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# Acidity of Light-Cured Glass Isomer Materials

Najwa Jowharji Loyola University Chicago

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### ACIDITY OF LIGHT-CURED GLASS IONOMER MATERIALS

**BY** 

NAJWA JOWHARJI

A Thesis Submitted to the Faculty of the Graduate School of Loyola University of Chicago in partial Fulfillment of the Requirments for the Degree of Master of Science January 1991

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### DEDICATION

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I dedicate this thesis to my parents; my husband, Abed and my sons Saif and Mhanna

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Special Thanks are given to my parents for their support, love, and for everything that they have done for me. Finally, I would like to acknowledge the financial support offered by Saudi Arabian Government.

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#### VITA

The author, Najwa Jowharji, is the daughter of Mansour Jowharji and Suad Alyaman. She was born October 16, 1961, in Jeddah, Saudi Arabia.

Her elementary education was obtained in the public schools of Saudi Arabia. Her secondary education was completed in 1979 at the First Secondary School, Taif, Saudi Arabia.

In 1979, Dr. Jowharji entered King Saud University, receiving the degree of Bachelor of dental surgery {B.D.S.) in May, 1985.

Dr. Jowharji was granted a scholarship from her school (King Saud University) in 1985, to study in the united states.

In September, 1985, Dr. Jowharji entered the general residency program at the University of Minnesota, which was completed in one year.

In June, 1987, Dr. Jowharji entered Loyola university of chicago, receiving the specialty degree in pediatric dentistry in June, 1989. During her second year residency she was the chief resident and she was teaching as a part-time faculty in the pediatric dental clinic.

In June, 1989, Dr. Jowharji was accepted in the graduate School of Loyola University in the Oral Biology Program, enabling her to complete the Master of Science in January 1991.

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## LIST OF FIGURES



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#### **INTRODUCTION**

Glass ionomers have a wide range of uses in dentistry today. They can serve as fillings, bases, liners, luting cements, cores and fissure sealants. Since their emergence in the early 1970's, they have undergone a tremendous development.

Recently, light-cured glass ionomer liners were introduced to replace the traditional chemical cured glass ionomers. Their major advantages are increased working time, shorter setting time, improved strength and increased acid resistance.<sup>12</sup> However, their acidity has not been studied.

Previous research suggested that pulpal irritation could be caused by the initial acidity of the prolonged chemical reaction of the self cured material. One of the major advantages of the light - cured glass ionomer liners is the setting reaction will be triggered by visible light which shorten the setting time (20-30 sec).

The purpose of the present study was:

- 1. to investigate in vitro the pH during setting of four types of light-cured glass ionomer liners.
- 2. to compare the pH of light cured glass ionomers with six self cured glass ionomers.
- 3. to compare the pH of the glass ionomer materials with widely used zinc polycarboxylate and zinc phosphate cements.

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### **LITERATURE REVIEW**

### Development of glass-ionomer cements

The glass-ionomer cements are a new and interesting development in adhesive dentistry. This dental cement system were developed in 1971 by Wilson and Kent<sup>1</sup> which is based on the hardening reaction between an ion-leachable aluminosilicate glass and aqueous solutions of polymers and co-polymers of acrylic acid (ASPA). The intention is to develop this material for a variety of dental applications such as the restoration of anterior teeth, the filling of erosion cavities, general cementation and cavity linings.<sup>2</sup>

In 1973, Kent et al. found a glass that was high in fluoride (G-200)<sup> $a$ </sup> and mixed with 50 percent aqueous solution of polyacrylic acid which gave a useable cement, ASPA I.<sup>3,4</sup> The properties of the ASPA cement were compared with those of existing dental cement. It appears to combine certain favorable properties of dental silicate and polycarboxylate cements.  $3$  However, one of the problem associated with ASPA I, is the limited working time and the slow rate of surface hardening. This has been improved by adding chelating agents such a tartaric acid which increase the rate of hardening without reducing the working time.<sup>5</sup> This refinement of ASPA I was termed ASPA II and constituted the first practical glassionomer cement. Even by today's standards its properties were excellent.<sup>3</sup>

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<sup>\*</sup>a. G-200 is a designation of the Laboratory of the Government Chemist (LGC) (London)

Attempts to improve the reactivity of glass powder by increasing the AL<sub>2</sub>O<sub>3</sub> :SiO<sub>2</sub> ratio have been also reported by Kent, Lewis and Wilson. <sup>4</sup> This discovery enabled more reactive glasses to be prepared suitable for forming rapid setting cement with polyacrylic acid which is a weaker acid than phosphoric acid used in dental silicate cement.

Problems associated with the use of polyacrylic acid have been reported. Its viscosity was high and the liquid tends to gel. This problem was solved by Crisp and Wilson<sup>6</sup>, who developed a copolymer of acrylic and itaconic acid that did not gel at 50% concentrations in aqueous solution. In this form glass ionomer cement was termed ASPA IV and was considered suitable for commercial production as a fissure filling material and for treatment of erosion cavities.  $7,8$ 

Studies have been made to combine the desirable properties of silicate cements, composite and polycarboxylate cements which have been achieved in the developments of the glass ionomer cement system. These new cements designed for a number of specific clinical applications.  $8,9,10$  The biological compatibility, effective maximum grain size, retentive ability, disintegration in and absorption of water and solubility in acid proved to be fully acceptable.<sup>11</sup>

Recently, light-cured glass ionomer liners were introduced. Their major advantages are increased working time, shorter setting time, improved strength and increased acid resistance.<sup>12</sup>

#### Glass Composition

Cement properties depend on chemical composition, particle-size distribution of the powder, molecular weight and concentration of the liquid polyacid. <sup>3</sup> The powder of a glass ionomer cement is a calcium fluoroaluminosilicate glass with a formula of SiO  $_2$ -Al  $_2$ O  $_3$ -CaF  $_2$ -Na  $_3$ AlF  $_6$ -AlPO  $_4$ . The nominal composition of the glass is listed in table 1.<sup>13,14</sup>

Investigations carried out on variants of these glasses showed that their reactivity depended on the ratio of alumina to silica in the fusion mixture used for their preparation. This ratio, which is the ratio of a basic oxide to an acidic oxide, determines the basicity of the glass. Because the reaction between glass and liquid is an acid base one, an increase in the basicity of the glass will increase the rate of setting reaction. <sup>2</sup> According to Wilson and McLean, <sup>15</sup> the Al <sub>2</sub>O <sub>3</sub>/SiO 2 ratio is required to be 1:2 or more and the fluoride content can be up to 23%. The visual appearance of the glass could be clear, opal or opaque depending on its chemical composition. Glasses high in calcium fluoride or alumina are opaque. This opaqueness arises from the presence of dispersed crystalline phases of fluoride or corundum. The addition of cryolite ( $Na<sub>3</sub>AIF<sub>6</sub>$ ) reduces the temperature at which the glass will fuse and increases the translucency of the set cement. Aluminum phosphate is added to improves the translucency and to add body to the cement paste.

