S H=0.1S C1=0.5 C2=0.5 H=0 33.20 S K=1(K+N)/D 33.51 (X), 4, 3, 7, 3, 4 33.51 (X), 4, 3, 7, 3, 4 33.75 S L=N 33.75 S L=N 34.15 T L!!!!!!!!!!!!!!!!!!!!!!!!!!!!!!!!!!!		t i mari		·	a an	e e
<pre>** ** ** ** ** ** ** ** ** ** ** ** **</pre>	+LL,\$	RDNN, Ø				
<pre>81.10 L 0, F1.U, H0.1 91.20 A 11, FC*, CF, FLC*, CL 91.20 F U=CF, CL, D 2:D 3:D 4 91.30 F U=CF, CL, D 2:D 3:D 4 91.40 T 111, L C, F1:0 92.15 D=1.1; 82.15 D=1.1; 82.25 D=1.2; 82.25 D=1.1; 82.25 D=1.2; 82.25 D=1.1; 82.25 D=1.2; 82.25 D=1; 82.25 D=1; 82.25 D=1; 82.25 D=1; 82.</pre>	+N C FOCA	-12				
<pre>01. 10 L 0. F1. 0. #0.1 01. 20 F 11. F1. F1. F1. 0 01. 00 F 11. L 0. F1.0 02. 10 T (U-1). 15. 2. 15. 2. 2 02. 15 5 D= 1. R 02. 20 T (U-7)2. 25. 2. 25. 2. 3 02. 25 5 D=1. R 02. 30 T (U-25)2. 35. 2. 35. 2. 4 02. 35 5 D=10. R 02. 40 T (U-23)2. 45. 2. 45. 2. 5 02. 45 5 D=10. R 02. 40 T (U-30)2. 55. 2. 55. 2. 6 02. 55 5 D=10. R 02. 60 5 D=1 03. 10 5 H=0.5 C1=0.5 C2=0.5 H=0 03. 20 5 K=U-1000+1.5 L=T1(K)/D 03. 30 5 K=14(K+N)/D 03. 35 T (X)2. 4. 3. 7. 3. 4 03. 40 T (X-1)3. 45. 35. 4. 5 04. 50 F (X-K)/D (X-K)/D 04. 10 T (11. X2*ROM*, U, 11. X8. 04. "HEAN ", H.1. *5D ", SD 04. 30 T (. "SDF STT(X). 1. "RANGE", H-L 04. 30 T (. "LON ", L, 1. "KIGH ", H</pre>			· · ·	• • • • •	··· ·· · · · ·	······
01.20 F U=CF, CL: D 2:D 3:D 4 01.40 T !!!:L C, FI:0 02.10 I (U=1).15:2.15:2.2 02.15 S D=.1.R 02.20 S U=-72.25:2.25:2.2 02.25 S D=1:1 02.30 I (U=25)2.25:2.25:2.2 02.40 I (U=25)2.45:2.45:2.5 02.45 S D=10:R 02.50 I (U=25)2.45:2.55:2.55:2.6 02.55 S D=10:R 02.60 S D=1 03.10 S N=0:S C1=0:S C2=0; S N=0 03.20 S K=U=1000+1:S L=F1(K)/D 03.30 S X=F1(X=N)/D 03.30 S X=F1(X=N)/D 03.40 I (X=L)3:45:3.5:3.5 03.40 I (X=L)3:45:3.5:3.5 03.40 I (X=L)3:45:3.5:3.5 03.60 S N=N=1:5 C1=0:4X:S C2=C2+X*2:0 3.3 03.70 S M=C1/N:S SD=FSDT((C2=C1*2/N)/(N=1)) 04.10 T !!!!,X3**R0N*,U,!!:X8:04:*MEAN *,H.+L 04.30 T !;*L0M *,L:!:XEIGH *:H +	01.10 01.20	_ U,F1,0,#0,1 A !!,"FC",CF,"LC",CL				
D: 40 1 :::::::::::::::::::::::::::::::::	01. 30 .	U=CF, CL; D 2; D 3; D 4			a e menuna de la marcia de anas	
02.10 I (U-1), 15, 2.15, 2.2 02.15 5 D = 1, R 02.25 5 D = 1, R 02.25 5 D = 1, R 02.25 5 D = 1, R 02.35 5 D = 1, R 02.35 5 D = 1, R 02.45 5 D = 1, R 02.45 5 D = 1, R 02.45 5 D = 1, R 02.55 5 D = 1, R 02.55 5 D = 1, R 02.55 5 D = 1, R 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 03.20 5 K = 1, C + 1, 5 C = 2, 5 H = 0 04.20 T : 1, *5 L = 7, 5 D + 5, 0 C + 0, * (R + R + ", H, I, *5 D *, 5 D + 5, 5 D + 1, 5 D	81.40	I III UFTIG				
<pre>e2 29 7 (U-7)2 25, 2 25, 2 25, 2 3 e2 25 5 D=1; R e3 20 7 (U-7)2 25, 2 35, 2 35, 2 4 e3 35 D=10; R e3 40 (U-25)2, 45, 2 45, 2 5 e4 40 (U-25)2, 45, 2 45, 2 5 e4 40 (U-25)2, 45, 2 45, 2 5 e4 40 (U-25)2, 45, 2 5, 2 55, 2 6 e4 55 D=1 e4 10 (U-25)2, 55, 2 55, 2 6 e4 55 D=1 e4 10 (U-25)2, 4 5, 2 6 e4 10 (U-25)2, 4 7 e4 10 (U-25)</pre>	02.10 02.15	( (U-1), 15, 2, 15, 2, 2 5 D= 1; R		• .		
<pre>02.25 5 D=1;R 02.36 I (U=25)2,25,2.35,2.4 02.46 I (U=23)2,45,2.45,2.5 02.46 I (U=23)2,45,2.55,2.6 02.56 I (U=30)2,55,2.55,2.6 02.55 D=10;R 02.66 S D=1 03.10 S N=0;S C1=0;S C2=0;S N=0 03.20 S K=D+1000+1;S L=F1(K)/D 03.35 I (X)3,4,3.7,3.4 03.46 I (X=1,3,45,3.5,3.5 03.55 S L=X 03.55 S L=X 03.56 I (N=X)3,45,3.5,3.5 03.55 S H=X 03.66 S N=N+1;S C1=C1+X;S C2=C2+X^2;6.3.3 03.67 S M=C1/N;S SD=FSDT(CC2-C12/N)/(N-1)) 04.10 T !!!!,Z3*R0N*,U,!!,Z0.04,*MERE*,H=L 04.30 T !,*L0N *,L.!,*HIGH *,H</pre>	82. 20	( (U-7)2. 25, 2. 25, 2. 3		•		
02 35 5 0=10;R 02 40 1 (U-33)2,45,2,45,2,5 02 45 5 0=10;R 02 55 1 (U-30)2,55,2,55,2,6 02 55 5 0=10;R 03 20 5 K=U=1000+1;5 L=F1(K)/D 03 30 5 X=F1(K+N)/D 03 35 1 (X)2,4,3,7,3,4 03 45 1 (X-L)3,45,3,5,3,5 03 45 1 (X+N)3,55,3,6,3,6 03 55 5 H=X 03 50 1 (H+X)3,55,3,6,3,6 03 55 5 H=X 03 60 5 N=+1+1;5 C1=C1+X;5 C2=D2+X^2;6 3,3 03 70 5 M=C1/N:5 SD=F507(C2-C12/N)/(N-L)) 04 10 7 !!!!,X2=RON",U,!!,X6,04,*MERN ",M.!,*SD *,SD 04 20 T !,*SE ",SD/F507(C2-C12/N)/(N-L) 04 10 T !!!L0N ",L,!,*KIGH ",H *	02.25 02.30	; D=1; R [ (U-25)2, 35, 2, 35, 2, 4				
<pre>be. 4b 1 (U-20/2. 43, 2. 45, 2. 5 22. 55 0 = 10; K 62. 55 5 D = 10; K 63. 10 5 K = U + 1000 + 1; 5 L = F1(K)/D 63. 30 5 X = F1(K+N)/D 63. 30 5 X = F1(K+N)/D 63. 30 5 X = 11(K+N)/D 63. 40 1 (X-L)3. 45. 3. 5, 3. 5 63. 45 5 L = K 63. 55 5 H = K 63. 60 S N = N+1; 5 C1 = C1+K; 5 C2 = C2+K^2; 6 3. 3 63. 60 S N = N+1; 5 C1 = C1+K; 5 C2 = C2+K^2; 6 3. 3 63. 70 5 M = C1/N; 5 SD = FSQT((C2-C1^2/N)/(N-1)) 64. 10 T !!!!, X3*RON*, U, !!, X8. 04, *MERN *, M. !, *SD 64. 20 T !, *SE *, SD/FSQT(K), !, *RNDE*, H-L 64. 30 T !, *LOM *, L. !, *KIGH *, H *</pre>	02:35	5 D=10; R				······································
02.50 I (U-3D)2.55.2.55,2.6 02.55 D=10.R 03.05 X=0v4D00+1.5 L=F1(K)/D 03.30 S X=F1(X+N)/D 03.30 S X=F1(X+N)/D 03.35 I (X+)3.5,3.5,3.5 03.40 I (X+L)3.45,3.5,3.5 03.50 I (X+L)3.55,3.6,3.6 03.50 I (H+X)3.55,3.6,3.6 03.50 I (H+X)3.5D=F50T((C2-C1*2/N)/(N+1)) 04.10 T !!!!,Z3*R0N*,U,!!,Z8.04.*MERN *,M.!,*5D *,5D 04.20 T !.*5E *,5D/F50T(X).!,*RANGE*,H-L 04.30 T !.*LOH *,L!.*NIGH *,H *	02.40 02.45	; (0-28)2, 45, 2, 45, 2, 5 5 D=109; R				
02.60 5 D=1 03.10 5 H=0; 5 C1=0; 5 C2=0; 5 H=0 03.20 5 K=U+1090+1; 5 L=F1(K)/D 03.30 5 X=F1(K+N)/D 03.35 5 X=F1(K+N)/D 03.35 5 L=X 03.55 5 L=X 03.55 5 H=X 03.60 5 H=N+1; 5 C1=C1+X; 5 C2=C2+X^2; 6 3.3 03.70 5 M=C1/N; 5 SD=F5QT((C2-C1^2/N)/(N-1)) 04.10 T !!!!, X3*RON*,U, !!, X8.04, *MERN *, H, !, *SD *, SD 04.20 T !, *SL *, SD(K), !; *RANGE*, H=L 04.30 T !, *LOH *, L, !, *RIGH *, H *	02.50 02.55	(U-30)2.55,2.55,2.6				
03 10 5 N=0; 5 C1=0; 5 C2=0; 5 H=0 03 20 5 K=0+1000+1; 5 L=F1(K)/D 03 35 1 (K>3, 4; 7, 7, 3, 4 03 40 1 (X+L)3, 45, 3, 5, 3, 5 03 55 5 L=X 03 55 5 L=X 03 55 5 H=X 03 60 5 N=N+1; 5 C1=C1+X; 5 C2=C2+X^2; 6 3, 3 03 70 5 M=C1/N; 5 SD=FSRT(C2=C1^2/N)/(N-1)) 04 10 T !!!!, X3*RON*, U, !!, X8, 04, *MEAN *, M, !, *SD *, SD 04.20 T !. *SE *, SD/FSRT(N), !; *RANGE*, H-L 04 30 T !, *LDH *, L, !, *KIGH *, H *	02.60	5 D=1		Concerning and a concern of the second second second		-
03:20 5 K=U+1000+1;5 L=F1(K)/D 03:35 X=F1(K+N)/D 03:35 1 (X)3, 4; 3, 7, 3, 4 03:40 1 (X+L)3, 45; 3, 5, 3, 6 03:55 L=X 03:60 5 N=N+1;5 C1=C1+X;5 C2=C2+X^2;6 3, 3 03:70 5 N=C1/N;5 SD=F5RT((C2-C1^2/N)/(N-1)) 04:10 T !!!!,X3*RON*,U, !!,X8.04, *MEAN *, M, !, *SD 04:20 T !.*SE *.SD/FSRT(N);!*RHNGE*,H+L 04:30 T !.*LON *,L,!,*RHNGH*,H *	A7 10	5 N=A: 5 C1=A: 5 C2=A: 5 H			· · ·	
03.35 5 X=F1(K+N)/D 03.35 1 (X)2, 4, 3, 7, 3, 4 03.40 1 (X+L)3, 45, 3, 5, 3, 5 03.45 5 L=X 03.50 1 (H+X)3, 55, 3, 6, 3, 6 03.50 5 N=N+1;5 C1=C1+X;5 C2=C2+X^2;6 3, 3 03.70 5 N=C1/N;5 SD=F5BT((C2-C1^2/N)/(N-1)) 04.10 T !!!!, Z3*RON*, U, !!, Z8, 04, *MERN *, M, !, *SD 04.20 T !, *SE *, SD/FSBT(N), !, *RANGE*, H-L 04.30 T !, *LOW *, L, !, *RIGH *, H *	03.20	5 K=U*1000+1;5 L=F1(K)/	>			
03 40 I (X-L)3. 45,3.5,3.5 03 45 S L=x 03 55 I (H-X)3. 55,3.6,3.6 03 55 S H=X 03 60 S N=N+1;5 C1=C1+X; S C2=C2+X^2; G 3.3 03 70 S M=C1/N; S SD=FSQT((C2-C1^2/N)/(N-1)) 04 10 T !!!,X3"RON",U,!!,X8.04. "MEAN ",H,!,*5D *,SD 04 20 T !, "SE ",SD/FSRT(N),!, "RANGE",H-L 04 30 T !, "LDN ",L,!, "KIGH ",H *	03.30 07.35	; X=F1(K+N)/D ( (X)% 4.% 7.% 4				
03.50 I (H-X)3.55,3.6,3.6 03.55 S H=X 03.60 S N=N+1; S C1=C1+X; S C2=C2+X^2; G 3.3 03.70 S M=C1/N; S SD=FSQT((C2-C1^2/N)/(N-1)) 04.10 T !!!!, X3"RON", U, !!, X8.04, "MERN ", M, !, "SD ", SD 04.20 T !, "SE ", SD/FSRT(N). !, "RANGE", H-L 04.30 T !, "LON ", L, !, "NIGH ", H * *	03.40	(X-L)3. 45, 3. 5, 3. 5	n a serie namena notre a la declara de analisman	and a second		
03.55 5 H=X 03.60 5 H=N+1;5 C1=C1+X;5 C2=C2+X*2;6 3.3 03.70 5 H=C1/N;5 SD=F5&T((C2-C1*2/N)/(N-1)) 04.10 T !!!!,Z3*RON",U,!!,Z8.04,*MERN *,H.!,*SD *,SD 04.20 T !,*SE *,SD/F5RT(N):!,*RANGE*,H-L 04.30 T !,*LDH *,L,!,*NIGH *,H *	03.45 03.50	i L=X (H-X)3,55,3,6,3,6				
03.60 \$ M=M+1; \$ C1=C1+X; \$ C2=C2+X"2; 6 3.3 03.70 \$ M=C1/N; \$ SD=FSDT((C2-C1-2/N)/(N-1)) 04.10 T !!!!, X3*RON*, U, !!, X8.04, *MERN *, M, !, *SD *, SD 04.20 T !, *SE *, SD/FSQT(N), !, *RANGE*, H-L 04.30 T !, *LOH *, L, !, *RIGH *, H *	<b>0</b> 3.55	H=X				
04.10 T !!!!, 23 "RON", U, !!, 28.04. "MERN ", H, !, "SD ", SD 04.20 T !, "SE ", SD/FSRT(N), !, "RANGE", H-L 04.30 T !, "LOH ", L, !, "NIGH ", H *	03.60 03.70	; N=N+1;5 C1=C1+X;5 C2=0 ; M=C1/N;5 SD=F5QT((C2-	;2+X^2;6_3.3 ;1^2/N)/(N-1);			
04.20 T !,";S ",SD/FSGT(A)!, "RANGE", H-L 04.30 T !, "LOH ",L.!, "KIGH ",H *	04 40					
04.30 T !, "LON ", L, !, "KIGH ", H	04.20	1,"SE ",SD/FSRT(N),	,"RANGE",H-L	3 30 30		
	04.30 *	' !,"LON ",L,!,"KIGH ".	н			
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\*L L, \$RLIN, 0 \*H C FOCAL-12 .... 01.10 L D, F1, U, #0, 1 01. 20 A !!, "FC", CF, "LC", CL 01.30 F U=CF, CL; D 2 01. 40 D 5; T 28. 04; L C, F1; Q 02.19 D 5 a second a second s 02, 20 F V=1, 13; D 3 02.30 D 5 82.40 F V=14,26;0 3 . \_\_\_\_\_ 03.10 5 A=U; D 6 03.20 5 XD=D 03.30 5 A=V; D 6 03.40 5 YD=D 03.50 D 4 04. 10 5 N=9; 5 C1=0; 5 C2=0; 5 C3=0; 5 C4=0; 5 C5=0 04.15 5 XL=U\*1000+1; 5 YL=V\*1000+1 04.20 5 X=F1(XL+N)/XD/5 Y=F1(YL+N)/YD I (X)4.3,4.45,4.3 84.25 04.30 5 N=N+1 04.35 5 C1=C1+X; 5 C2=C2+X^2; 5 C3=C3+Y 04. 40 5 C4=C4+Y^2; 5 C5=C3+X+Y; G 4. 2 84.45 5 DX=02-01-2/N: 5 DY=04-03-2/N 5 NU=C5-C1\*C3/N; 5 R=NU/FSQT(DX\*DY) 84. 50 84.55 5 M=NU/DX; 5 B=(C3-C1\*M)/N 04.60 5 5=0Y-0X+H12/5 E=F5QT(5/(N-2)) 84.65 T !!!, %2. 0, "X", U, " Y", V, %9.04 E\*, E, \* R", R, B", B, " M", M+1000, " 94.70 T " 5", 5, " N", N, " D\*, DX, \* ¥\*, R^2 04.75 T !," \_\_\_\_\_ 05.10 F I=1,14; T " · · · · · 05. 20 T "LINEAR FIT- Y=8+X\*M/1000+E" 06.10 I (R-1)6.2,6.2,6.3 the second second second second is the second se 06.20 5 D=. 1; R 96. 38 I (8-7)6. 4, 6. 4, 6. 5 \_\_\_\_\_\_ 06,40 5 D=1;R 86.50 I (8-25)6.6,6.6,6.7 06.60 5 D=10;R 06.70 5 D=100 . 