#### Liquid Composition

The liquid typically is a 47.5% solution of 2:1 polyacrylic acid/itaconic acid copolymer (average molecular weight 10,000) in water.<sup>14</sup> The copolymer may also be freeze-dried and incorporated into the powder. In addition to the acrylic aciditaconic acid copolymer, it also contains a small amount of tartaric acid, in the range of 5%. The itaconic acid reduces the viscosity of the liquid and inhibits gelation. The tartaric acid can be added to improve the working and setting characteristics.<sup>5,6,16,17</sup>

## **Table 1**

Nominal composition of calcium fluoroalumino silicate glass used in powder

of glass ionomer cement.<sup>13</sup>



Polyacrylic acid is a weaker acid than phosphoric acid and a more basic glass is required to produce equivalent setting, hence the proportion of alumina to silica has to be greater.<sup>2</sup> When polyacrylic acid is dissociated, hydrogen ions tends to be bonded to the polyelectrolyte chain and the large polyacrylic molecules will show less tendency to diffuse along dentinal tubules than the smaller phosphoric acid molecules. In addition, with a long chain polyacid containing a multiplicity of functional groups, ion binding at only one of these to the bulk of the cement will tend to hinder its migration. $2$ 

Recently, four light-cured glass ionomer systems have become commercially available.<sup>12,39</sup> In Vitrabond liner/base, the powder contains a fluoroaluminosilicate glass and some of the chemical components of the light activated resin accelerator. The liquid contains a polyacrylic acid copolymer with pendant methacrylate groups, 25% HEMA (hydroxyethylmethacrylate), additional photo accelerators, and water. After mixing the resulting material contains 10% HEMA

The second system called XR-lonomer (Kerr, Manufacturing Co.), the powder is a calcium aluminofluorosilicate glass and the liquid is polyacrylic acid with pendent methacrylate groups. The XR-lonomer liquid differs from Vitrabond's in that its polyacrylic acid contains about half the number of pendant methacrylate groups. In addition there is no HEMA in the liquid.

The third system called Timeline (L.D. Caulk), is not a glass ionomer system. Its a one-part material of medium viscosity containing a relatively hydrophobic dimethacrylate resin matrix, filled with radiopaque glass and sodium fluoride powder. It has an initial fluoride release (20 ppm). However, this drops to 40% of the release of a conventional glass ionomer liner after 1 year. An

additional brand of glass ionomer, Zionomer (DentMat), was used in this study, however, no published data on its composition exist in the literature at this time. Chemistry and setting reaction of glass ionomer cement

Chemical studies on the reaction of the glass ionomer cement showed that the setting mechanism is an acid base reaction between the acidic polyelectrolyte and the alumino silicate glass. <sup>14,18,19</sup> The setting reaction of glass ionomer cement is reported to take place in several overlapping stages. $^{10,20}$ 

In a freshly mixed paste, its presumed that hydrated protons from the liquid penetrate the surface regions of the powder particles, displacing cations (Al  $3+$ ,  $Ca<sup>2+</sup>$ ) and degrading the alumino silicate network into the aqueous phase of the cement paste. Metallic salt bridges are then formed between the long chains of charged polycarboxylate ions, cross linking them and causing the aqueous phase to gel and the cement to set to an amorphous mass.  $18,19,20$ 

At the first stage of the reaction calcium ions are more rapidly bound to the polyacrylate chains than aluminum ions and are chiefly responsible for its initial set. 2 15• At the second stage of the reaction, the aluminum salt is formed and it is responsible for the final hardening of glass ionomer cement. In this stage the cement shows considerable increase in hardness and stiffness as well as resistance to plastic deformation.<sup>21,22,23</sup> McLean and Wilson stated that the cement initially sets to a condition which enables it to be carved like an amalgam (calcium ion-exchange), later it sets rock hard (aluminium ion-exchange).<sup>7</sup> The fluoride and phosphate ions form insoluble salts and complexes. The sodium ions form a silica gel. The structure of the fully set cement is a composite of glass particles surrounded by silica gel in a matrix of polyanions cross-linked by ionic bridges.

Within the matrix are small particles of silica gel containing fluorite crystallites.<sup>14</sup>

### Effects on pulp tissue

The dentin and the pulp must be considered as one organ (the pulp-dentin complex) because of the intimate relationship between the cellular tissue within the dentin and the peripheral pulp tissue. The dentinal tubules occupy from 20%- 39% of dentin, and the dentinal fluid within represents about 22% of the total volume of dentin.  $24,25,26$ 

Reports as to the cause of pulpal irritation from glass ionomer cements have fluctuated between the initial acidity of the material and the influence of bacteria. Brannstrom in 1984 reported that the pulpal inflammation may arise from bacterial infection rather than from the filling material or the pre-treatment procedures.  $27$  In another study, however, Plant, et. al showed no correlation between pulpal inflammation and microleakage of all glass ionomer cements tested. Upon histological examination all pulps in teeth filled with glass ionomer cements revealed some degree of inflammation.<sup>28</sup>

In a report to the American Dental Association's Council on Dental Materials, Instruments, and Equipment it was noted that sensitivity and pulpal death occurred in some cases when glass ionomers were used for crown cementation as a luting agent. <sup>29</sup> This hypersensitivity was explained by Gunilla and Brannstrom who indicated that some materials are hygroscopic and may dehydrate dentin producing centrifugal flow of fluid in the dentinal tubules. This dehydration of dentin which may elicit pain and result in aspiration of odontoblasts into tubule.<sup>30</sup> A luting mix has a higher toxicity than a thick base mix and after a four days a tremendous number of neutrophils have been found to infiltrate the pulp tissue.<sup>31</sup>

To investigate the pulp response a clinical study by Norman and Wright compared the responses of patients to a glass ionomer cement (Ketac-Cem) and zinc phosphate cement (Tenacin) used in cementation of various types of castings. They concluded that, after six months, both cements produced similar pulpal response and either cement can be used safely for crown cementation. They also indicated that bacterial or marginal leakage can induce hypersensitivity<sup>32</sup>. This finding has been studied by Hey's et.al using different types of glass ionomers and zinc phosphate cement (Tenacin) in Rhesus monkeys. They found that hypersensitivity after crown cementation did not result from bacteria or marginal leakage. Since evaluation of the pulp response was not statistically significant, they concluded that other factors may contribute to hypersensitivity after crown cementation.<sup>33</sup>

In order to distinguish material toxicity from bacterial effect, Patterson and Watts examined ASPA (De-Trey) by placing it directly on exposed dental pulps of germ free rat molars. They found a localized zone of pulpal necrosis with inhibition of calcific repair.<sup>34</sup>

A human histological study showed evidence of severe pulpal response beneath glass ionomer compared to zinc oxide-eugenol, and a significant positive correlation was found between pulpal inflammation and bacterial leakage.  $35$  In another study using monkeys, evaluation of pulpal response showed no significant difference between glass ionomer cement and zinc oxide-eugenol.<sup>36</sup> Additionally, the culture tissue study showed less cytotoxic action than zinc oxide-eugenol.

Other varying degrees of toxicity have been described when glass ionomer cements were placed in tissue culture. Hume and Mount reported that each of the tested glass ionomer cements was severely toxic. This finding supports the proposal that acid release may be a factor contributing to the observed  $c$ vtotoxicity. $37$  The pH and the amount of the free acid depend on the setting rate of the cement.<sup>31</sup> This also was a concern when Smith and Ruse suggested that the initial acidity of glass ionomer cements may contribute to their damaging effect on the pulp. 38

Light-cured glass ionomer liners were introduced in late 1989, at this time very little material has been reported in the literature. Some of the chemical and physical properties of three new types of light cured glass ionomer (TimeLine, Vitrabond, and XR-lonomer) have been reported. Light-cured glass ionomer had a lower acidity and a setting time of 20-30 seconds compared with 4.5-5.0 minutes for conventional types.  $12.39$ 

### **MATERIALS AND METHODS**

### **Materials Investigated**

Four commercially available light-cured and six self-cured glass ionomers were used in this study. Two zinc polycarboxylate and zinc phosphate cements were also investigated in this study for comparison and as control groups(table 2).

The materials selected represent the leading brands on the markets. Light cured glass ionomers, zinc phosphate cement are American products. GC Fuji I, GC-Dentin cement, shofu glass ionomer and shofu polycarboxylate are Japanese products. Ketac-cem, Katac-Bond, Durelon and Baseline represent the European products.

Details of the chemical composition, mode of supply, methods of polymerization, and manufacturer are presented in table 2.

### Assembly and specimens preparation

The pH of the tested materials were measured using the following assembly(Fig.1)

- 1. A corning module 10 pH meter<sup>a</sup>.
- 2. pH electrode (flat surface polymer body combination electrode)<sup>a</sup>.
- 3. A standardized metal stand to hold the electrode at fixed distance from the sample surface each time.

<sup>\*</sup>a. Corning Medical and Scientific, Corning Glass Works. Medfield, MA 02052 USA.

			Glass Ionomer Cements, Liner/Base Investigated			
No.	<b>Materials</b>	Cure	Mode of supply	code	Batch No.	<b>Manufacturer</b>
$\blacksquare$	vitra bond	light	liquid/powder	<b>VB</b>	7510	3M Company, St. Paul, MN 55414
$\mathbf{z}$	<b>TimeLine</b>	light	paste	<b>TL</b>	012389	<b>Caulk Company</b> Milford, DW 19963
3	<b>XR-lonomer</b>	light	liquid/powder	<b>XR</b>	3606 $-21626$	<b>Kerr Company</b> Romulus, MI 48174
4	<b>Zionomer</b>	liaht	liquid/powder	ZI	powder 498013 liauid 499008	Den-Mat Corp. Santa Maria, CA 93456
5	Ketac-Cem	chemical	llquid/powder	<b>KC</b>	021787	<b>ESPE-premier</b> praparate GMBH Co.KG D-8031 seefeld/oberbay
6	<b>GC Full I</b>	chemical	liquid/powder	F1	210971	<b>G-C Industrial Corp.</b> Tokyo, Japan
7	Shofu Type I	chemical	liquid/powder	<b>SG</b>	082086	<b>Shofu Dental Corp.</b> Menio Park, CA 94025
8	<b>Katac-Bond</b>	chemical	liquid/powder	<b>KB</b>	080486	<b>ESPE-premier</b> praparate GMBH Co.KG D-8031 seefeld/oberbay
9	<b>BaseLine</b>	chemical	liquid/powder (water)	<b>BL</b>	890181	DeTrey-Dentsphy Weybridge,Surrey,England
10	<b>GC Dentin cement</b>	chemical	liquid/powder	DC	080592	<b>G-C Industrial Corp.</b> Tokyo, Japan
11	<b>Shofu</b> Hy-Bond polycarboxylate	chemical	liquid/powder	<b>SP</b>	103086	Shofu Dental Corp. Menlo Park, CA 94025
12	<b>Durelon</b>	chemical	liquid/powder	<b>DP</b>	0135	<b>ESPE</b> praparate GMBH Co.KG D-8031 seefeld/oberbay
13	Zinc phosphate	chemical	liquid/powder	<b>ZP</b>	0208710	<b>Mission White Dental, INC</b> Tinton Falls, NJ 07724

Table 2







Sample dimensions were made using a standardized metal ring measuring 2omm. in diameter and 1mm. in thickness, ADA specification No. 27,4.3.6. Two square glass plate 5 x 5 cm and 2 mm thick, two square myler plastic sheets .0635 mm thick and two binder clips were also used to make the samples (fig 2).