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あるがないので

#L L. \$REXP. 0 \*14 C FOCAL-12 . . . 01. 10 L D, F1, U, #8, 1 01.20 A !!, "FC", CF, "LC", CL 01.30 F U=CF, CL; D 2 81. 48 D 5; T %8. 84; L C, F1; Q 02.10 D 5 02.20 F V=1,13; D 3 02.30 D 5 02.40 F.V=14,26;D 3 83. 18 5 R=U; D 6 03.20 5 XD=D 03.30 5 A=V; D 6 the second se 03. 40 5 YD=D 83.58 D 4 فاستحادهم منام منام المراجع المراجع المراجع 04.10 5 N=0;5 C1=0;5 C2=0;5 C3=0;5 C4=0;5 C5=0 04.15 5 XL=U\*1000+1; 5 YL=V\*1000+1 04.28 5 X=F1(XL+N)/XD; 5 Y=F1(YL+N)/YD 04.25 I (X)4.3,4.45,4.3 04.30 5 Y=FLOG(Y); 5 N=N+1 04.35 5 C1=C1+X; 5 C2=C2+X^2; 5 C3=C3+Y 04.40 5 C4=C4+Y^2; 5 C5=C5+X+Y; 6 4.2 04: 45 5 DX=C2-C1^2/N; 5 DY=C4-C3^2/N 04.50 5 NU=C5-C1\*C3/N; 5 R=NU/FSQT(DX\*DY) . . . . . . . . . . . . . 04.55 5 M=NUZDX; 5 B=(C3-C1\*H)ZN 04.60 5 5=DY-DX+H^2;5 E=FSQT(5/(N-2)) 04.65 T !!!, 22.0, "X", U, " Y", V, 29.04 04.70 T " B", B, " M\*, H\*1000, " E\*, E, " R", R 5", 5, " V", R^2 N", N, " D\*, DX, \* 04.75 T !," 05.10 F I=1,14; T " ", ! 05.20 T "EXPONENTIAL FIT-Y=EXP(6+X\*M/1000+E)" 06.10 I (8-1)6.2,6.2,6.3 06.20 5 D=.1;R 86.38 I (8-7)6.4,6.4,6.5 06,40 5 D=1;R 86.50 I (8-25)6.6,6.6,6.7 86.60 5 D=10;R 06.70 5 D=100 \*

..... \*L L, \$RLDG, 0 \*11 C FOCAL-12 01, 10 L D, F1, U, #0, 1 81. 20 A !!, "FC", CF, "LC", CL 01.30 F U=CF, CL; D 2 01.40 0 5; T 28.04; L C. F1; Q . ...... 02.10 D 5 82.28 F V=1,13; D 3 82.38 D 5 03.10 5 A=U; D 6 03.20 5 XD=D 03.30 5 A=V:D 6 03.40 5 YD=D 03.50 D 4 . . . . 04.10 5 N=0;5 C1=0;5 C2=0;5 C3=0;5 C4=0;5 C5=0 04.15 5 XL=U+1000+1; 5 YL=V+1000+1 04.20 S X=F1(XL+N)/XD; S Y=F1(YL+N)/YD 04.25 I (X)4.3,4.45,4.3 04.30 5 X=FLOG(X);5 N=N+1 04.35 5 C1=C1+X; 5 C2=C2+X^2; 5 C3=C3+Y 04. 40 5 C4=C4+Y^2; 5 C5=C5+X\*Y; 6 4. 2 04.45 5 DX=C2-C1^2/N; 5 DY=C4-C3^2/N 04.50 S NU=C5-C1\*C3/N; S R=NU/FSQT(DX\*DY) 84.55 5 M=NU/DX; 5 B=(C3-C1\*H)/N 04.60 5 5=0Y-0X\*M^2;5 E=FSQT(5/(N-2)) 04.65 T !!!,%2.0, "X",0, " Y",V,%9.04 04.70 T " B",D, " M",M, " E",E, " R",R N\*,N,\* D\*,DX,\* S\*,S,\* Y\*,R^2 84.75 T !." 05.10 F I=1,14; T " ",! Y=B+LN(X)+M+E" ... 05.20 T "LOGARITHMIC FIT-06.10 I (8-1)6.2,6.2,6.3 06.20 5 D=.1; R 86.30 I (A-7)6.4,6.4,6.5 06,40 5 D=1;R 06.50 I (A-25)6.6,6.6,6.7 06.60 5 0=10; R 86.70 5 D=100 \*

- - - - -.. .. .. +L L, \$RLLG, 0 \*N C FOCAL-12 · . . 01.10 L 0, F1, U, #0, 1 81. 28 A !!, "FC", CF, "LC", CL 01.30 F U=CF, CL; D 2 01. 40 D 5; T 28. 04; L C, F1; 0 . . . . . . . . ...... 02.10 D 5 82.20 F V=1,13;D 3 02.30 D 5 02.40 F V=14,26;0 3 د. مربق می است. مربقهای با این است. این است. این است. میشونین میتونین می دون این این این این این این این این این ا 03.10 5 A=U; D 6 03.20 5 XD=D 83.30 5 A=V;D 6 03.40 5 YD=D 03.50 D 4 04.10 5 N=0; 5 C1=0; 5 C2=0; 5 C3=0; 5 C4=0; 5 C5=0 04.15 5 XL=U+1000+1;5 YL=V+1000+1 04.20 5 X=F1(XL+N)/XD;5 Y=F1(YL+N)/YD 04.25 I (X)4.3,4.45,4.3 04.30 5 X=FLOG(X); 5 Y=FLOG(Y); 5 N=N+1 04.35 5 C1=C1+X; 5 C2=C2+X^2; 5 C3=C3+Y 04.40 5 C4=C4+Y^2; 5 C5=C5+X\*Y; 6 4.2 04.45 5 DX=C2-C1 2/N; 5 DY=C4-C3 2/N 04.50 5 NU=C5-C1\*C3/N; S R=NU/FSQT(DX\*DY) 04.55 5 M=NU/DX; 5 B=(C3-C1\*H)/N 04.60 5 5=DY-DX+H^2;5 E=FSQT(5/(N-2)) 04.65 T !!!, %2.0, "X", U, " Y", Y, %9.04 04.70 T " B", B, " M", N\*1000, " E", E, " 04.70 T " B", B, " R", R S", 5, \* D", DX, " ¥", R^2 N", N, " 94.75 T !+ " 05.10 F I=1,14; T " ",! 05.20 T "LOG-LOG FIT-Y=EXF(B+LN(X)\*H/1000+E)" 86.18 I (8-1)6.2.6.2.6.3 06.20 5 D=.1;R 05.30 I (8-7)6.4,6.4,6.5 06.48 5 D=1; R 06.50 I (A-25)6.6.6.6.6.7 85.60 5 D=10; R 06.70 5 D=100 \*

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\*L L, \$REG5D, 0 \*₩ C FOCAL-12 01. 10 A !!, "N1", N1, !, "N2", N2 01.20 A !, "D1", D1, !, "D2", D2 81.30 A !, "51", 51, !, "52", 52 an annual search an annual annual annual a 01. 48 A !, "M1", H1, !, "M2", M2 01.50 5 DF=N1+N2-4;5 5=(51+52)/DF . . . . . 01.60 5 DI=F5QT(5/(D1+D2)) 01.70 5 T=FRB5((H1-H2)/DI) والمستقدم والومين والمراجع المراجع المراجع والمستقلين والمراجع ومراجع والمراجع 02.10 5 C=. 63661977 \_ 82.28 5 D=FSQT(DF) 02.30 5 TH=FATN(T/D); 5 X=DF/(DF+T^2) and a subsection of the second sec 02.40 I (DF-1)2.5,2.5,3.1 02.50 5 A=C\*TH; 6 4.5 the second s 03.10 5 TS=FITR(0F/2);5 TS=2\*TS 03.20 I (DF-T5)3.3,3.3,3.4 03.30 5 IX=1;6 3.5 03.40 5 IX=2 03.50 5 A=1;5 Y=1;5 Z=IX;5 W=Z+1 03.60 I (DF-N)4.1,4.1,3.7 ...03.70 5 Y=X\*Y\*Z/₩ 03.80 5 R=R+Y; 5 Z=Z+2; 5 N=N+2; 6 3.6 . . . . . . . . . . . 04.10 I (2-IX)4.2,4.2,4.4 84. 28 5 N=F5QT(X-X-2) 94.30 5 A=C\*(TH+A\*N); 6 4.5 04.40 5 N=F5QT(1-X);5 A=9\*N 04.50 5 P=1-A 05.10 T !!, "DF=", DF, !, "T= ", T, !, "P= ", P, !!! \*..... the second s جاجامه بدرامر المرعبو ليتورك الرزين والر 1.

سير والالم المواد ومواد ومراد المراد المراد المراد المراد المراد المراد والمحمد المحمد ومرور والمحمد والمراجع المحمد والمحمد والمحمول والمحمد والمحمد والمحمد والمحمد . the second states and second states #L L, \$RSIGD, 0 \*₩ C FOCAL-12 01.10 A !!, "N1", N1, "N2", N2, "R1", R1, "R2", R2 01. 20 5 21=(FL06(1+R1)-FL06(1-R1))/2 01.30 5 Z2=(FLOG(1+R2)-FLOG(1-R2))/2 01.40 5 5=1/(N1-3)+1/(N2-3) 01. 50 5 C=FAB5((Z1-Z2)/FSQT(S)); T !, "C=", C 01.60 D 2 01.70 6 1.1 02.10 I (C-1.959964)2.14,2.17,2.2 N5 P>. 05"; R 02.14 T " 5 P=. 05"; R 02.17 T " 02.20 I (C-2.053749)2.24,2.27,2.3 5 PC. 05"; R 02.24 T " P=, 04"; R 02.27 T " 5 02.30 I (C-2.170090)2.34,2.37,2.4 5 PC. 04"; R 02.34 T " P=. 03";R 02.37 T " 5 (C-2. 326348)2. 44, 2. 47, 2. 5 02.40 I 5 PC. 03"; R . 02.44 T " 02. 58 1 (C-2. 575829)2. 54, 2. 57, 2. 6 5 PK. 02"; R 02.54 T " P=. 01"; R 02.57 T " 5 PC. 01"; R 02.60 T " S \* ... فالمناف مسترابية المتراف مرامل يتوج الممتوعية والرواد والمتعادية ومتراري والمرابع المترار الرواد ----- .. متر المراجع والموسور المراجع مراجع

382 . . . . . . . . +L L, \$PVALR, 0 \*N C FOCAL-12 . . 01.10 A !!, "N", N, !, "R", R 01. 20 5 DF=N-2; 5 D=FSQT(DF) 01\_30 5 T=F5QT(1-R^2);5 T=R\*D/T 02.10 5 C=. 63661977 02.20 5 D=F5QT(DF) 02.30 5 TH=FRTN(T/D); 5 X=DF/(DF+T^2) 02.40 I (DF-1)2.5,2.5,3.1 02.50 5 R=C+TH; G 4.5 nya anya si ya kana manya manya manya manya manya kana anya manya na anya kana manya kana manya manya manya man 03.10 5 T5=FITR(DF/2);5 T5=2\*T5 03. 20 I (DF-T5)3. 3, 3. 3, 3. 4 IX=1;6 3.5 03.30 5 03.40 5 IX=2 03. 50 \$ A=1; 5 Y=1; 5 Z=IX; 5 H=Z+1 03.60 I (DF-W)4. 1, 4. 1, 3. 7 03.70 5 Y=X+Y+2/W 03.80 5 A=R+Y;5 Z=Z+2;5 N=N+2;G 3.6 04.10 I (2-IX)4.2,4.2,4.4 04.20 5 N=F5QT(X-X-2) 04.30 5 A=C\*(TH+R\*N); G 4.5 04.40 5 N=F5QT(1-X); 5 R=R\*N 04.50 5 P=1-R 85.10 T !, "DF=", DF, !, "T= ", T 05. 20 T 1, %10. 10, "P= ", P, %8. 04 05.30 6 1.1 \* . . . . . . . . . . an share a second se