Five specimens of each material were dispensed accurately according to the respective manufacturer's instructions and mixed under room conditions (22-23° C and 30% to 50% relative humidity). (table 3)

After mixing, the cement was immediately placed in the metal ring. In making specimens, the cement-filled metal ring was pressed between the mylar sheets and two glass plates to extrude the excess cement and to insure parallel and smooth surfaces by means of the two metal paper clips. If its a light cured material, the sample was cured for 20-30 second using the same light activating machine each time.

The specimens were placed in a humidity chamber at 37' C and 80% relative humidity. At the time of measurement each specimen was removed from the humidity chamber and placed on the stand at room temperature and a two drops of deionized water (.1 ml) were placed on the surface of the set cement. Before taking any measurements, the pH meter was calibrated by using a standard pH 4 buffer solution (potassium acid phthalate). The electrode was then placed to contact the water at a fixed distance and the reading was recorded.

This procedure was repeated after 15, 30, 45, 60, 120, 180 minutes and after 24 hours from mixing time. Between measurements, the electrode was cleaned, recalibrated and stored in a potassium acid phthalate, pH 4.







**Diagrammatic illustration of the assembly used to prepare specimens** 



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### Statistical Methodology

A two way analysis of variance (ANOVA) was performed to test the difference between the acidity level for all materials stored for seven different times. Whenever the two-way (ANOVA) revealed a significant time by material interaction difference, a one way ANOVA was performed for each material, to test the effect of storage times and at each storage time to compare between materials. In all cases for which the one-way ANOVA showed an overall difference between means, a Schaff'e test was used to compare all possible pairs of means at  $(p=.01$  level).

#### **RESULTS**

A summary of mean pH values, standard deviations, and number of specimens are presented in Table 4 for light-cured glass ionomers, polycarboxylates and zinc phosphate cement; and in Table 5 for self-cured glass ionomer materials. Mean values  $\pm$  standard deviation are also graphically presented in the Appendix Figures 6 through 9.

Light-cured glass ionomer materials shows a minimum mean range of pH  $(4.52 \pm 0.16)$  to  $(5.47 \pm 0.02)$  for XR-lonomer and Zionomer, respectively at 15 minutes from mixing time. A maximum mean range of pH (5.57  $\pm$  0.17) to (6.72 ± 0.08) for Vitrabond and Zionomer, respectively after 24 hours of storage time.

Self-cured glass ionomer materials shows a minimum mean range of  $pH \pm$ standard deviation (3.65  $\pm$  0.27) to (4.79  $\pm$  0.66) for BaseLine, and Shofu Type I glass ionomer, respectively at 15 minutes storage time. A maximum range of (4. 70  $\pm$  0.22) to (6.47  $\pm$  0.04) is showed for BaseLine and Ketac-Bond, respectively at 24 hours storage time.

Polycarboxylate materials (Shofu Hy-Bond and Durelon) show a minimum of pH mean  $\pm$  standard deviation of (4.32  $\pm$  0.52, 4.57  $\pm$  0.11) at 15 minutes storage time and a maximum of  $(6.5 \pm 0.17, 6.3 \pm 0.19)$  at 24 hours storage time respectively. Zinc phosphate cement, shows a minimum of  $(4.31 \pm 0.33)$  at 15 minutes and a maximum of (6.18  $\pm$  0.72) at 24 hours storage time.

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### **Table 4**

Mean pH values (x), standard deviation (s.d.) and number **(N)** of specimen for light-cured glass ionomers and control groups.



### **Storage Times In Minutes**

ZI = Zionomer

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### Table 5

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Mean pH values (x}, Standard deviation (s.d.) and number (N) of specimen for self-cured glass ionomers.



## Storage Times In Minutes

#### Two-Way Analysis of Variance

A two way analysis of variance (ANOVA) to test the effect of storage time, material, and their interaction was performed. The analysis revealed a significant material-by-time interaction ( $p = 0.0001$ ) at alpha nominal level = 0.01, as shown in Table 19 in the Appendix. The overall effect of time or the overall effect of material could not be assessed; therefore a one way analysis of variance was performed to compare the difference between materials at each storage time, and to evaluate the storage times effect on each material.

#### Material Effect

Values for material specific pH means at each storage time, are presented in Figure 6 in the Appendix. To evaluate the difference between materials at each storage time, a one-way analysis of variance at 1% nominal level is performed between:

- A Light-cured glass ionomer materials
- B Self-cured glass ionomer materials
- C All tested materials

#### One-Way Analysis of Variance Between Light-Cured Materials

Results of the one way ANOVA, between light-cured glass ionomer materials, Tables 20 through 26 in the Appendix revealed a highly significant difference between materials at all storage times ( $P<sub>≤</sub>$  0.0003) except at 120 storage time where there is no significant difference with  $p = 0.157$ . Results of the Scheff'e specific comparison between means, at the 1 percent nominal level and 15 minutes storage time (Table 6) indicate the significant differences between the low pH values of XR-lonomer (4.52  $\pm$  0.16) vs TimeLine (5.4  $\pm$  0.31) and Zionomer (5.47 ± 0.02). After 24 hours storage time, Scheff'e specific comparison, (fable 7), indicates significant differences are between:

- \* Vitrabond vs. Timeline, XR-lonomer and Zionomer.
- \* Timeline vs. Zionomer

Scheff'e specific comparison between means also performed for other test times and the results are summarized in, Table 8.

#### **Comparing Light-Cured with Control Groups**

To compare light-cured glass ionomers with control groups (Shofu polycarboxylate, Durelon and Zinc phosphate) another one-way ANOVA was performed at each storage time and at 1 percent alpha level. ANOVA Tables are listed in the Appendix Table 27 through 33. The analysis revealed a highly significant difference between light cured glass ionomers and control groups ( $p_{\leq}$ 0.0002). Results of Scheff'e test between means, at 1 percent nominal level, indicate the differences are caused by the low mean pH value of all control groups vs. all light-cured glass ionomer except for XR-lonomer, at 15 minutes storage time, Table 9. At 24 hours storage time, Scheff'e test, Table 10, shows that the significant difference is between the low mean pH values of Vitrabond (5.57  $\pm$  0.17) vs the highest mean pH values of Shofu Hy-Bond polycarboxylate,  $(6.5 \pm 0.17)$ .