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+L L, \$STTEST, 0 \*H C FOCAL-12 01. 10 5 C1=0; 5 C2=0; 5 R=0 01.20 A !!, "NX", N 01.30 F J=1, N; A !, V; 5 C1=C1+V; 5 C2=C2+V^2 01.40 5 MX=C1/N; 5 K=(C2-C1^2/N)/(N-1); 5 DX=F5QT(K) 01.50 5 EX=DX/FSQT(N);5 DF=N -01.60 D 1.1; A !!, "NY", N; D 1.3 01.70 5 MY=C1/N; 5 K=(C2-C1^2/N)/(N-1); 5 DY=F5QT(K) 01: 80 5 EY=DY/FSQT(N); 5 DF=DF+N-2 01.85 A 11, "PAIRED?", Y/I (Y-25)1.95,1.9,1.95 01. 90 A !, "R", R; S DF=DF/2 01.95 5 T=FAB5((MX-MY)/F5QT(EX^2+EY^2-2\*R\*EX\*EY)) 02.10 5 C=. 63661977 82.28 5 D=F5QT(DF) 02.30 5 TH=FATN(T/D); 5 X=DF/(DF+T^2) 82.40 I (DF-1)2.5,2.5,3.1 02.50 5 A=C+TH; 6 4.5 03.10 5 TS=FITR(DF/2); 5 TS=2\*T5 83. 28 1 (DF-T5)3. 3, 3. 3, 3. 4 93.30 5 1X=1;6 3.5 03.40 5 IX=2 03.50 5 A=1; 5 Y=1; 5 Z=IX; 5 W=Z+1 03:60 I (DF-W)4.1,4.1,3.7 03.70 5 Y=X\*Y\*Z/W 03. 80 5 A=A+Y; 5 Z=Z+2; 5 W=W+2; 6 3. 6 84. 10 I: (2-IX)4. 2, 4. 2, 4. 4 04.20 5 N=FSQT(X-X^2) 04.30 5 A=C\*(TH+A\*N); G 4.5 04.40 5 N=F5QT(1-X);5 R=A\*N 04.50 5 P=1-A 05.10 T !!, "MX=", MX, !, "SD=", DX, !, "SE=", EX 05.20 T !!, "MY=", MY, !, "SD=", DY, !, "SE=", EY 05.30 T !!, "DF=", DF, !, "T= ", T, !, "P= ", P, !!!;@ \* . .

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384 and the second ..... \_+L L, \$TIMFOL, 0 \*H C FOCRL-12 01. 10 5 M=0; 5 D=0; 5 5=0; T 28.02 DIFF" MIN 01.20 T !, "TL 01.30 A !!.L:D 5:5 Z=T:T M.D 01. 40 A !!, L; D 5; 5 H=T-2; 5 D=M-5 01.45 I (L)1.5,1.6,1.5 and the state of the 01. 50 T M, D; 5 5=H; G 1. 4 01.60 T !!!, 28.04; Q 05.15 5 T=(L-8)/10.5; R 05.20 I (L-130)5.25,5.25,5.3 05.25 5 T=(L-10)/10;R 05.30 I (L-206)5.35,5.35,5.4 05.35 5 T=(L-16)/9.5; R ار مستعومها و در این از این است. این مستعومها و در این این این این این میشود میرون میرون میرون این در میروش میرون میرون میرون این و میرود این و 05.40 I (L-278)5.45,5.45,5.5 05.45 5 T=(L-26)/9; R 05.50 I (L-380)5.55,5.55,5.6 the contraction of the second s 05.55 5 T=(L-40)/8.5;R 05, 60 I (L-476)5, 65, 5, 65, 5, 7 05.65 5 T=(L-60)/8,R - 85.78 I (L-596)5.75,5.75,5.8 05.75 5 T=(L-86)/7.5; R 05.80 I (L-708)5,85,5.85,5.95 05.85 5 T=(L-120)/7;R 05.95 5 T=(L-162)/6.5;R and the second sec \* ----. . . •

مراجع المتصرية بستصر التيني and the second second second \*L L, %PLOT, 0 +11 C FOCAL-12 . . 01.10 L D, F0, I, #0, 0 01.15 L D, F1, I, #0,1 81. 28 0 C 01.25 A !!, "PEN DONN", G:S P=0;5 C1=0;5 C2=0;5 T=0 01.30 5 A=FDIS(0,0);5 A=FDIS(0,.68) 01.35 5 A=FDIS(1.02,.68);5 A=FDIS(1.02,0) 01.40 5 A=FDI5(0,0);0 P 01.45 0 C 01.50 5 R=FDI5(0, 34);5 R=FDI5(1.02, 34);0 P 01.55 0 C 01.60 5 A=FDIS(.34,0);5 A=FDIS(.34,.68);0 P 01.65 0 C 01.70 5 A=FDI5(.68,0); 5 A=FDI5(.68,.68); 0 P and the second 01.75 0 C \_\_\_ 01. 80 A "PEN UP", G and a second and a second burger of the second s 02.10 5 P=P+1; 5 C1=FAB5(C1-.34) 02.20 I (P-3)2.4,2.3,2.4 02.30 5 C2=.34;5 T=1 02.40 I (P-5)2.6,2.5,2.6 02.50 5 C2=.68;5 T=0 02.60 I (P-6)3.1,3.1,2.7 and a second sec 02.70 0 R 02.80 T !!!;5 G=F0(0);L C,F0;L C,F1;Q 03.10 T !!!, 22. "PLOT", P. 28.04 03. 20 A 1, "X ROW", XR, 1, "X SCALE", XS 03.30 5 U=XR\*1000;5 D=XR;D 5;5 X5=X5\*D 03.40 A 1, "Y RON", YR, 1, "Y SCALE", YS . . ... 03. 50 5 V=VR\*1000; 5 D=VR; D 5; 5 Y5=Y5\*D 04.10 5 K=0 \_\_\_\_84. 15 5 K=K+1 84, 20 I (T)4, 25, 4, 25, 4. 3 04.25 5 X=F0(U+K);5 Y=F0(V+K);6 4.35 04.30 5 X=F1(U+K);5 Y=F1(V+K) 04.35 I (X)4.4,4.65,4.45 04.40 5 X=X+4096 84. 45 I (Y)4. 5, 4. 65, 4. 55 04.50 5 Y=Y+4096 04.55 5 A=FDIS(C2+X\*.34/X5,C1+Y\*.34/Y5). 04.60 6 4.15 04.65 0 P 04.70 0 C 04.75 6 2.1 ----05.10 I (0-1)5.2,5.2,5.3 05.20 5 D=.1;R 85.30 I (D-7)5.4,5.4,5.5 05.40 5 D=1; R 05.50 I (D-25)5.6,5.6,5.7 05.60 5 D=10;R 05,70 5 D=100 \*

1.

\*L L, %REGP1, 0 +11 C FOCAL-12 1 M ( 1 . . 01.10 A !!!, "PEN DOWN", G 01. 20 5 P=0; 5 C1=0; 5 C2=0 01.30 5 P=P+1; 5 C1=FAB5(C1-.34) 01.40 I (P-3)1.6,1.5,1.6 01. 50 5 C2=. 34 81.60 I (P-5)1.8,1.7,1.8 01.70 5 C2=.68 81, 80 I (P-6)2, 1, 2, 1, 1, 9 01.90 D R . . ... 81. 95 6 1. 2 02.10 0 C 82. 15 T !!!, %2. 0, "PLOT", P, %8. 04 02.20 A !, "REG FIT", R, !, "B", B, !, "M", M, !, "E", E 02.25 A !, "X LON", XL, !, "X HIGH", XH; 5 B=B-2\*E 02.30 A !, "X SCALE", XS, !, "Y SCALE", YS; S S=(XH-XL)/25 02.35 I (R-1)2.4,2.4,2.5 82.40 F I=1,3;0 3 82, 45 6 1.3 82.50 I (R-2)2.55,2.55,2.65 02.55 F I=1,3;D 4 **82.60 G 1.3** والمراجع المراجع والمراجع والمراجع والمراجع والمراجع والمتعاد والمستعم والمراجع 02.65 I (R-3)2.7,2.7,2.8 02.70 F I=1,3;0 5 02.75 6 1.3 02.80 I (R-4)2.85,2.85,2.15 82.85 F I=1,3;0 6 02, 90 G 1. 3 03.10 5 B=B+E 03.20 0 C 03.30 F J=XL, 5, XH; 5 Y=(B+M+J)\*.34/Y5; D 7 03.40 0 P . . . . . . . . . 04.10 5 B=8+E 04.20 0 C 04.30 F J=XL, 5, XH; 5 Y=FEXP(B+M\*J)\*.34/Y5; D 7 04.40 0 P 05.10 5 B=B+E 05.20 0 C 05.30 F J=XL, 5, XH; 5 Y=(B+M\*FLOG(J))\*.34/Y5; D 7 05,40 0 P 06.10 5 B=B+E 06.20 0 C 05.30 F J=XL, S, XH; S Y=FEXF(B+M\*FLOG(J))\*.34/YS; D 7 06.40 0 P 07.10 I (Y)7.4,7.2,7.2 07.20 I (Y-.34)7.3,7.3,7.4 07.30 5 A=FDIS(C2+J\*.34/X5,C1+Y) 07.40 R

	.GP2, 0	•
+H		
C FOCAL-	12	-
<b>91</b> , 10 A	"PEN DOWN", G. !!!; O C	
01.15 5	P=0; 5 C1=0; 5 C2=0	
01. 20 5	A=FDIS(0,0); 5 A=FDIS(0, 68)	
01.25 5	R=FDI5(1,02,.68);5 H=FDI5(1,02,0) D=FDI5(9,0);0 P	
01.30 5 01 35 D		
81.40 5	A=FDI5(0, 34); 5 A=FDI5(1.02, 34); 0 P	
<b>01</b> . 45 0	C	
	A=FDI5(.34,0);5 A=FDI5(.34,.68);0 P	
01.33 U 91 69 5	L A=FDIS( 68, A); S A=FDIS( 68, 68); D P	
<b>81.65</b> 0		
82.10 5	P=P+1; 5 C1=FAB5(C134)	
02.15 I	(P-3)2, 25, 2, 2, 2, 25	
82.20 J	(P-5)2, 35, 2, 3, 2, 35	
02.30 5	C2=. 68	
82.35 I	(P-6)2. 5, 2. 5, 2. 4	
<b>22.40</b> 0	R	
02.45 U		george an a company
02.55 F	K=1, N; D 3	
<b>8</b> 2.60 0	C	
02.65 G	2.1	
87 18 0		
93.15 T	!!, %2, "PLOT", P, %8. 04	
03.20 A	!, "REG FJT", R, !, "B", B, !, "M", M	
03.25 A	1, "X LON", XL, 1, "X HIGH", XH	
- 83.30 H	(R-1)3 4.3 4.3 5	
93.40 0		
03.42 F	J=XL,5,XH;5 Y=(B+M*J)*.34/YS;D 4	
03.44 0	P	
03.46 K A7 58 T	(8-2)3 55.3 55.3 65	
03.55 0	С	
03.57 F	J=XL, 5, XH; 5 Y=FEXP(B+M*J)*. 34/Y5; D 4	
03.59 0	P to the second s	
83.61 K	د مان ماند ماند می میکند. با میکند میکن در ۲۰۰ میکند میکند. در در ۲۰۰ میکند میک	
03.03 I 03.70 D	C	
03.72 F	J=XL, S, XH; S Y=(B+M*FLOG(J))*. 34/YS; D 4	
03.74 D		
03.76 R	40 412 05 2 05 2 4	
03.801 87.85 D	(R-4)3, 63, 3, 63, 3, 1	
03.87 F	J=XL, 5, XH; 5 Y=FEXP(B+M*FLOG(J))*. 34/Y5; D 4	
<b>0</b> 3.89 0	Ρ	
04.10 I	(Y24、424、ビノ4、ビ イビニーでは3は「ア、4」で、4」4	
84 20 1 84 20 5	A=FDIS(C2+J*, 34/X5, C1+Y)	
94.40 R		
*		

-----+L L, %LINEP. 0 \*11 C FOCAL-12 283.2 01.10 L 0, F1, I, #0, 1 01.20 A !!, "PEN DOWN", G 01.30 D 7 01.40 A !!!, "FDP", PF, !, "LDP", PL 02.10 A !!, "T100", D; 5 M=. 34 02.20 F J=2:5:0 5 . ..... 82.30 A !!, "TL", D; 5 M=. 68 02.40 F J=6,7;0 5 82.50 A !!, "FI/LI", D; 5 D=D\*10; 5 M=1.02 02.60 F J=10,12;D 5 82.70 0 R 02.80 D 7 \_\_\_\_03.10 A !!, "MEN", D; 5 D=D\*10; 5 M=. 34 03.20 F J=13,15;0 5 03. 30 A !!, "N100", D; 5 D=D\*10; 5 M=. 68 03.40 F J=16,19;D 5 03.50 A !!, "RR/ST", D; 5 D=D+10; 5 M=1.02 03.60 F J=8,9;0 5 The second second reaction in the second 03. 80 D 7 مرجع سمرد المرجع المستحد مرتوس والوالوالي 04.10 R !!, "5L", D; 5 D=-D\*100; 5 M=.34 04.20 5 J=26; D 5 04.30 5 D=1030; 5 H=.68 \_04.49 F J=20.23;0 5 \_\_\_ 84,50 S H=1.02 84.60 F J=24,25;0 5 04.70 0 R 84.89 G 1.3 05.10 5 L=J+1000 05.20 F K=PF, PL; 5 V=F1(L+K); D 6 05.30 0 P 05.40 0 C 86.10 I (V)6.2,6.3,6.3 06.20 5 V=V+4096 86.30 5 8=FDI5(N-V\*.34/D, 68\*(K-PF)/(PL-PF)) 07.10 0 C 87.20 5 A=FDI5(0,0);5 A=FDI5(0,.68) 07.30 5 R=FDIS(1.02, 68); 5 A=FDIS(1.02,0) 07.40 5 R=FDIS(0,0);0 P 07.50 0 C 07.60 5 A=FDIS(.34,0);5 A=FDIS(.34,.68);0 P 07.70 0 C 87.80 5 A=FDIS(.68,0);5 A=FDIS(.68,.68);0 P 07.90 0 C 3**8** 

Tabl	e VII	I.	Regression equations of 24 parameters on respiration rate for I-VO cells.
1.	т50	=	147.2220 + 21.1092 · ln(RR) + 98.7780
2.	<b>T70</b>	=	156.0950 + 63.3316 • ln(RR) <u>+</u> 165.1760
3.	<b>T90</b>	=	405.9660 + 44.2711 • ln(RR) <u>+</u> 253.2590
4.	T100	=	EXP[6.8533 - 0.0193(RR + 0.7480]
5.	PL	=	792.7180 - 16.8713(RR) <u>+</u> 273.1040
6.	TL	ш	EXP[7.9172 - 0.0355(RR) + 0.2342]
7.	FI	=	88.0191 - 1.5262(RR) <u>+</u> 25.5480
8.	MI	=	36.6944 - 4.5819 · ln(RR) + 10.8402
9.	LI	=	75.3811 - 13.1186 · ln(RR) + 12.7498
10.	MEN	=	52.9135 - 7.5962 • ln(RR) + 12.4183
11.	MED	=	43.3729 - 5.4107 · ln(RR) + 11.9047
12.	MOD	H	35.1646 - 3.3601 · ln(RR) + 10.9786
13.	N50	=	-0:0234 + 1.4496 • ln(RR) + 1.7945
14.	N70	=	-1.4086 + 3.1496 • ln(RR) + 4.4809
15.	N90	Ш	3.9172 + 3.4890 · ln(RR) + 6.5986
16.	N100	=	EXP[3.3038 - 0.0088(RR) + 0.4769]
17.	ST	=	$124.0940 - 24.1712 \cdot \ln(RR) + 25.8741$
18.	SL	=	EXP[-0.6432 - 0.0583(RR) + 0.9638]
19.	T5P	=	-6.4697 + 7.1477 • ln(RR) + 6.0545
20.	T7P	=	-14.6178 + 12.9528 • ln(RR) + 9.6405
21.	T9P	=	14.2368 + 17.3266 • ln(RR) <u>+</u> 14.9481
22.	TlOP	=	6.1723 + 16.8245 · ln(RR) <u>+</u> 21.9979
23.	$\mathtt{P}\mathtt{L}\mathtt{P}$	=	$EXP[2.4491 + 0.3447 \cdot ln(RR) + 0.4723]$
24.	TLP	=	$EXP[2.3434 + 0.4872 \cdot ln(RR) + 0.2374]$