Scheff'e test also performed at 1 percent nominal level, at the other storage times, and results are presented in Table 11.
$\bar{\bar{z}}$ 

Matrixes of Scheff'e multiple comparison tests between Light-cured Glass

Ionomer Materials at 15 minutes storage time.

(Stars indicate significant difference at 1% Alpha level)



### **Table 7**

Matrixes of Scheff e multiple comparison tests between Light-cured Glass

Ionomer Materials at 24 hours storage time.

(Stars indicate significant difference at 1% Alpha level).



Matrixes of Scheff'e multiple comparison.tests between Light-cured Glass Ionomer Materials. (Stars indicate significant difference at I% . Alpha level).



Matrixes of Scheffe multiple comparison tests between Light-cured Glass

Ionomers and Control Materials at 15 minutes storage times.

(Stars indicate significant difference at 1% Alpha level).



### **Table 10**

Matrixes of Scheffe multiple comparison tests between Light-cured Glass Ionomers And Control Materials at 24 hours storage time.

(Stars indicate significant difference at 1% Alpha level).



# Matrixes of Scheffe multiple comparison tests between Light-cured Glass Ionomers and Control Materials. (Stars indicate significant difference at

<b>Storage Times</b> In Minutes		$\underline{VB}$	<b>TL</b>	XR	$\overline{\mathbf{Z}}$	$S_{\rm P}$	DP	$\overline{\text{ZP}}$
30	<b>VB</b>		$\ast$		$\frac{1}{2}$		*	
	<b>TL</b>			*		*		
	$\ensuremath{\text{XR}}$				$\frac{1}{2}$			
	<b>ZI</b>					*		
	SP						永	
	DP							*
45	VB			ماعا	$\ddagger$		$\ast$	
	<b>TL</b>			sk.				
	<b>XR</b>				ź.			
	ZI							
	SP							
	DP							
60	<b>VB</b>		$\frac{1}{2}$			$\frac{1}{2}$	$\frac{1}{2}$	
	<b>TL</b>			$\star$				$\ast$
	<b>XR</b>							
	ZI							$\ast$
	<b>SP</b>							*
	$\mathbf{DP}$							*
120	$\mathbf{V}\mathbf{B}$							
	<b>TL</b>							
	<b>XR</b>							
	ZI							*
	SP							*
	DP							
180	VB		$\pmb{\ast}$	$\ast$	$\ddot{}$		--	
	<b>TL</b>							
	<b>XR</b>							
	ZI							
	SP							
	$\mathbf{D}\mathbf{P}$							--

1 % Alpha level).

#### One-Way Analysis of Variance Between Self-Cured Materials

Results of the one-way ANOVA between self-cured glass ionomer materials are presented in the Appendix Tables 34 through 40. The analysis shows a highly significant difference between materials at all storage times ( $p = 0.0001$ ), except at 15 minutes storage time with  $p$  value = 0.0004. Scheff'e specific comparison between materials at 1 percent nominal level and 24 hours storage time (Table 12), indicate the significant difference is caused by the low mean value of Baseline (4. 7  $\pm$  0.22) vs. each of the following: Ketac-Bond (6.47  $\pm$  0.04) Dentin cement (6.39  $\pm$  6.17), Ketac-Cem (6.32  $\pm$  0.33) and Shofu glass ionomer Type I (6.23  $\pm$  0.23).

Scheff'e specific comparison test was also performed for other storage times at the 1 percent nominal level. Results are presented in Table 13.

#### Comparing Self-Cured with Control Group

In order to compare self-cured glass ionomer with control groups (Shofu Hy-Bond, Durelon and Zinc phosphate) another seven one-way ANOVA was performed at 1 percent alpha level, ANOVA Tables are presented in appendix Tables 41 through 47. The analysis revealed a highly significant difference between materials  $p = 0.0001$  at all times. The Scheff'e test indicates, at 15 minutes storage time, the significant difference is between Baseline vs. Shofu glass ionomer Type I. It also indicates that there is no significant difference between selfcured glass ionomers and control groups. At 24 hours storage time (Table 14) the test shows that the significant difference is caused only by the low mean pH values of BaseLine (4.7  $\pm$  0.22) vs. all self-cured glass ionomers and all control groups.

Matrixes of Scheffe multiple comparison tests between Self-cured

Glass Ionomer Materials after 24 hours storage time.

(Stars indicate significant difference at 1% Alpha level).



Matrixes of Scheffe multiple comparison tests between

Self-cured Glass Ionomer Materials. (Stars indicate significant difference



# at 1% Alpha level).

Matrixes of Scheffe multiple comparison tests for Self-cured Glass

Ionomers and Control Materials after 24 hours.

(Stars indicate significant difference at I% Alpha level).



 $\alpha$ 

Scheff'e test was also performed for other storage times, at 1 percent nominal level, and results are tabulated in Table 15a and 15b.

#### **Comparison Between All Materials**

The overall one-way ANOVA for four light-cured glass ionomers, six selfcured glass ionomers, two polycarboxylates and zinc phosphate cements are presented in the Appendix Table 48 through 54. Results show a highly significant difference between materials at all storage times ( $p = 0.0001$ ). Results of the Scheff'e multiple comparison at 1 percent nominal level for 15 minutes and 24 hours storage times are as the following:

- 1. At 15 minutes storage time (Table 16) the significant difference was caused by the low mean values of self-cured Fuji I (3.71  $\pm$  0.2) and BaseLine  $(3.65 \pm 0.27)$  vs. each of the light-cured, Zionomer  $(5.47)$  $\pm$  0.2), TimeLine (5.4  $\pm$  0.3) and VitraBond (5.21  $\pm$  0.33).
- 2. At 24 hours storage time (Table 17) the significant difference is mainly caused by the low mean pH values of self-cured BaseLine  $(4.7 \pm$ 0.22) vs each of the following:



### **Table 15-a**

# Matrixes of Scheffe multiple comparison tests between Self-cured Glass

Ionomer and Control Materials for 15, 30 and 45 minutes.

(Stars indicate significant difference at 1% Alpha level).



### Table 15-b

# Matrixes of Scheff'e multiple comparison tests between Self-cured Glass

Ionomer and Control Materials for 60, 120 and 180 minutes.

(Stars indicate significant difference at 1% Alpha level).



 $\alpha$ 

Matrixes of Scheffe multiple comparison tests between all materials at 15 minutes storage time. (Stars indicate significant difference at 1% Alpha level).



### **Table 17**

Matrixes of Scheffe multiple comparison tests between all materials at 24 hours storage time. (Stars indicate significant difference at 1%) Alpha level).





Scheff'e multiple comparison test was also performed for other storage times, at 1 percent nominal level. Results are presented in Table 18.

#### Storage Time Effect

To evaluate the effect of storage times (15 minutes, 30 minutes, 45 minutes, 1 hour, 2 hours, 3 hours and 24 hours) for each materials, seven separate oneway ANOVA were performed. The ANOVA Tables are presented in the Appendix Table 55 through 67. The analysis revealed a highly significant difference for all materials except Vitrabond, where there is no significant storage time effect  $p =$ 0.0784.

All materials show the increase in pH values with time, as expected, up to 24 hours from mixing time. The patterns of pH increase are presented graphically in Figure 3 for light-cured, Figure 4 for self-cured and Figure 5 for control groups.

Matrixes of Scheff'e multiple comparison tests between all materials at all storage times. (Stars indicate significant difference at 1% Alpha level).



# Figure 3







Storage time in minutes (Log Time).

# Figure 4

Acidity level as function of storage time



for Self-cured Glass Ionomer Materials.

Storage time in minutes (Log Time).



Figure 5

Storage times in minutes (Log Time).

#### **DISCUSSION**

The objective of this study was to evaluate in vitro the acidity of four lightcured glass ionomers, six self-cured glass ionomers, and to compare them with polycarboxylate and zinc phosphate cements. Materials were tested after seven periods of storage (15 minutes, 30 minutes, 45 minutes, 60 minutes, 120 minutes, 180 minutes and after 24 hours). Also this investigation compared the pH level of all materials. All cements tested behaved differently with respect to the pH.

#### Light-Cured Glass lonomer Liners

The results show a high pH value for all light-cured materials 15 minutes after mixing with a range of 5.21 - 5.47, except for XR-lonomer which was 4.5. This may be explained by the absence of HEMA in the XR liquid, which results in a material with an initial set that is clinically workable, but much softer than the other liners.  $12$ 

Although the initial setting of the light-cured ionomers is fast since an initial covalent bond is formed between the methyacrylate groups on the polyacid chain, there still exists auto curing ionic bonds between the glass to the polyacrylic acid matrix. <sup>12</sup> This setting reaction is reflected in pH changes up to 24 hours.

Vitrabond behaved differently in that the pH did not change with time from the initial set up to 24 hours. This may reduce the chance of having free acid available to cause a pulpal reaction, however, the pH of this material after 24 hours

40

is still acidic (pH  $5.6 \pm 0.17$ ).

Initially XR-lonomer showed a hydrophilic behavior. After light-curing the material contracted away from the ring. When two drops of water were added, the material expanded. This supports the claims made by the manufacturer that XRlonomer shrinks 3% during light curing and after setting it absorbs a slight amount of water from the oral environment, resulting in a 4.5% expansion.<sup>12</sup> This material behavior may dehydrate the dentin and conceivably elicit pain and result in aspiration of odontoblasts into the tubules although its a light-cured material<sup>30</sup>.

Zionomer showed the highest pH of all light-cured materials at 15 minutes  $(5.5 \pm 0.02)$  and after 24 hours  $(6.7 \pm 0.08)$ .

#### Self-Cured Glass lonomers

The data indicated a slower but similar increase in the pH for the self-cured materials from 15 minutes up to 24 hours except for Fuji lonomer and Baseline.

Fuji lonomer at 15 minutes started at low pH (3.7  $\pm$  0.20) which gave an indication that this material at early stage (0 minutes) exhibits a very low pH. This low pH may be explained since this material is used as a luting cement rather than a base/lining cements. Smith, et. al suggested that with lining cements the period of pH 2 or 3 is shorter than the luting cement for the first two minutes. Thus pulpal response is less likely with lining materials. <sup>40</sup>

Baseline when compared with the other materials that are used as a base/lining cements, shows the lowest pH (3.7  $\pm$  0.27) at 15 minutes and it shows the lowest, slowest rate reaction up to 24 hours (pH =  $4.7 \pm 0.22$ ). This may indicate a less complete setting of the material.

The differences in the delivery system between Baseline and the other

materials may account for the low pH level of this material. The active polyacid in Baseline is in powder form mixed with glass powder and the liquid is water.

#### Between All Materials

Previous research <sup>37,38,40</sup> has implied that the pH of a setting dental cement is critical to producing pathological pulpal responses. Plant and Tyas suggested that if the pH is near 2, pulpal response depends on the duration of the low pH and is enhanced by the quantity of available acid.  $41$  Smith and Ruse found there was a rapid rise in pH during the first 15 minutes after mixing, showing a pH of 2 for at least 5 minutes and 3 for at least 10 minutes for all glass ionomer cements. They concluded that the early acidity of the glass ionomer cements may be a major contributor to pulp sensitivity, <sup>38</sup> However, none of these studies specified the exposure time that is needed for a low pH to elicit a pulp response, neither did they specify the level of pH that might cause pulp pathology.

A study done by Svare and Meyer<sup>42</sup> showed that acids at pH 2.8 to 2.9 induced vascular thrombosis in the pulps of rats. They conclude that if the pH is not below 2 or 3 there will be no effect on the pulp, however, that approach is misleading.

The present data supports the findings of Smith and Ruse $36$  that after 15 minutes all materials show a slow increase of pH up to 24 hours. The pH at 15 minutes for all materials ranges between 3.65 - 5.47 and at 24 hours the pH ranges between 4.70 -6.72. This slow increase indicates that the setting reaction is not complete and there is still free acid present. This free acid even at late stages (after 15 minutes - 24 hours) may cause mild pulp response. So we suggested that pulp irritation may occur not only at the early stages of setting but also at the later stages as long as the reaction is not complete and free acid still exists. The severity of pulp responses may vary depending upon the setting rate of the cement.

The pH values of self-cured materials obtained in this study are slightly higher than those reported in previous studies.<sup>38,40</sup> A possible explanation for the higher value could be that the pH values in this study were obtained via a deionized water bridge between the electrode and the set cements, which seemed to affect the results by 1 or 2 pH units.  $38$  The fact that most of these materials were mixed and measured as base/lining material and are used in a thicker mixture at a higher powder /liquid ratio (Table II), except for Fuji lonomer and Hy-Bond polycarboxylate which are used as a luting cement may account for higher pH values.