Tabl	e IX.	Regression equations of 24 parameters on respiration rate for I=VI cells.
1.	<b>T</b> 50	= EXP[5.2791 - 0.0168(RR) + 0.4879]
2.	<b>Ŧ7</b> 0	= EXP[5.9359 = 0.0207(RR) + 0.4527]
3.	<b>Ŧ</b> 90	= 544,7000 - 5,3169(RR) + 110.3810
4.	<b>Ŧ1</b> 00	= 1822.4400 - 367.3070 · ln(RR) + 151.5740
5.	PL	$= EXP[8.9515 - 0.9727 \cdot \ln(RR) + 0.5897]$
6.	TL	= EXP[7, 4751 - 0, 0216(RR) + 0.3241]
7.	FI	= EXP[4.1577 - 0.0144(RR) + 0.4247]
8.	MI	= EXP[3.0236 = 0,0097(RR) + 0.4929]
9.	ΪI	= EXP[3.4636 - 0.0084(RR) + 0.5742]
10.	MEN	= EXP[3.3497 - 0.0103(RR) + 0.4487]
11.	MED	= EXP[3.2064 = 0.0101(RR) + 0.4596]
12.	MOD	= EXP[3.0901 - 0.0097(RR) + 0.4704]
13.	N50	= EXP[1.3283 - 0.0029(RR) + 0.5420]
14.	N70	= EXP[2.1464 - 0.0079(RR) + 0.6085]
15.	N90	$= EXP[3.2366 - 0.1684 \cdot \ln(RR) + 0.5423]$
16.	N100	$= EXP[4.4251 - 0.3482 \cdot \ln(RR) + 0.5332]$
17.	ST	= 133.7710 - 24.1028 · ln(RR) + 26.2316
18.	SL	= 0.2676 + 0.0009 (RR) + 0.1664
19.	T5P	$= EXP[1.6797 + 0.2574 \cdot ln(RR) + 0.6053]$
20.	T7P	$= 13.8721 + 3.2756 \cdot \ln(RR) + 12.3565$
21.	T9P	$= 14.4688 \pm 8.2056 \cdot \ln(RR) \pm 14.5038$
22.	<b>T10</b> P	= 44.8520 + 5.2108 · 1n(RR) + 15.8760
23.	PLP	= 53.8008 = 5.4440 · ln(RR) + 13.9808
24.	TLP	= EXP[3, 1710 + 0, 1823 + ln(RR) + 0.3230]

Table	e X.	Regression equations of 24 parameters on respi- ration rate for E-VI cells.
1.	<b>T</b> 50	= 414.4040 - 80.5027 · ln(RR) + 49.1951
2.	<b>T7</b> 0	= 675.8920 - 133.5940 · ln(RR) + 78.0391
3.	<b>T90</b>	= 1438.1000 - 299.7580 · ln(RR) + 147.7610
4.	T100	= 2617.3300 - 569.2290 · ln(RR) + 219.7980
5.	PL	= 1495.4300 - 325.7690 · ln(RR) + 162.7690
6.	TL	$= 3048.0900 - 632.1220 \cdot \ln(RR) + 203.9220$
7.	FI	= 164.2190 - 31.3311 · ln(RR) + 15.0115
8.	MI	$= 47.4782 - 8.5725 \cdot \ln(RR) + 5.9890$
9.	LI	$= 50.0437 - 7.2535 \cdot \ln(RR) + 7.5328$
10.	MEN	= 63.2751 - 11.2802 · ln(RR) + 7.1998
11.	MED	= 55.7401 - 10.0034 · ln(RR) + 6.7460
12.	MOD	$= 51.5672 - 9.4249 \cdot \ln(RR) + 6.4786$
13.	N50	= 2.8954 + 0.0026 (RR) + 1.0860
14.	N70	$= EXP[1.9225 - 0.0856 \cdot \ln(RR) + 0.4301]$
15.	N90	$= EXP[3.3632 - 0.2598 \cdot ln(RR) + 0.5371]$
16.	N100	$= EXP[4.8054 - 0.4883 \cdot \ln(RR) + 0.5994]$
17.	ST	= EXP[3.8809 - 0.0087(RR) + 0.4402]
18.	SL	= 0.3539 - 0.0007 (RR) + 0.1330
19.	T5P	= 12.1021 + 0.1206 (RR) + 5.9030
20.	<b>T7</b> P	= 18.5201 + 0.1848(RR) + 8.2920
21.	T9P	= 41.1972 + 0.1200 (RR) + 12.9830
22.	T10P	= 105.7470 - 9.9173 · ln(RR) + 16.8018
23.	PLP	= 49.2392 - 0.2522(RR) + 13.3991
24.	$\mathbf{TLP}$	= 31.3642 + 0.3127(RR) + 12.2442

Table	e XI.	1	Regression equations of 24 parameters on mode for I=VO cells.
1.	<b>T</b> 50	#	$EXP[1.0320 + 1.2984 \cdot ln(MOD) + 0.4121]$
2.	<b>T7</b> 0	Ŧ	EXP[0,8938 + 1.4780 · $\ln(MOD) + 0.4866$ ]
3.	<b>T</b> 90	Ŧ	EXP[1.3322 + 1.4884 · $\ln(MOD) + 0.5060$ ]
4.	<b>T</b> 100	H	EXP[2.8979 + 1.1556 • ln(MOD) + 0.4785]
5.	PL	Ħ	EXP[4.8709 + 0.3974 · ln(MOD) + 0.4734]
6.	ŢĿ	=	EXP[6.9655 + 0.0141(MOD) + 0.2555]
7.	FI	Ŧ	EXP[1.6716 + 0.7526 · $\ln(MOD) + 0.2953$ ]
§.	MI	æ	$EXP[-0.2865 + 1.0628 \cdot ln(MOD) + 0.0819]$
9.	LI	Ŧ	EXP[3.1848 + 0.0164(MOD) + 0.3305]
10.	MEN	Ħ	$EXP[0.6723 + 0.8603 \cdot \ln(MOD) + 0.0963]$
11.	MED	=	$EXP[0.1401 + 0.9860 \cdot \ln(MOD) + 0.0701]$
12.	RR	Ţ	EXP[2.8361 - 0.0035(MOD) + 0.3519]
13.	N50	=	EXP[=0.2682 + 0.4897 • ln(MOD) + 0.3919]
14.	N70	=	EXP[-0.3260 + 0.6783 · ln(MOD) + 0.5045]
15.	N90	Ŧ	EXP $[0.5364 + 0.6099 \cdot \ln(MOD) + 0.5160]$
16.	N100	=	$EXP[2.7940 + 0.1159 \cdot \ln(MOD) + 0.4755]$
1Ż.	ST	=	EXP[5.7306 - 0.5586 · $\ln(MOD) + 0.2817$ ]
18.	$\mathtt{SL}$	=	$1.5777 - 0.4054 \cdot \ln(MOD) + 0.1762$
19.	T5P	=	EXP[-0.7570 + 1.0007 · ln(MOD) + 0.4944]
<u>2</u> 0.	T7P	÷	EXP[-0.9009 + 1.1821 • ln(MOD) + 0.5395]
21.	T9P	=	$EXP[-0.4554 + 1.1903 \cdot ln(MOD) + 0.5328]$
22.	TlOP	=	EXP[1.1015 + 0.8601 · $\ln(MOD) + 0.4767$ ]
23.	PLP	I	EXP[3.0794 + 0.1005 · $\ln(MOD) + 0.4852$ ]
24.	ŢLP	ŧ	9.3865 + 10.1569 • ln(MOD) + 10.7925