Comparing Fuji lonomer and Hy-Bond polycarboxylate, Fuji lonomer shows a higher acidity level and a longer setting time than Hy-Bond polycarboxylate. This supports the finding that the initial setting of the glass ionomer cements are slow since first calcium and then aluminum ions are leached from the glass on reaction with the aqueous polyacid.<sup>19</sup>

Analysis of these results showed light-cured glass ionomer liners were significantly less acidic than polycarboxylates (Shofu Hy-Bond and Durelon) and zinc phosphate cement. Since the pH and the free acidity depend on the setting rate of the cement, light-cured materials will have more complete setting in the early stages than the self-cured materials. Thus, it seems unlikely that an initial pulp response would be expected with these materials.

The pH level of self-cured glass ionomer cements were similar to that of

polycarboxylate and zinc phosphate cements. This finding indicates that glass ionomer cements may be safely used in dentistry as well as the widely used polycarboxylate and zinc phosphate, as far as acidity is concerned.

All pH measurements were made at room temperature which affects the setting rate, the pH may rise more rapidly in the mouth than at the room temperature.<sup>38</sup>

Previous research<sup>43,44</sup> suggested that premature moisture contamination of the glass ionomer before completion of its setting reaction may allow fluids to contact cut dentin surfaces, thereby giving rise to sensitivity. With light-cured glass ionomer this may not occur since the setting reaction of this material will be triggered by visible light which shortens the setting time.

An unexpected sharp drop in pH was observed after 120 minutes storage time. This drop in pH was generally observed with the self-cured glass ionomers (Figure 3) and polycarboxylate (Durelon, Figure 5). This phenomena may be explained by one of the following:

1. Technical error: the drop in pH values of the materials may be caused by temperature change when the sample is removed from the humidity chamber to the room temperature  $(37^{\circ}C - 22^{\circ}C)$  respectively.

2. Chemical Reaction Change: the sharp drop phenomena might result from a change in the nature of the chemical reaction at that time. This assumption is more favorable than the technical error, because this drop occurs only with self-cured materials and not with light-cured materials, even though all materials were stored in the same manner. This hypothetical explanation can only be confirmed with more investigation using specific analysis like Fourier Transform Infrared spectroscopy (FTIR).

If the initial acidity is one factor of pulp sensitivity, light-cured glass ionomer liners may reduce this factor. However, routine use of calcium hydroxide continues to be suggested <sup>34,37</sup> especially in deep preparations near the pulp. Proper isolation and material mainpulation remain critical to this success.

#### **CONCLUSION**

In conclusion, inflammation and possible irreversible damage to dental pulp due to prolonged exposure to acidity, should always affect the dentist's decision in choosing a particular dental material. Other factors which may be the cause of pulp sensitivity observed with glass ionomer cements must include: mechanical irritation, microleakage, bacterial contamination during cavity preparation, the preexisting condition of the tooth before tooth preparation, the depth and extent of preparation and age of the patient.

Under the conditions of this study:

- 1. The acidity of light-cured glass ionomer liners with exception of XR is less than that of self-cured glass ionomers, polycarboxylate and zinc phosphate cements up to 1 hour storage time.
- 2. Of the materials tested, Baseline and Fuji lonomer are the most acidic up to 24 hours. However, the pH of Fuji lonomer rises above Baseline at 24 hours (pH =  $6 \pm 0.59$ )
- 3. Almost all materials after 24 hours storage time, show an increase in pH values to a final pH approaching 7 except Baseline which showed the lowest pH value  $(4.7 \pm 0.22)$  at 24 hours.
- 4. From the acidity point of view, self-cured glass ionomer cements as well as polycarboxylate and zinc phosphate cements may be safely used in restorative dentistry as bases and liners.

5. In light of the results obtained in this study, light-cured glass ionomer cements appear to be a material that can be successfully used in restorative procedures as Base/Lining materials, however, further data for pulp sensitivity and clinical studies are needed.

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APPENDIX

 $\label{eq:2.1} \mathcal{L}(\mathcal{L}^{\text{max}}_{\mathcal{L}}(\mathcal{L}^{\text{max}}_{\mathcal{L}})) \leq \mathcal{L}(\mathcal{L}^{\text{max}}_{\mathcal{L}}(\mathcal{L}^{\text{max}}_{\mathcal{L}}))$ 

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Two-way analysis of variance for materials and storage times.



# One-way analysis of variance for Light-cured materials tested





# Table 21

# One-way analysis of variance for Light-cured materials tested

after 30 minutes storage time.



# One-way analysis of variance for Light-cured materials tested

after 45 minutes storage time.

Source:	df:	Sum of Squares:	Mean Square:	F-test:	P value:
Between subjects	14	.282	.071	.228	.9185
Within subjects	15	4.641	.309		
treatments	3	3.78	1.26	17.568	.0001
residual	12	.861	.072		
Total	19	4.923			

Table 23

# One-way analysis of variance for Light-cured materials tested

after 60 minutes storage time.



 $\sim 10^{-1}$ 

One-way analysis of variance for Light-cured materials tested

after 120 minutes storage time.





One-way analysis of variance for Light-cured materials tested

after 180 minutes storage time.



# One-way analysis of variance for Light-cured materials tested

after 24 hours storage time.



### Table 27

One-way analysis of variance for Light-cured materials

including control groups tested after 15 minutes storage time.



One-way analysis of variance for Light-cured materials

including control groups tested after 30 minutes storage time.

Source:	dt:	Sum of Squares:	Mean Square:	F-test:	P value:
Between subjects	14	1.184	.296	.888	.4831
Within subjects	30	10.005	.333		
treatments	6	8,466	1.411	22.011	.0001
residual	24	1.539	.064		
Total	34	11.189			

Table 29

One-way analysis of variance for Light-cured materials

including control groups tested after 45 minutes storage time.


One-way analysis of variance for Light-cured materials including control groups tested after 60 minutes storage time.



Table 31

One-way analysis of variance for Light-cured materials

including control groups tested after 120 minutes storage time.



# One-way analysis of variance for Light-cured materials

including control groups tested after 180 minutes storage time.



Table 33

# One-way analysis of variance for Light-cured materials

including control groups tested after 24 hours storage time.



### One-way analysis of variance for Self-cured materials tested



### after 15 minutes storage time.

### Table 35

### One-way analysis of variance for Self-cured materials tested

after 30 minutes storage time.



### One-way analysis of variance for Self-cured materials tested

### after 45 minutes storage time.



Table 37

### One-way analysis of variance for Self-cured materials tested

after 60 minutes storage time.



# One-way analysis of variance for Self-cured materials tested

after 120 minutes storage time.



### Table 39

# One-way analysis of variance for Self-cured materials tested

after 180 minutes storage time.



 $\bar{z}$ 

### One-way analysis of variance for Self-cured materials tested



### after 24 hours storage time.

### Table 41

One-way analysis of variance for Self-cured materials

including control groups tested after 15 minutes storage time.



### One-way analysis of variance for Self-cured materials

including control groups tested after 30 minutes storage time.

Source:	df:	Sum of Squares:	Mean Square:	F-test:	P value:
Between subjects	4	1.325	.331	.906	.4698
Within subjects	40	14.629	.366		
treatments	8	10.635	1.329	10.649	.0001
residual	32	3.995	.125		
Total	44	15.954			

Table 43

One-way analysis of variance for Self-cured materials

including control groups tested after 45 minutes storage time.



## One-way analysis of variance for Self-cured materials including

control groups tested after 60 minutes storage time.

Source:	df:	Sum of Squares:	Mean Square:	F-test:	P value:
Between subjects		.233	.058	.206	.9336
Within subjects	40	11.316	.283		
treatments	8	10.613	1.327	60.344	.0001
residual	32	.703	.022		
Total	44	11.549			

Table *45* 

One-way analysis of variance for Self-cured materials including

control groups tested after 120 minutes storage time.



One-way analysis of variance for Self-cured materials including

control groups tested after 180 minutes storage time.

Source:	df:	Sum of Squares:	Mean Square:	F-test:	P value:
Between subjects	4	.318	.079	.21	.9316
Within subjects	40	15.165	.379		
treatments	a	13.412	1.676	30,596	.0001
residual	32	1.753	.055		
Total	44	15.483			

Table 47

One-way analysis of variance for Self-cured materials including

control groups tested after 24 hours storage time.



# One-way analysis of variance for all materials tested after



### 15 minutes storage time.

Table 49

# One-way analysis of variance for all materials tested after

30 minutes storage time.



# One-way analysis of variance for all materials tested after

### 45 minutes storage time.



### Table 51

# One-way analysis of variance for all materials tested after

### 60 minutes storage time.



### One-way analysis of variance for all materials tested after

### 120 minutes storage time.



### Table 53

## One-way analysis of variance for all materials tested after

180 minutes storage time.



### One-way analysis of variance for all materials tested after

24 hours storage time.



Table 55

One-way analysis of variance for Light-cured Vitra bond



# One-way analysis of variance for Light-cured TimeLine

material tested after seven different lengths of storage times.

Source:	df:	Sum of Squares:	Mean Square:	F-test:	P value:
Between subjects	4	.246	.062	.626	.6479
Within subjects	30	2.951	.098		
treatments	6	2.459	.41	19.972	.0001
residual	24	.492	.021		
Total	34 <sup>°</sup>	3.197			

Table 57

One-way analysis of variance for Light-cured XR-Ionomer



One-way analysis of variance for Light-cured Zionomer

material tested after seven different lengths of storage times.

Source:	df:	Sum of Squares:	Mean Square:	F-test:	P value:
Between subjects	4	.015	.004	.022	.999
Within subjects	30	5.06	.169		
treatments	6	4.559	.76	36.343	.0001
residual	24	.502	.021		
Total	34	5.075			

Table 59

One-way analysis of variance for Self-cured Ketac-Cem



# One-way analysis of variance for Self-cured GC Fuji I

material tested after seven different lengths of storage times.

Source:	df:	Sum of Squares:	Mean Square:	F-test:	P value:
Between subjects	$\overline{\phantom{a}}$	2.918	.729	1.356	.2727
Within subjects	30	16.143	.538		
treatments	6	14.34	2.39	31.817	.0001
residual	24	1.803	.075		
Total	34	19.06			

Table 61

One-way analysis of variance for Self-cured Shofu Type I



# One·way analysis of variance for Self-cured Katac·Bond material tested after seven different lengths of storage times.





One·way analysis of variance for Self·cured Baseline



# One-way analysis of variance for Self-cured GC Dentin cement

material tested after seven different lengths of storage times.

Source:	df:	Sum of Squares:	Mean Square:	F-test:	P value:
Between subjects	4	.71	.177	.476	.7531
Within subjects	30	11.184	.373		
treatments	6	10.186	1.698	40.829	.0001
residual	24	.998	.042		
Total	34	11.894			

Table 65

One-way analysis of variance for Shofu Hv-Bond polycarboxvlate



One-way analysis of variance for Durelon material tested

after seven different lengths of storage times.

Source:	df:	Sum of Squares:	Mean Square:	F-test:	P value:
Between subjects		.142	.035	.095	.9832
Within subjects	30	11.145	.371		
treatments	6	10.556	1.759	71.77	.0001
residual	24	.588	.025		
Total	34	11.286			

Table 67

One-way analysis of variance for Zinc phosphate material



### **APPROVAL SHEET**

The thesis/dissertation submitted by: **NAJWA M. JOWHARJI**  has been read and approved by the following committee:

### **Dr. James L. Sandrik, Director**

Professor and chairman of Dental Material department, Loyola.

#### **Dr. Roger G. Noonan,**

Associate Professor and Director of Post graduate students, Department of Pediatric Dentistry, Loyola.

#### **Dr. Joseph M. Gowgiel,**

Professor and chairman of Dental Anatomy Department, Loyola.

The final copies have been examined by the director of the thesis/dissertation and the signature which appears below verifies the fact that any necessary changes have been incorporated and that the thesis/dissertation is now given final approval by the Committee with reference to content and form.

The thesis/dissertation is therefore accepted in partial fulfillment of the requirements for the degree of **{Master Of Science).** 

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 $u$ L. Sandik

Director's Signature

Date