Table	e XII	•	Regression equations of 24 parameters on mode for I-VI cells.
1.	<b>T</b> 50	=	EXP[3.4807 + 0.4385 • ln(MOD) + 0.4992]
2.	<b>T7</b> 0	=	EXP[4.2152 + 0.3596 • ln(MOD) + 0.5112]
3.	т90	=	EXP[5.0715 + 0.2638 · ln(MOD) + 0.4108]
4.	<b>T100</b>	=	EXP[5.5763 + 0.2304 · ln(MOD) + 0.4115]
5.	PL	=	118.0350 + 74.1879 · ln(MOD) + 214.8230
6.	TL	=	EXP[5.8916 + 0.2984 · ln(MOD) + 0.4226]
7.	FI	=	EXP[1.8325 + 0.6608 · ln(MOD) + 0.3431]
8.	MI	H	$EXP[-0.1469 + 1.0296 \cdot \ln(MOD) + 0.0848]$
9.	LI	Ξ	$EXP[0.5052 + 0.9691 \cdot \ln(MOD) + 0.3438]$
10.	MEN	Ш	EXP $[0.4260 + 0.9319 \cdot \ln(MOD) + 0.1187]$
11.	MED	=	$EXP[0.1874 + 0.9697 \cdot \ln(MOD) + 0.0754]$
12.	RR	=	57.9943 - 8.2390 · ln(MOD) + 13.6773
13.	N50	=	EXP[1.5490 - 0.0186(MOD) + 0.5220]
14.	N70	=	12.3624 - 0.2541(MOD) <u>+</u> 5.6031
15.	N90	=	EXP[3.2714 - 0.0358(MOD) + 0.4619]
16.	N100	=	EXP[3.9485 - 0.0425(MOD) + 0.4265]
17.	ST	=	EXP[4.4601 - 0.0402 (MOD) + 0.4317]
18.	SL	=	0.4408 - 0.0518 · ln(MOD) + 0.1649
19.	T5P	=	EXP[2.4029 + 0.0101(MOD) + 0.6075]
20.	<b>T7</b> P	=	EXP[3.0127 + 0.0048(MOD) + 0.5512]
21.	T9P	=	49.1428 - 2.1869 · ln(MOD) + 14.7922
22.	<b>T10</b> P	=	75.3259 - 4.4685 · ln(MOD) + 15.8466
23.	PLF	=	EXP[3.5634 - 0.0067 (MOD) + 0.4934]
24.	TLP	=	$EXP[3.5274 + 0.1022 \cdot ln(MOD) + 0.3264]$

Table	e XIII	Γ.	Regression equations of 24 parameters on mode for E-VI cells.
1.	т50	Ħ	43.8866 + 4.6491(MOD) <u>+</u> 51.7531
2.	т70	=	75.7932 + 6.8930(MOD) <u>+</u> 87.0515
3.	<b>T90</b>	=	92.4733 + 15.4179 (MOD) + 171.5270
4.	T100	=	178.3820 + 22.8032(MOD) + 312.2210
5.	PL	=	205.4960 + 7.1587(MOD) + 224.2730
6.	TL	=	406.0200 + 21.6303(MOD) <u>+</u> 336.7980
7.	FI	=	19.3363 + 1.8472(MOD) + 15.9847
8.	MI	=	EXP[0.0741 + 0.9541 • ln(MOD) + 0.0576]
9.	LI	=	EXP[1.4074 + 0.6132 · $\ln(MOD) + 0.2543$ ]
10.	MEN	=	2.9307 + 1.1204(MOD) + 1.7804
11.	MED	=	1.4173 + 1.0386(MOD) + 1.1502
12.	RR	H	EXP[4.2340 - 0.0372 (MOD) + 0.4073]
13.	N50	=	4.1876 - 0.4250 · ln(MOD) + 1.0718
14.	N70	=	8.5037 - 1.0773 · ln(MOD) + 2.2008
15.	N90	=	24.4363 - 4.1020 · ln(MOD) + 5.6749
16.	N100	=	58.5247 - 11.7915 · ln(MOD) + 13.4960
17.	ST	=	98.2588 - 21.4823 · ln(MOD) + 16.2235
18.	SL	=	0.3880 - 0.0034(MOD) <u>+</u> 0.1308
19.	T5P	=	EXP[2.2873 + 0.1666 · ln(MOD) + 0.3945]
20.	<b>T7</b> P	=	$EXP[2.8490 + 0.1194 \cdot ln(MOD) + 0.3965]$
21.	<b>T9</b> P	=	37.6028 + 0.4654(MOD) + 12.6321
22.	T10P	=	60.9340 + 0.5264(MOD) <u>+</u> 17.0150
23.	PLP	=	52.2560 - 4.6586 · ln(MOD) + 14.0615
21	mr.D	=	$EXP[4, 644] = 0.32, 46 \cdot ln(MOD) + 0.2601]$

Table XIV. Best fitting regression equations for 24 parameters on respiration rate and mode for I-VO, I-VI and E-VI cells: linear (LIN); exponential (EXP); logarithmic (LOG); loglog (LLG).

	Parameter	$\frac{I-VO}{(RR)}$	$\frac{I-VI}{(RR)}$	$\frac{E-VI}{(RR)}$	I-VO (MOD)	I-VI (MOD)	E-VI (MOD)
1	T50	LOG	EXP	LOG	LLG	LLG	LIN
2	т70	LOG	EXP	LOG	LLG	LLG	LIN
3	<b>T90</b>	LOG	LIN	LOG	LLG	LLG	LIN
4	<b>T100</b>	EXP	LOG	LOG	LLG	LLG	LIN
5	PL	LIN	LLG	LOG	LLG	LOG	LIN
6	TL	EXP	EXP	LOG	EXP	LLG	LIN
7	FI	LIN	EXP	LOG	LLG	LLG	LIN
8	MI	LOG	EXP	LOG	LLG	LLG	LLG
9	LI	LOG	EXP	LOG	EXP	LLG	LLG
10	MEN	LOG	EXP	LOG	LLG	LLG	LIN
11	MED	LOG	EXP	LOG	LLG	LLG	LIN
12	MOD (RR)	LOG	EXP	LOG	(EXP)	(LOG)	(EXP)
13	N50	LOG	EXP	LIN	LLG	EXP	LOG
14	N70	LOG	EXP	LLG	LLG	LIN	LOG
15	N90	LOG	LLG	LLG	LLG	EXP	LOG
16	N100	EXP	LLG	LLG	LLG	EXP	LOG
17	ST	LOG	LOG	EXP	LLG	EXP	LOG
18	SL	EXP	LIN	LIN	LOG	LOG	LIN
19	T5P	LOG	$\mathtt{LLG}$	LIN	LLG	EXP	LLG
20	T7P	LOG	LOG	LIN	LLG	EXP	LLG
21	T9P	LOG	LOG	LIN	LLG	LOG	LIN
22	T10P	LOG	LOG	LOG	LLG	LOG	LIN
23	PLP	LLG	LOG	LIN	LLG	EXP	LOG
24	TLP	LLG	LLG	LIN	LOG	LLG	LLG

## APPROVAL SHEET

The dissertation submitted by Charles Lewis Webber, Jr., has been read and approved by the following Committee:

> Dr. Clarence N. Peiss, Chairman Professor, Physiology and Associate Dean, Graduate School, Loyola

Dr. Walter C. Randall Professor and Chairman, Physiology, Loyola

Dr. Robert D. Wurster Associate Professor, Physiology, Loyola

Dr. Syogoro Nishi Professor, Pharmacology, Loyola

Dr. Joseph D. Brain Assistant Professor, Harvard University, Boston

The final copies have been examined by the director of the dissertation and the signature which appears below verifies the fact that any necessary changes have been incorporated and that the dissertation is now given final approval by the Committee with reference to content and form.

The dissertation is therefore accepted in partial fulfillment of the requirements for the degree of Doctor of Philosophy.

Quernst 9, 1973 Date

Corona M. Ka Signature of Advisor